

# Non-Equilibrium Dynamics of Biological Matter and Cellular Mechanosensing

Christoph Schmidt



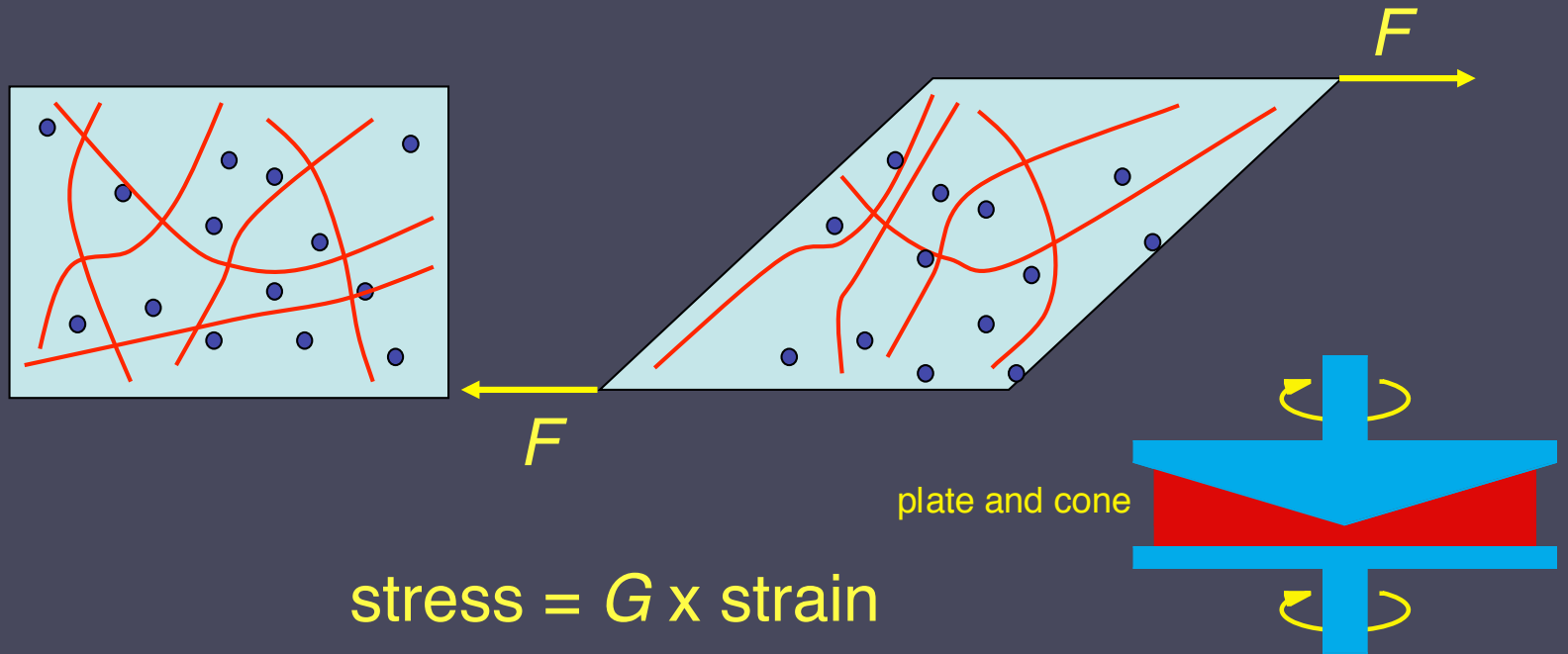
# non-equilibrium mechanics of cells



dancing fish keratocytes

keratocyte waltz, Cyrus Wilson,  
Julie Theriot's lab, Stanford

# shear deformation of a viscoelastic object

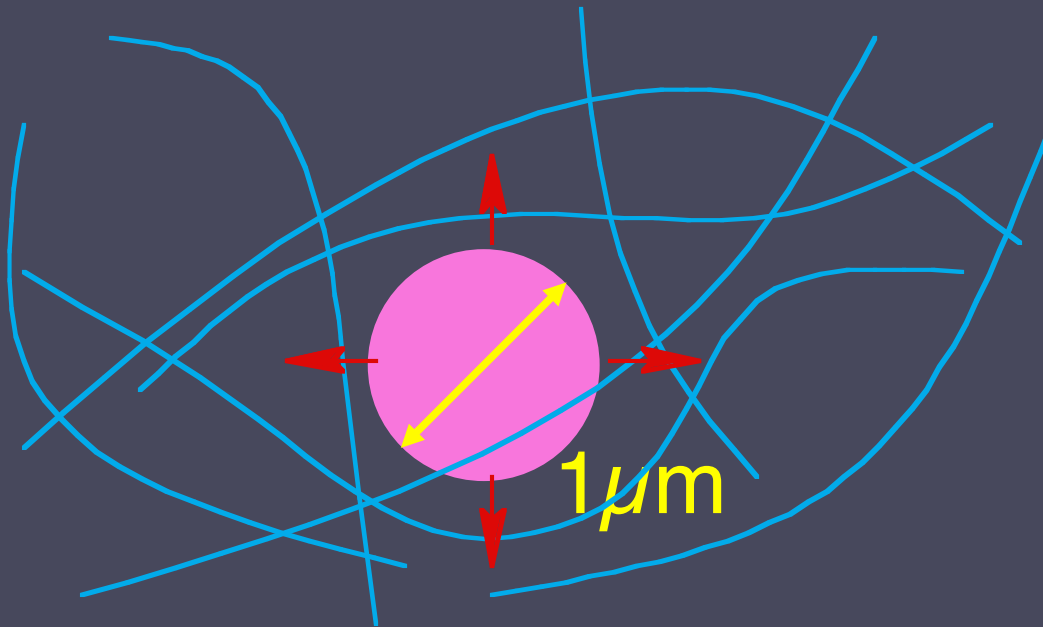


complex shear modulus:  $G^*(\omega) = G'(\omega) + i G''(\omega)$

↑  
storage modulus

↑  
loss modulus

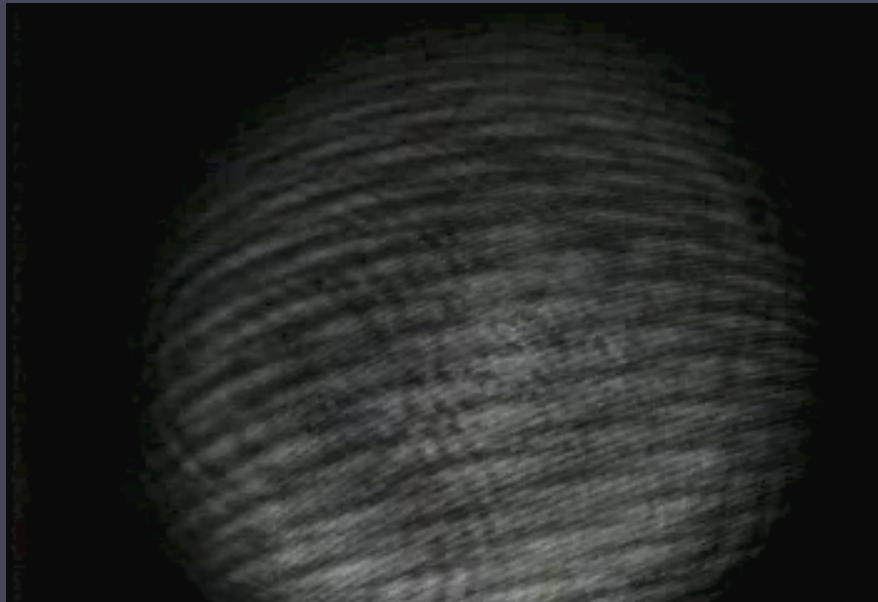
# Microrheology



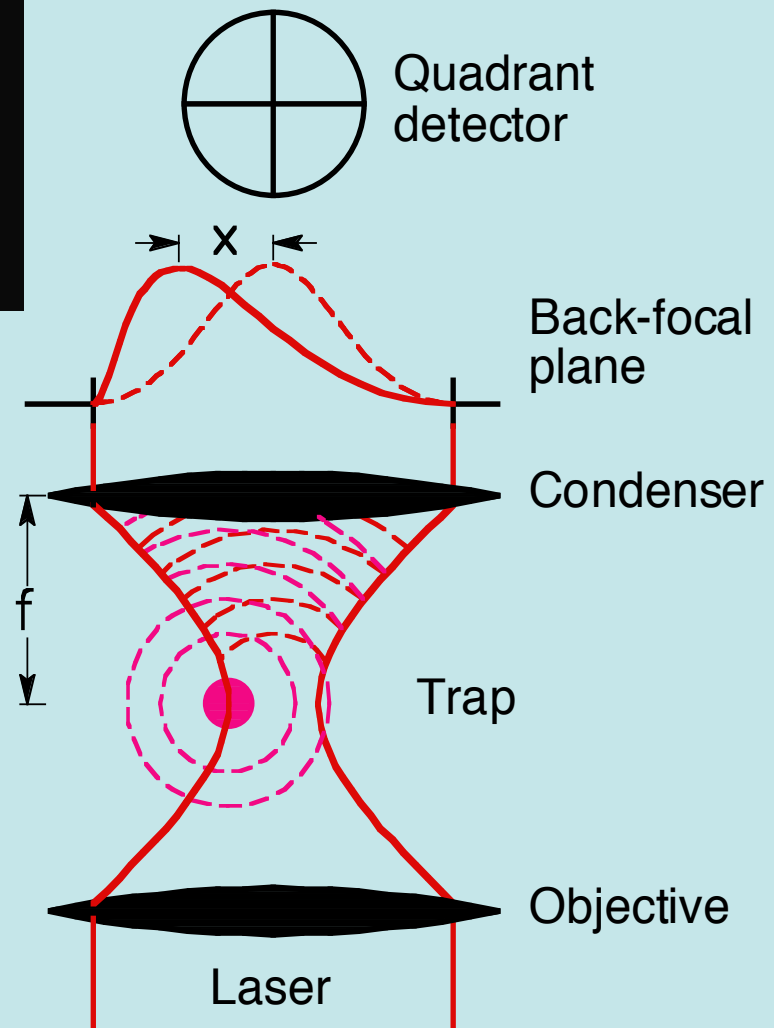
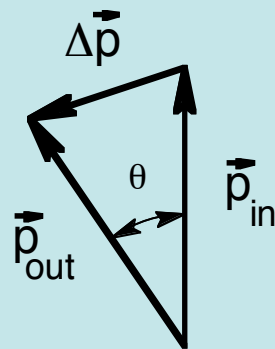
## advantages:

- study inhomogeneities
- study small samples, biological cells
- reach high frequencies ( $\rightarrow$  MHz) w/o inertial effects
- probe scale dependent material properties by varying probe size
- active vs. passive, single bead vs multiple bead (Sackmann, Valberg, Zaner Fredberg, Weitz & Co.: Mason, Crocker)

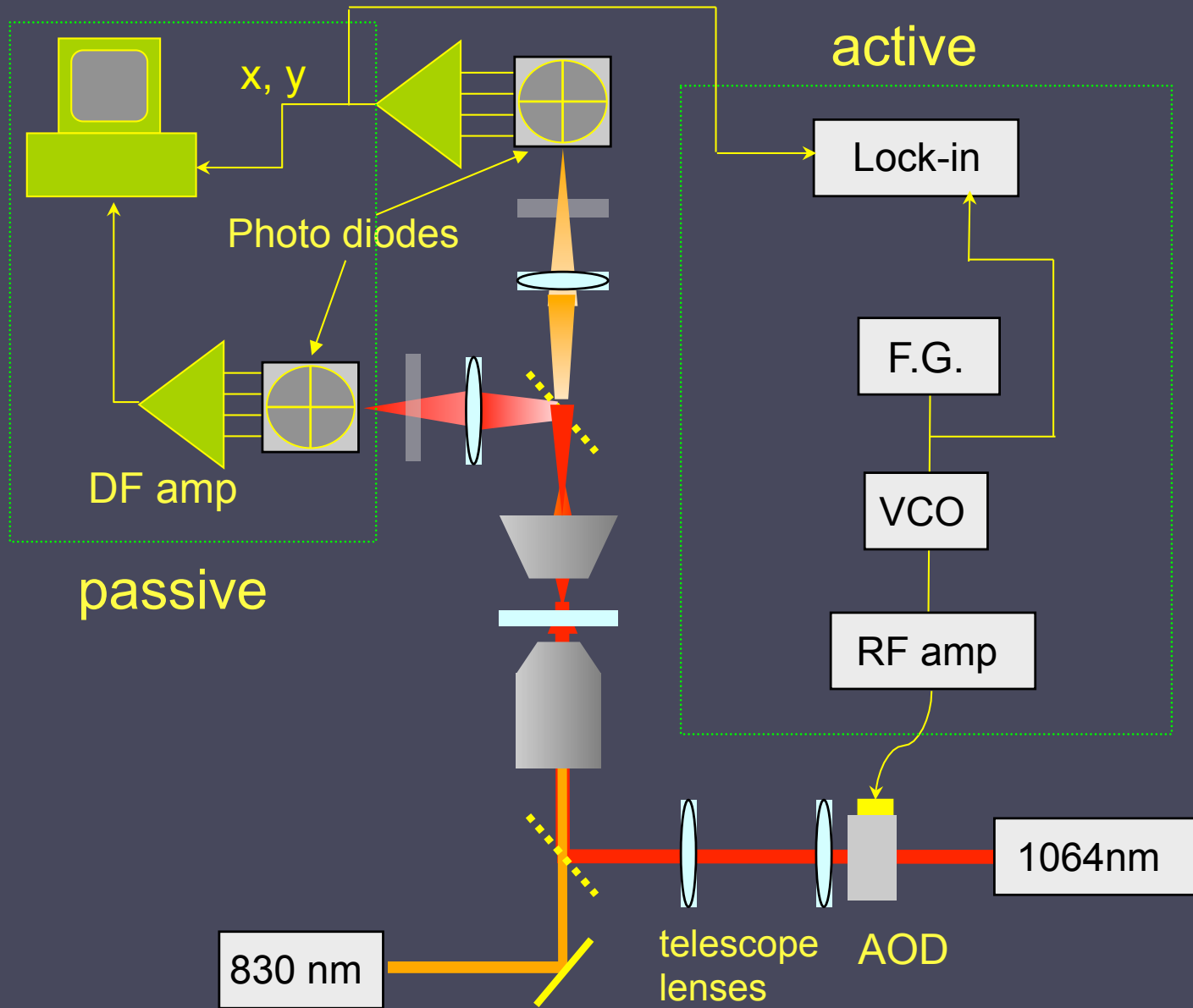
# interferometric position detection



$$F = \frac{dp}{dt} = \frac{l}{c} \sin \theta = \frac{l}{c} \frac{x}{f}$$



# passive and active microrheology



# passive microrheology, data processing

parameters:

entanglement length > mesh size

persistence length > mesh size

$0.1 \text{ Hz} < \omega/2\pi < 20 \text{ kHz}$

for larger beads and higher frequencies:

generalized Stokes-Einstein:

$$x_\omega = \alpha^*(\omega) f(\omega)$$

$$\alpha^*(\omega) = \frac{1}{6\pi G^*(\omega) a}$$

data processing:

time-series data,  $x(t)$

power spectral density,  $\langle x_\omega^2 \rangle$

$G'(\omega), G''(\omega)$

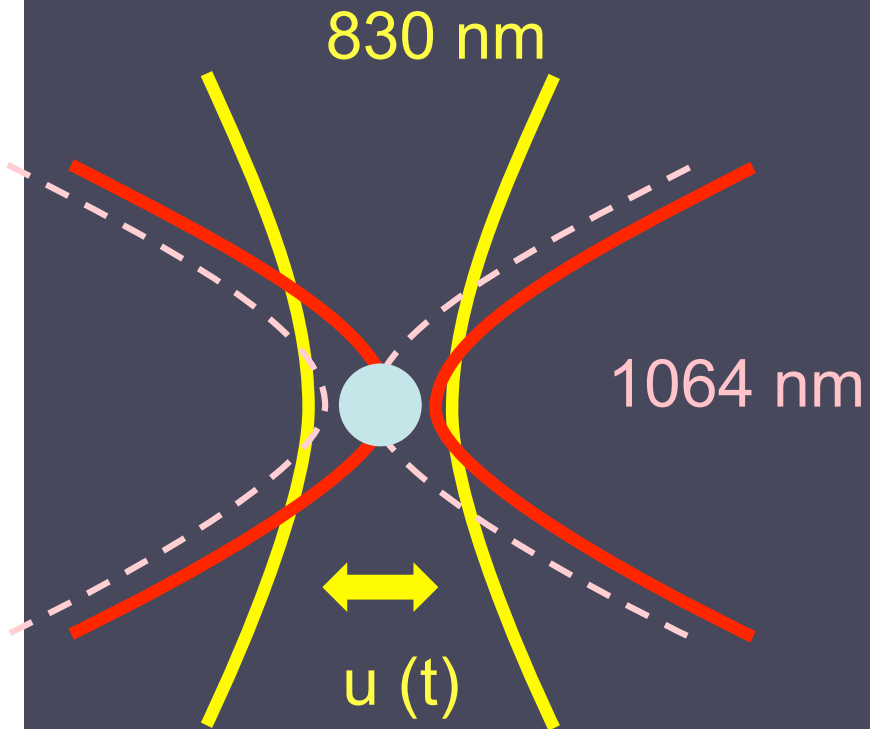
fluctuation-dissipation:  $\langle x_\omega^2 \rangle = \frac{4k_B T \alpha''(\omega)}{\omega}$

Kramers-Kronig:

$$\alpha'(\omega) = \frac{2}{\pi} P \int_0^\infty \frac{\xi \alpha''(\xi)}{\xi^2 - \omega^2}$$

Gittes, Schnurr, MacKintosh, Schmidt, PRL 79:3286 ('97)  
Schnurr, Gittes, MacKintosh, Schmidt, Macromol. 30:7781 ('97)

# active microrheology



Response function

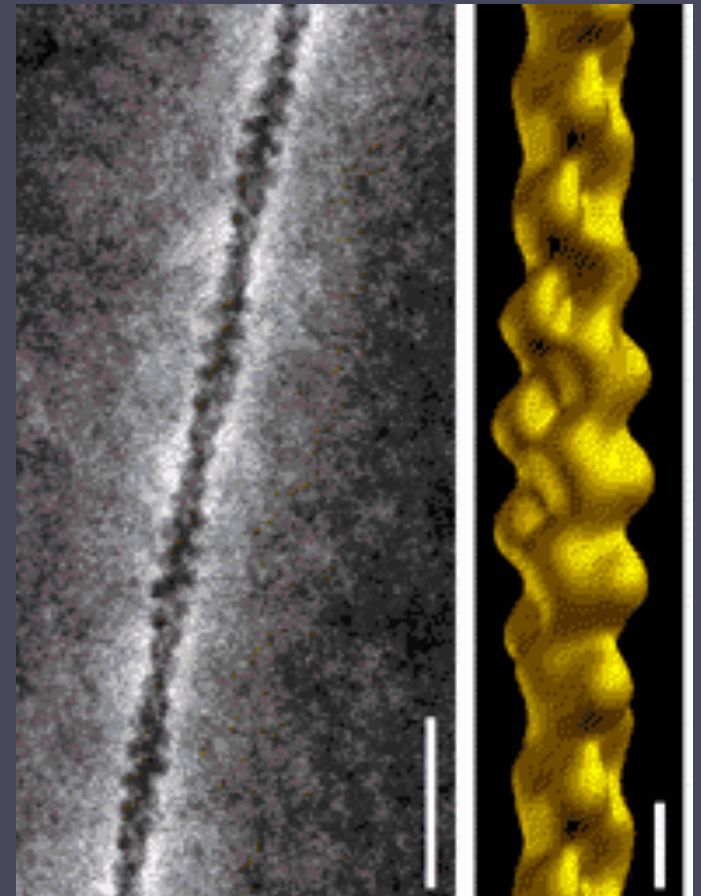
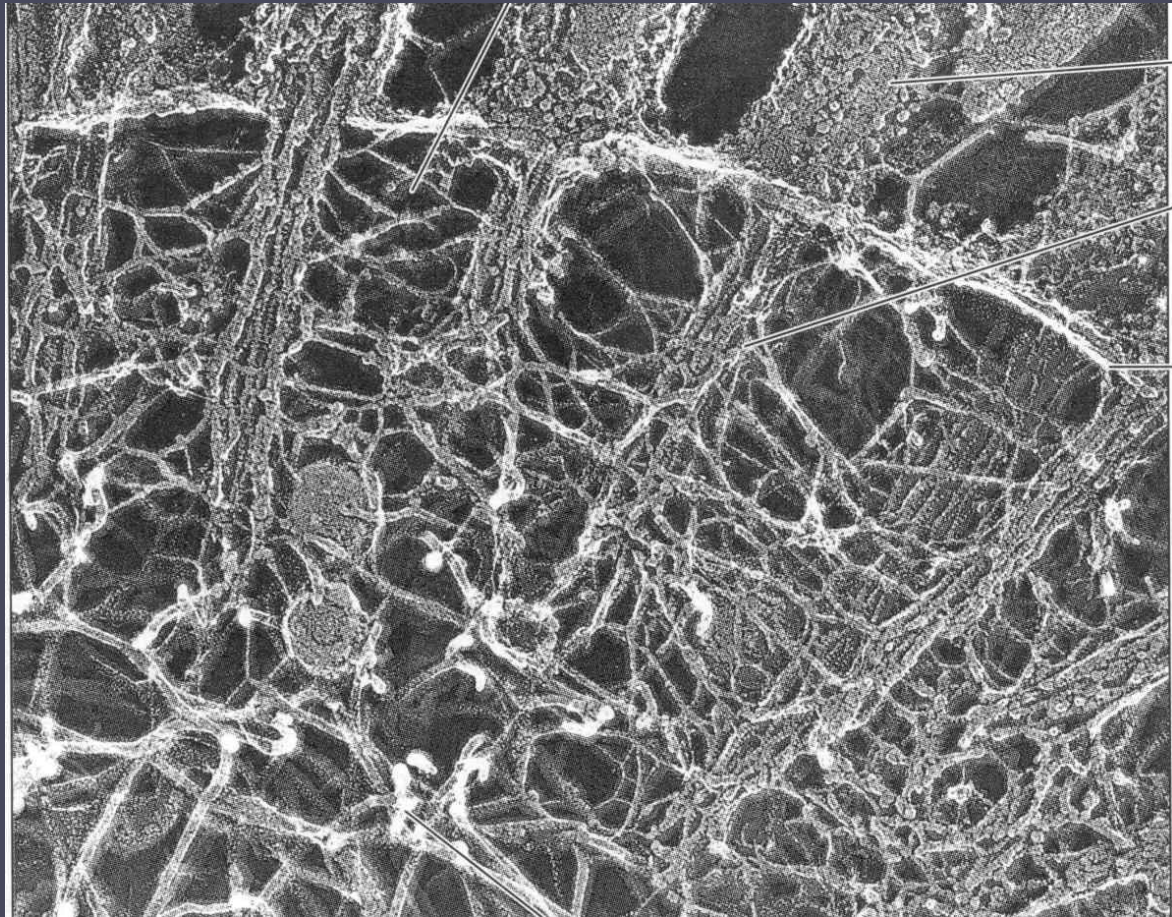
$$u(\omega) = A(\omega) F(\omega)$$

Fluctuation-dissipation:

$$C(\omega) = \frac{2k_B T}{\omega} A''(\omega)$$



# biological non-equilibrium network: actin cortex



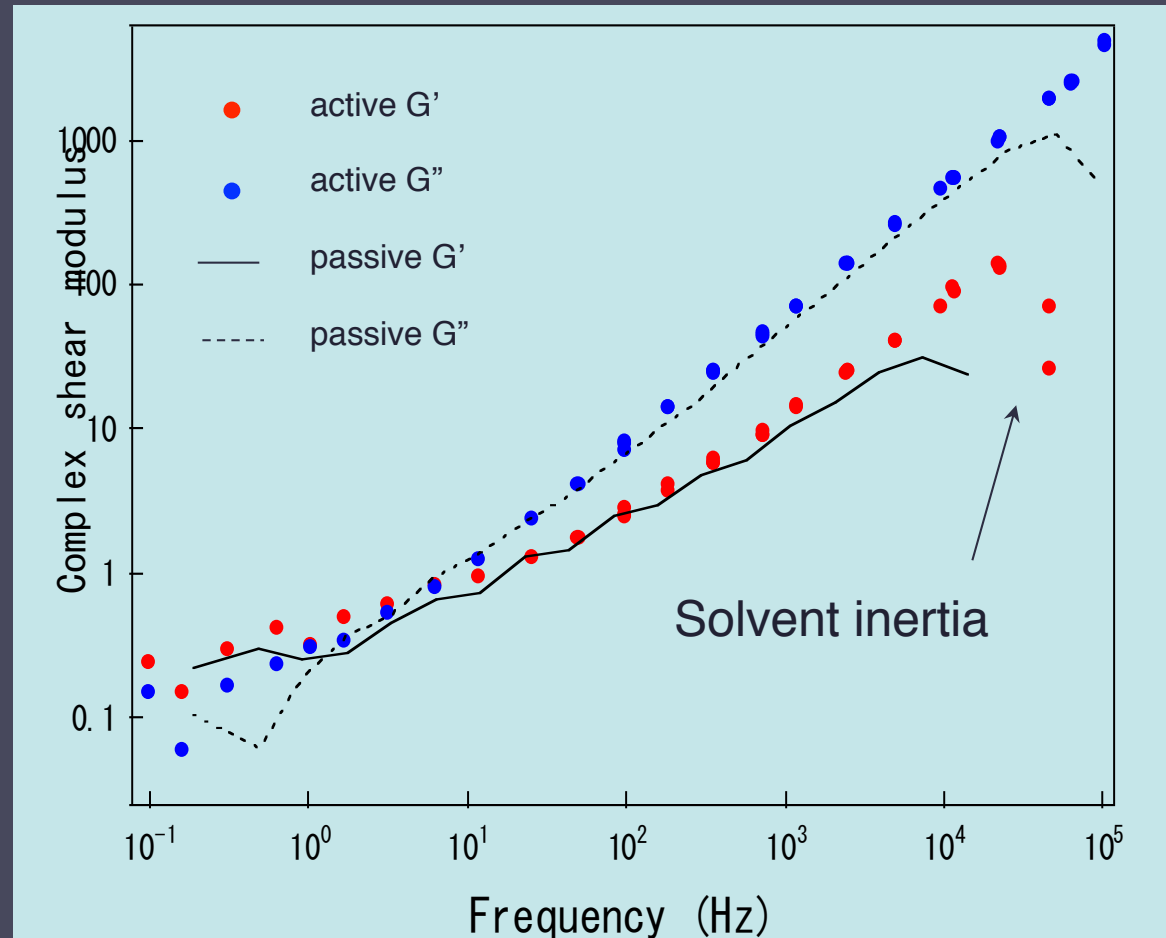
John Heuser, Washington University

# comparison active/passive method

bead size  $2.56 \mu\text{m}$

actin solution (1mg/ml)

$$\lim_{\omega \gg \tau_{\perp}^{-1}} B(\omega) = \frac{\kappa^2}{k_B T} \left( \frac{2i\omega\zeta_{\perp}}{\kappa} \right)^{3/4}$$

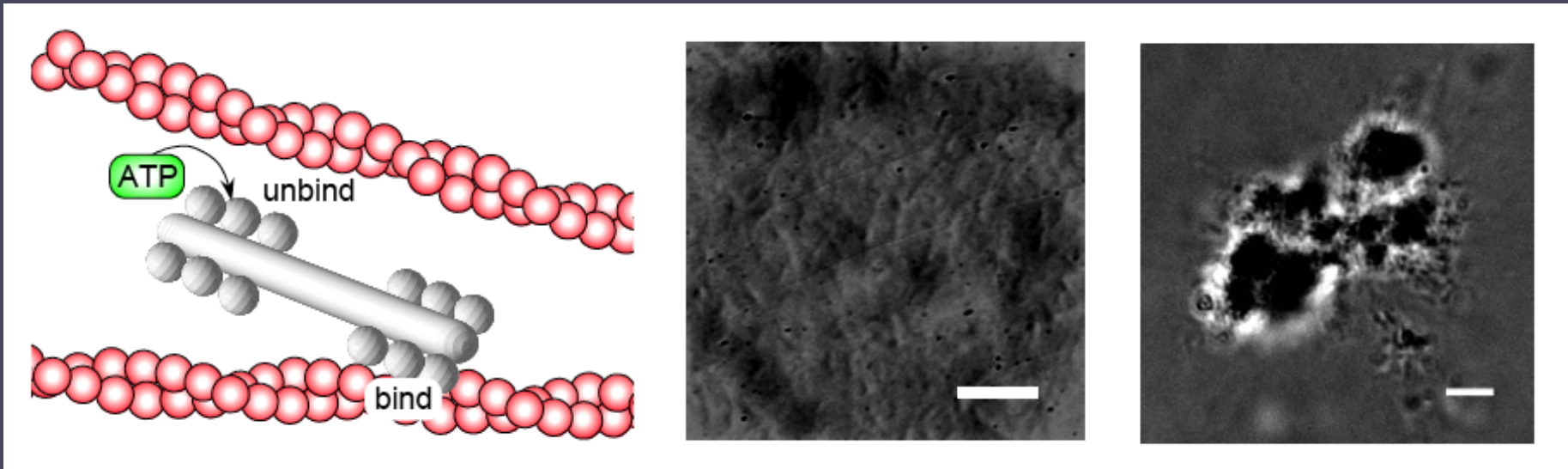


active method : no influence of cut-off in Kramers-Kronig integral,  
but see solvent inertia

solvent inertia: Atakhorrami, Koenderink, MacKintosh, Schmidt, PRL 95:208302 (2005)

3/4 theory: Gittes and MacKintosh: PRE, 58, R1241 (1998); Morse, Macromolecules, 31:7044 (1998)

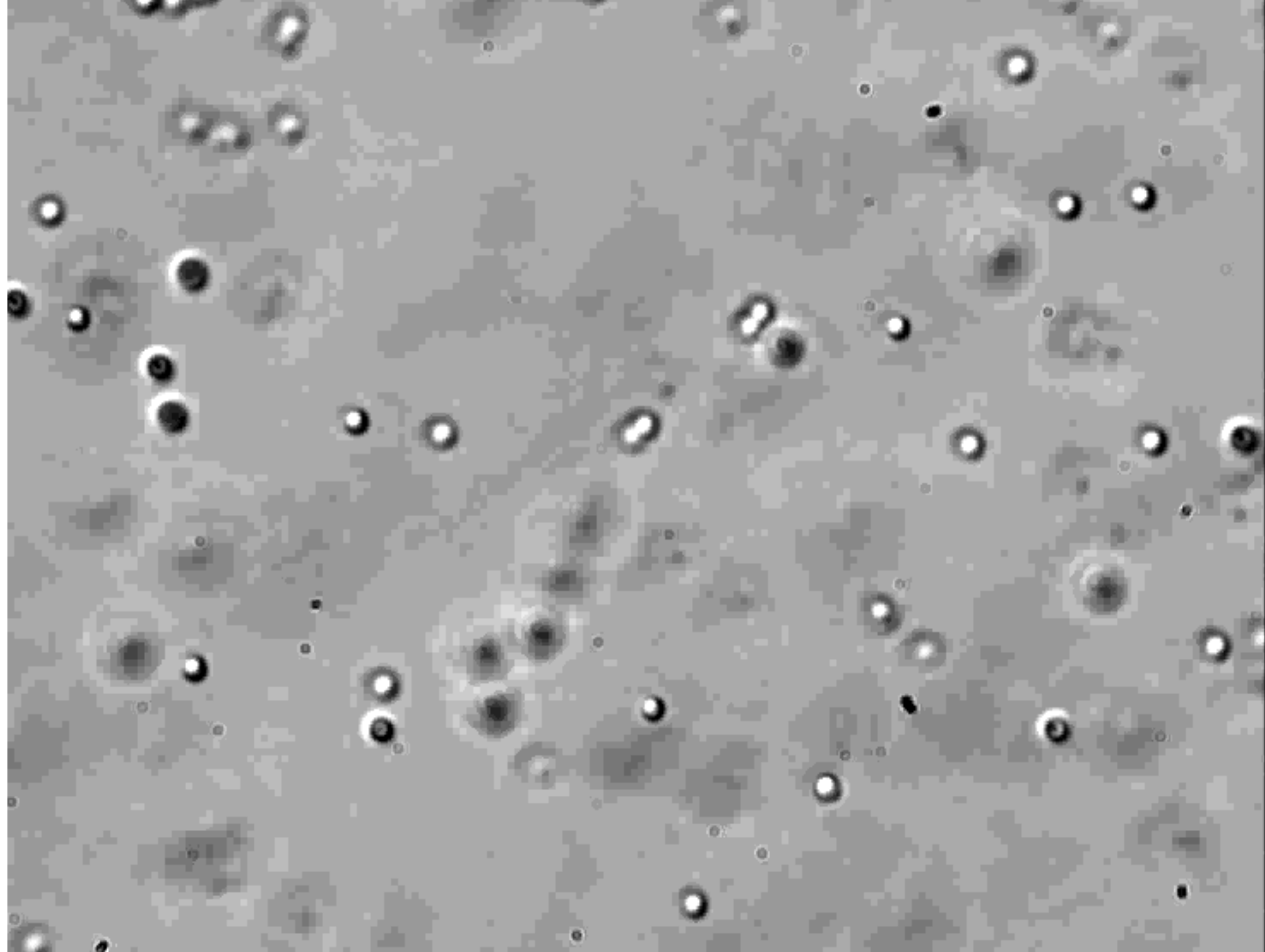
non-equilibrium model network,  
actin + myosin + cross-linker



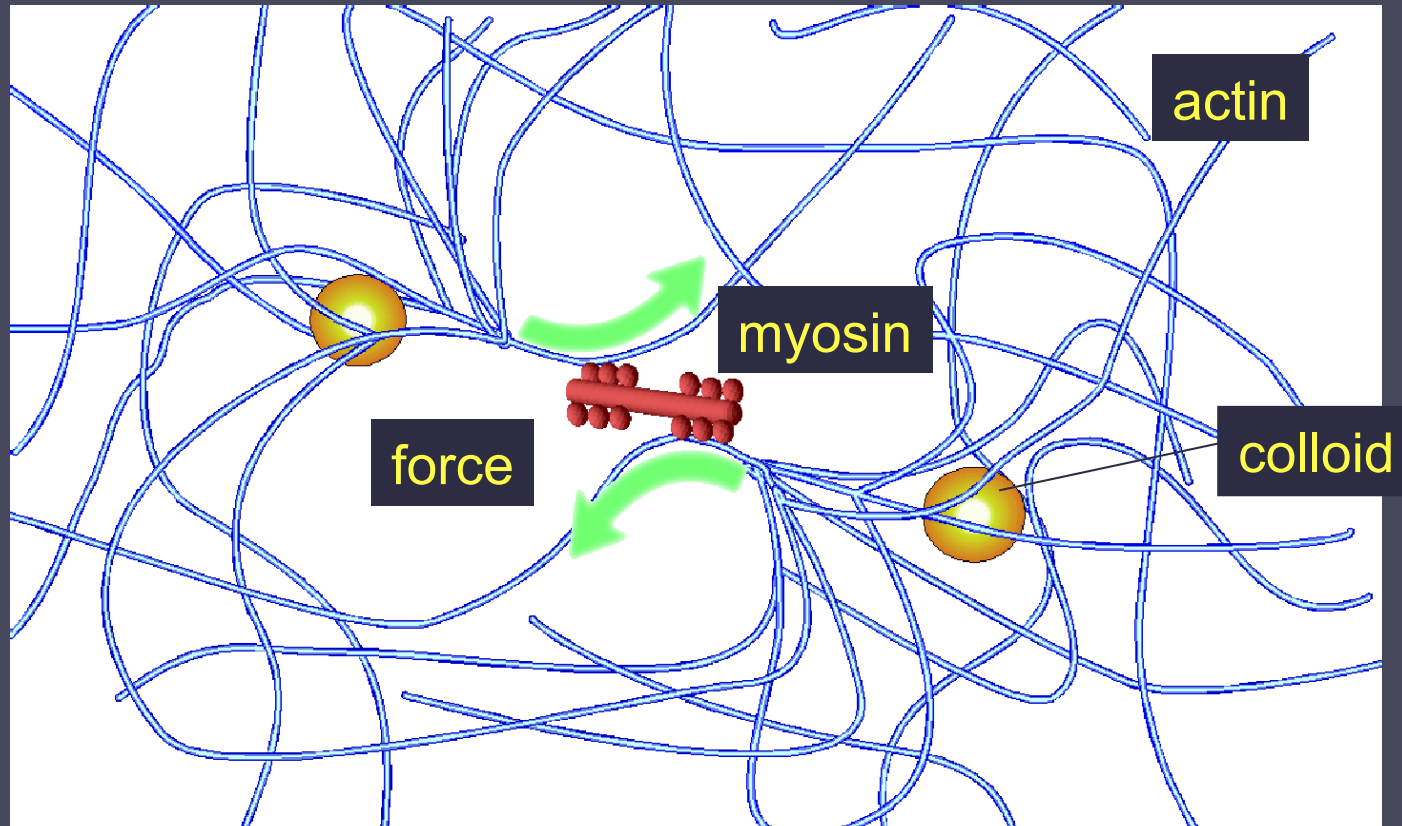
cross-linker: biotin + streptavidin

Mizuno, Tardin, Schmidt, MacKintosh (2007), Science 315, 370



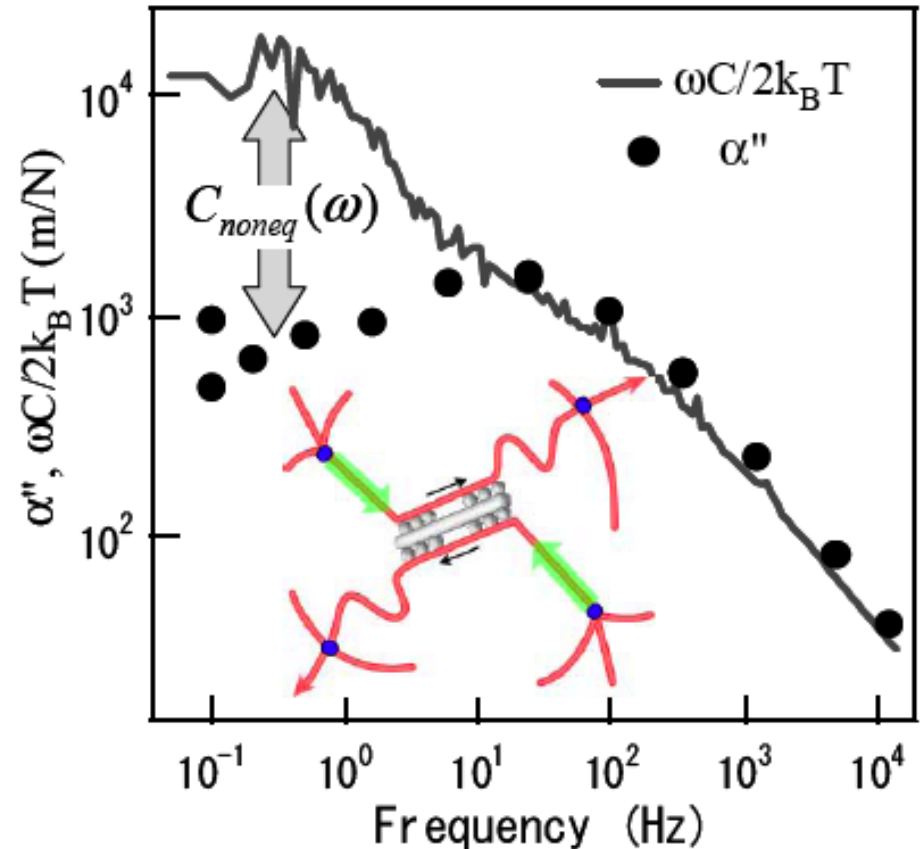
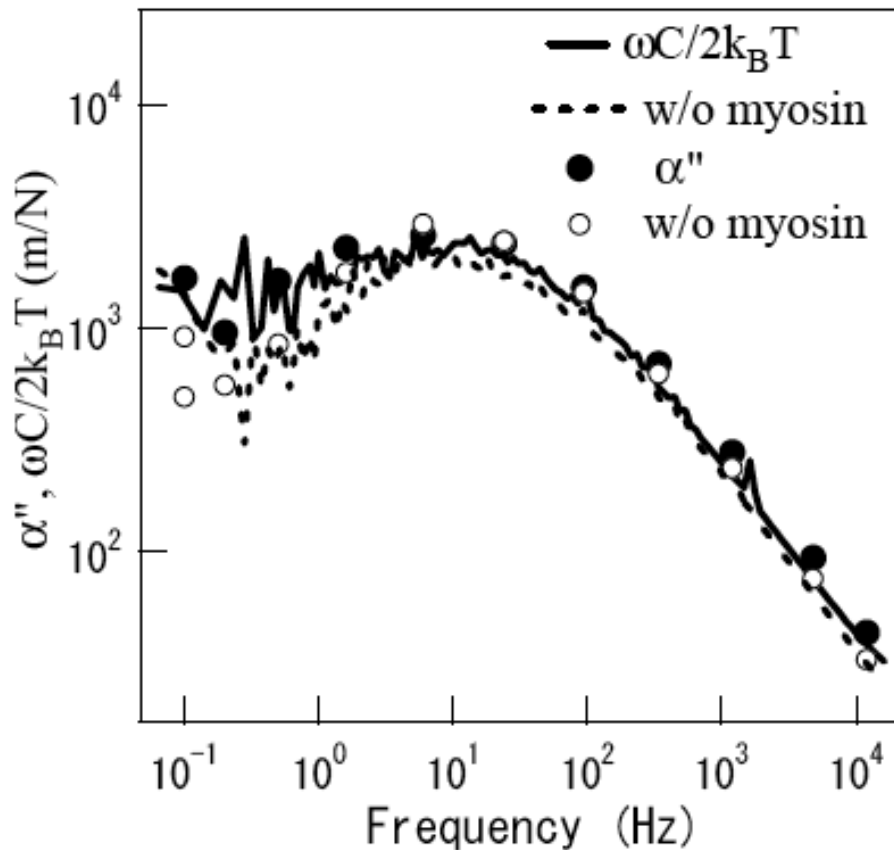


# microrheology in active cytoskeletal networks



# complex response function, imaginary part

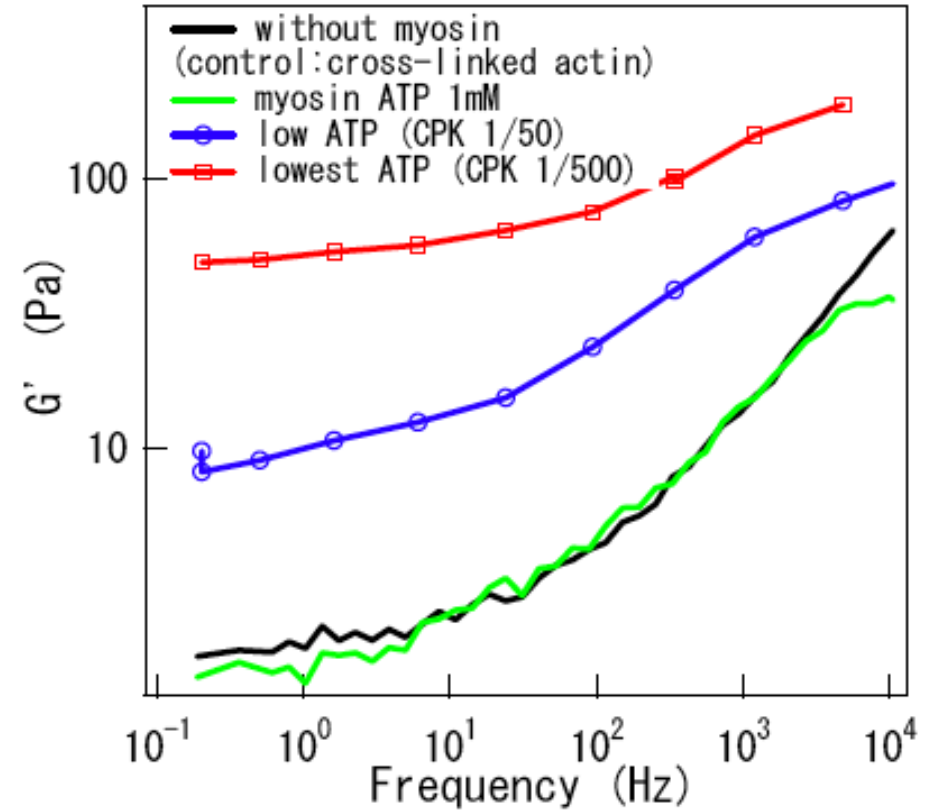
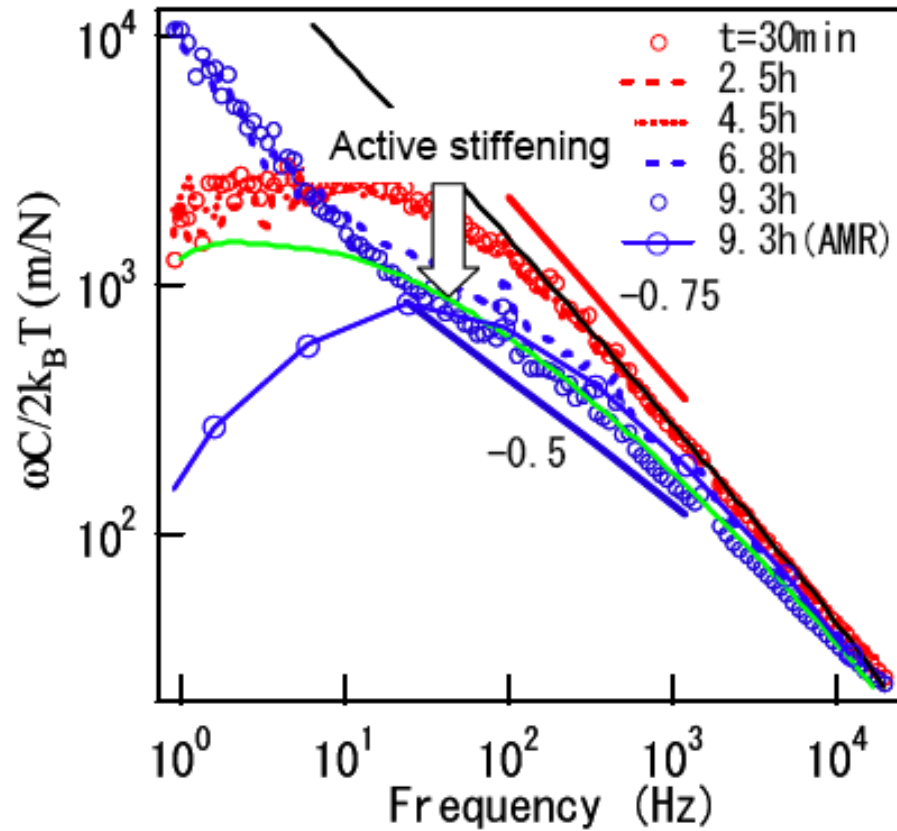
active MR (dots) and passive MR (lines)



fluctuation-dissipation theorem:

$$\langle x_\omega^2 \rangle = \frac{4k_B T \alpha''(\omega)}{\omega}$$

# active stiffening with increasing motor-generated tension



$$\alpha = \frac{5}{2\pi a \rho l_c} \sum_q \frac{2k_B T q^4}{\omega_q \zeta^2 (2\omega_q - i\omega)}$$

$$\omega_q = (\sigma q^2 + \kappa q^4) / \zeta$$

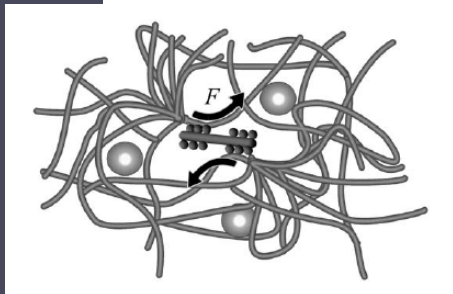
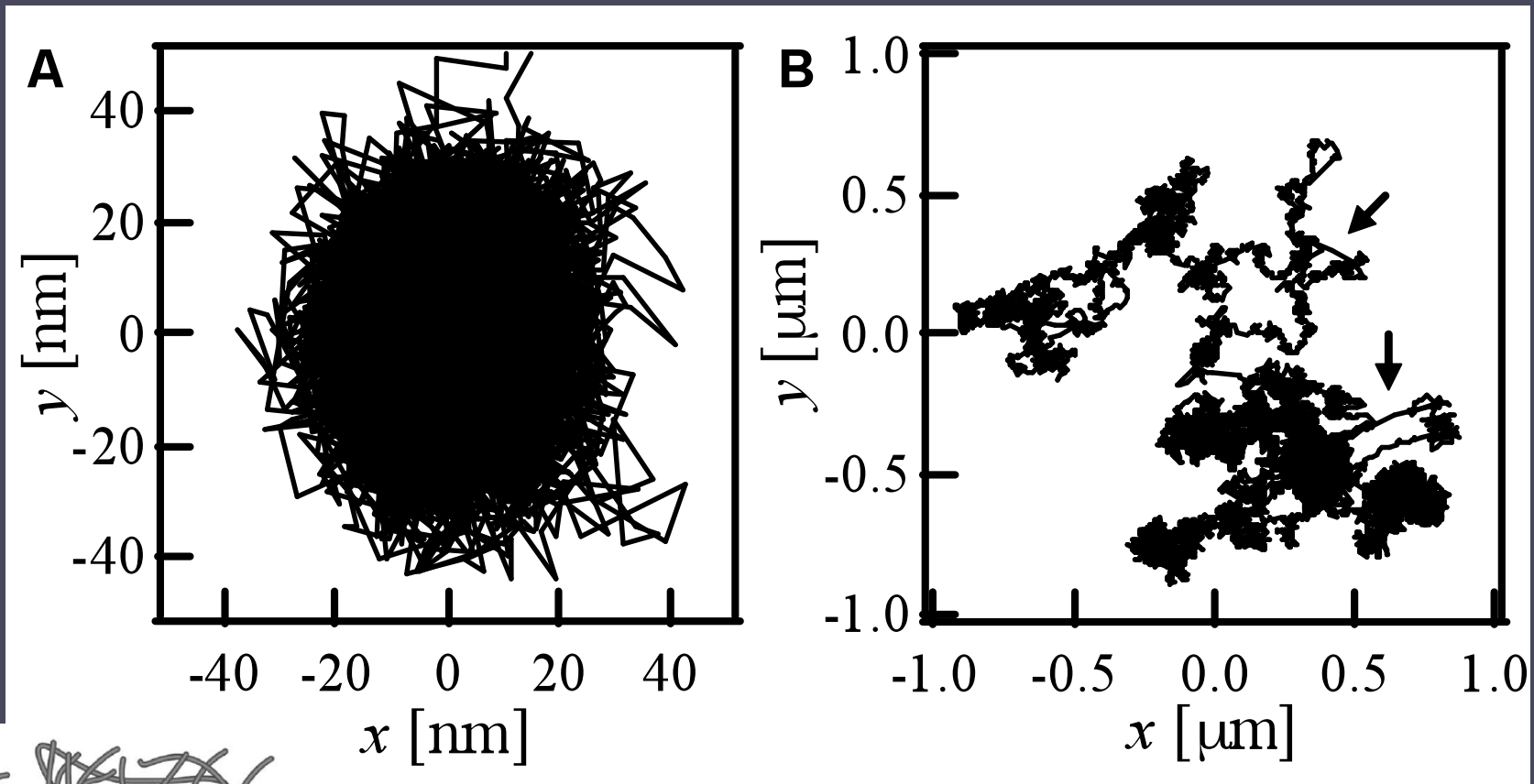
$$l_c = 2.6 \mu\text{m}, \quad \sigma \sim 1 \text{ pN}$$



# model network: particle trajectories, video microscopy

equilibrium: no myosin

active: with myosin

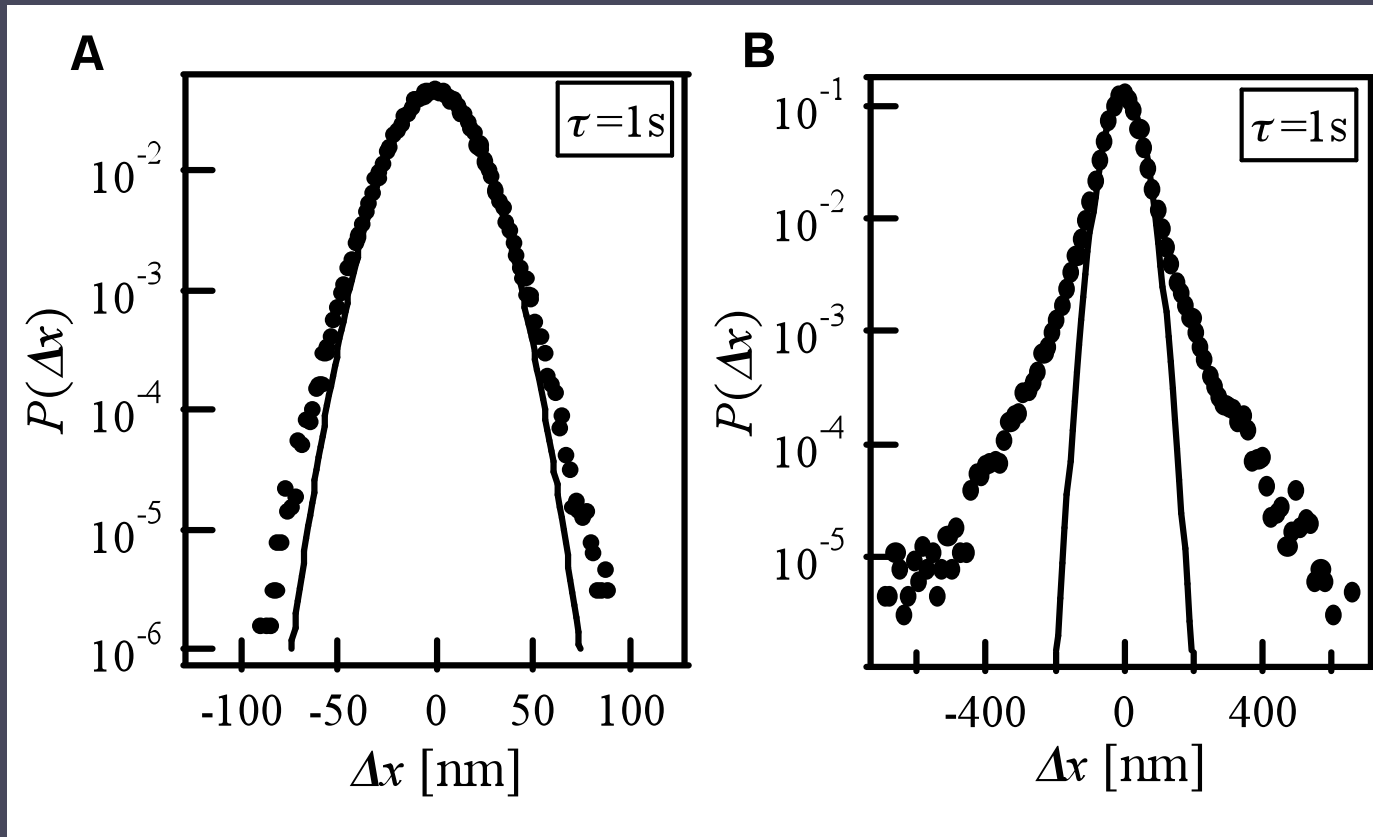


1  $\mu\text{m}$  beads, actin + myosin + cross linker

# van Hove displacement correlation functions

equilibrium: no myosin

active: with myosin



— Gaussian

$$P(\Delta x(\tau)), \Delta x(\tau) = x(t + \tau) - x(t)$$

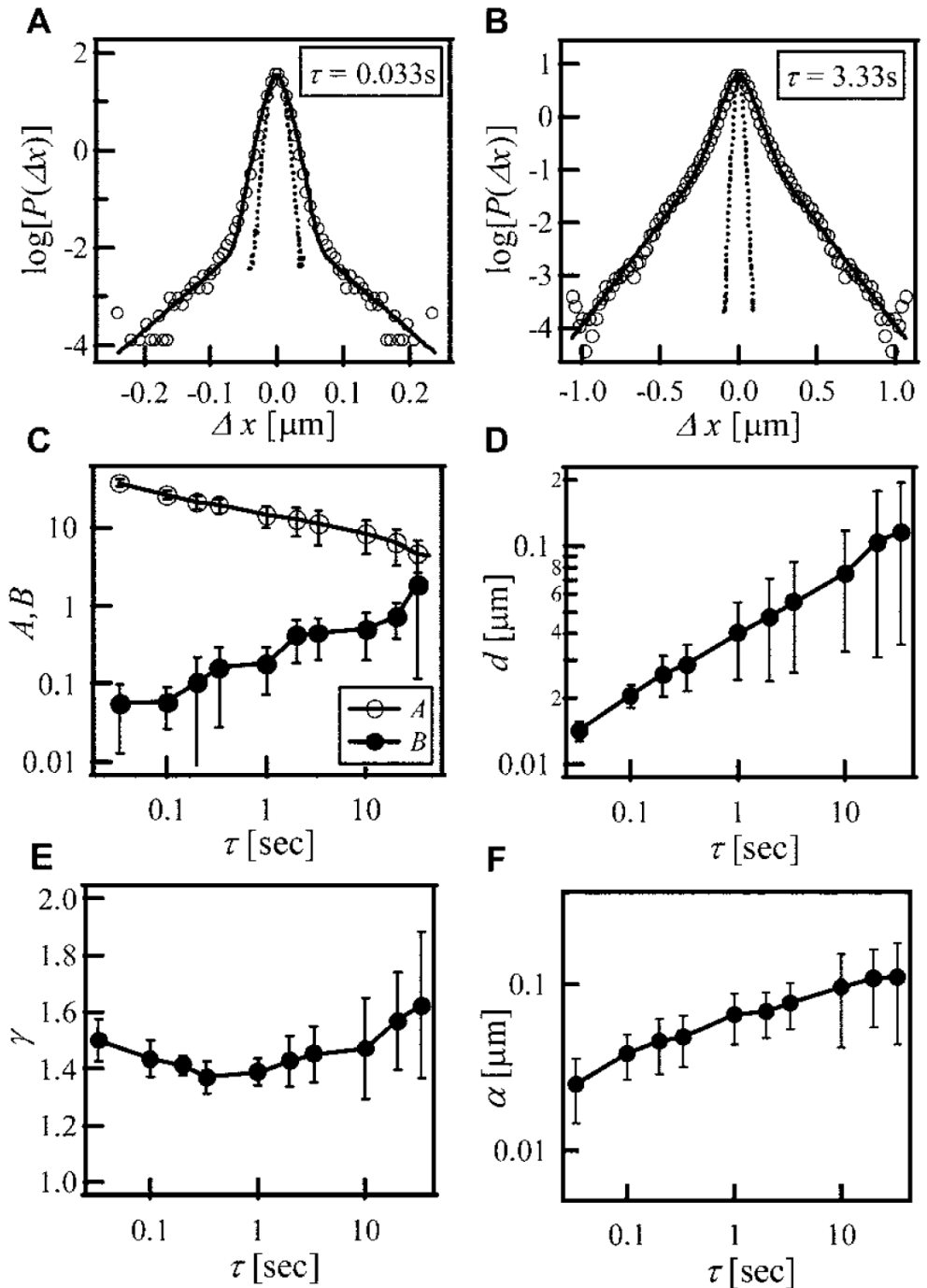
fit with sum of  
Gaussian and exponential:

$$f(x) = A \exp[-(x/d)^\gamma] + B \exp[-x/\alpha]$$

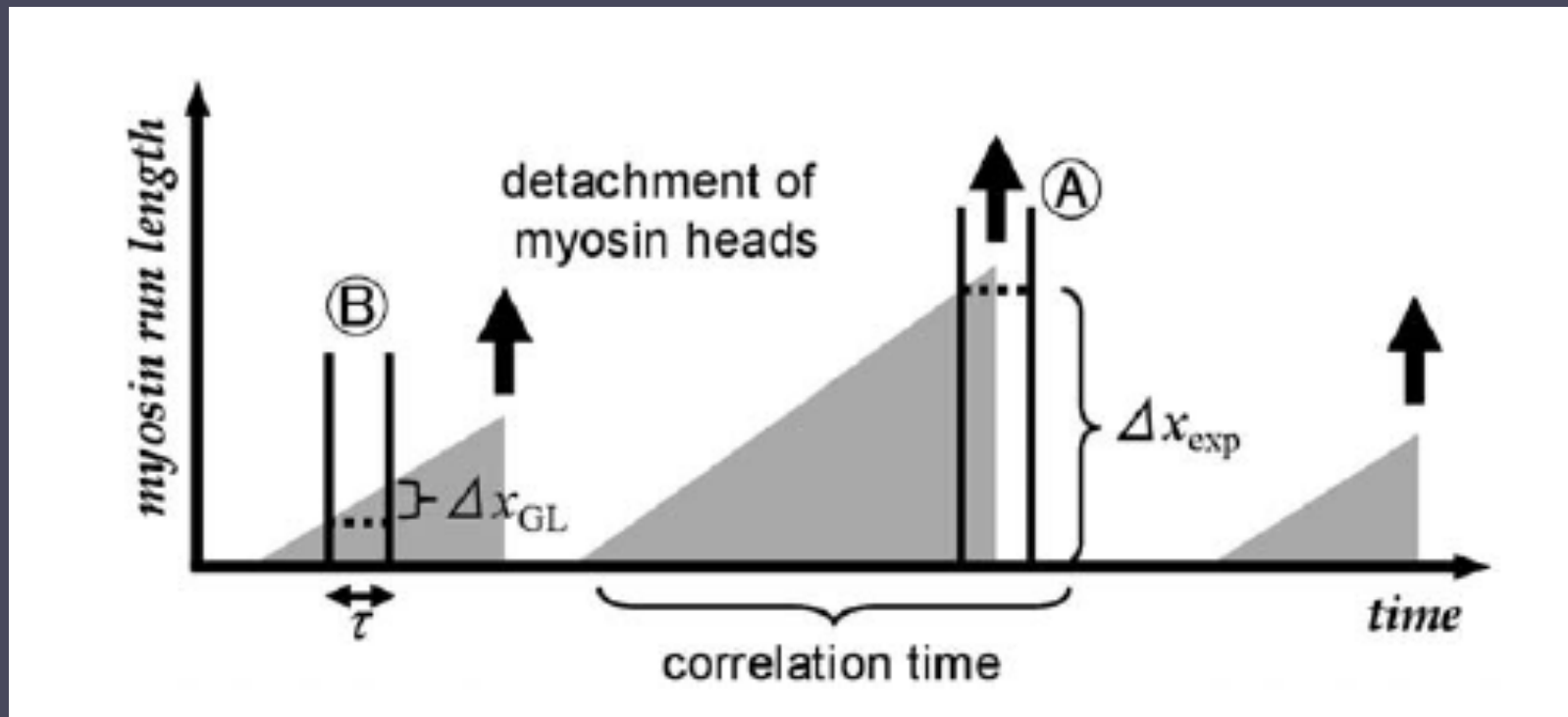
Gaussian:  
many motors far away  
↔ short distances

exponential:  
single closest motor, Poisson  
statistics

↔ long distances



# time dependence of force generation



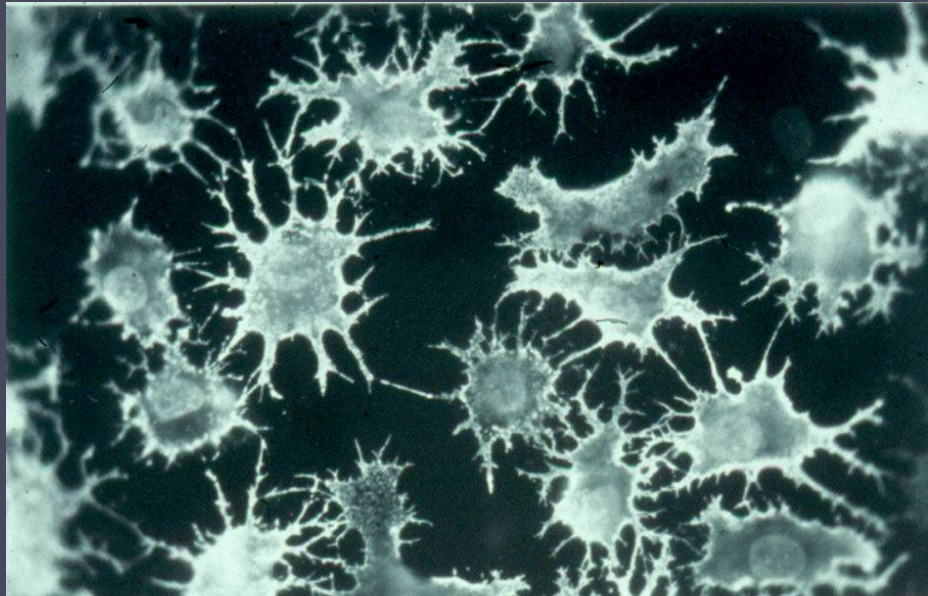
random release => Poisson process, exponential distr.

See also: Zaid, Dunkel, Yeomans: Levy fluctuations and mixing in dilute suspensions of algae and bacteria, Interface online 2-2011

# cells

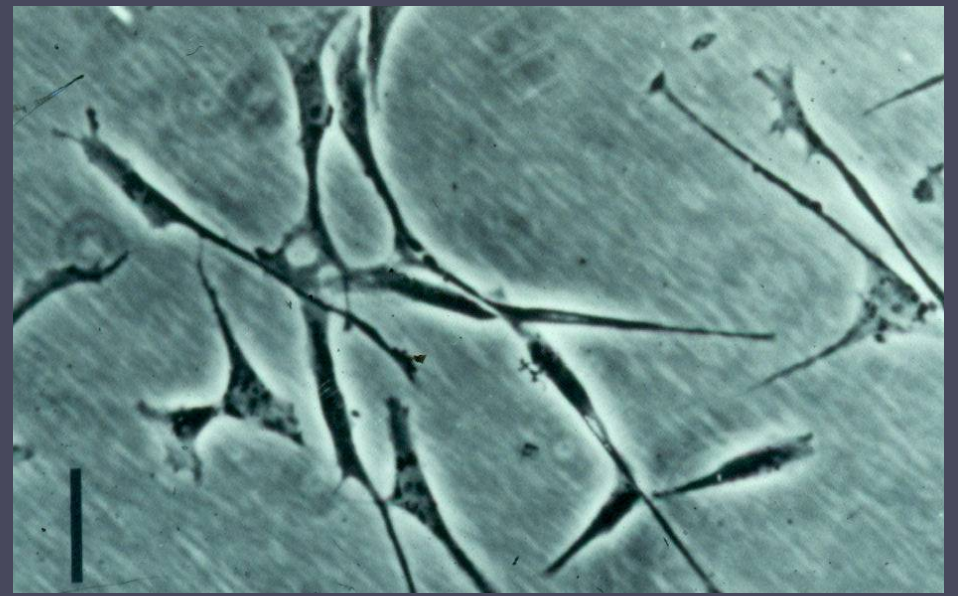
## osteocytes

- MLO-Y4
- Mechanosensory cells embedded in compact bone



## fibroblasts

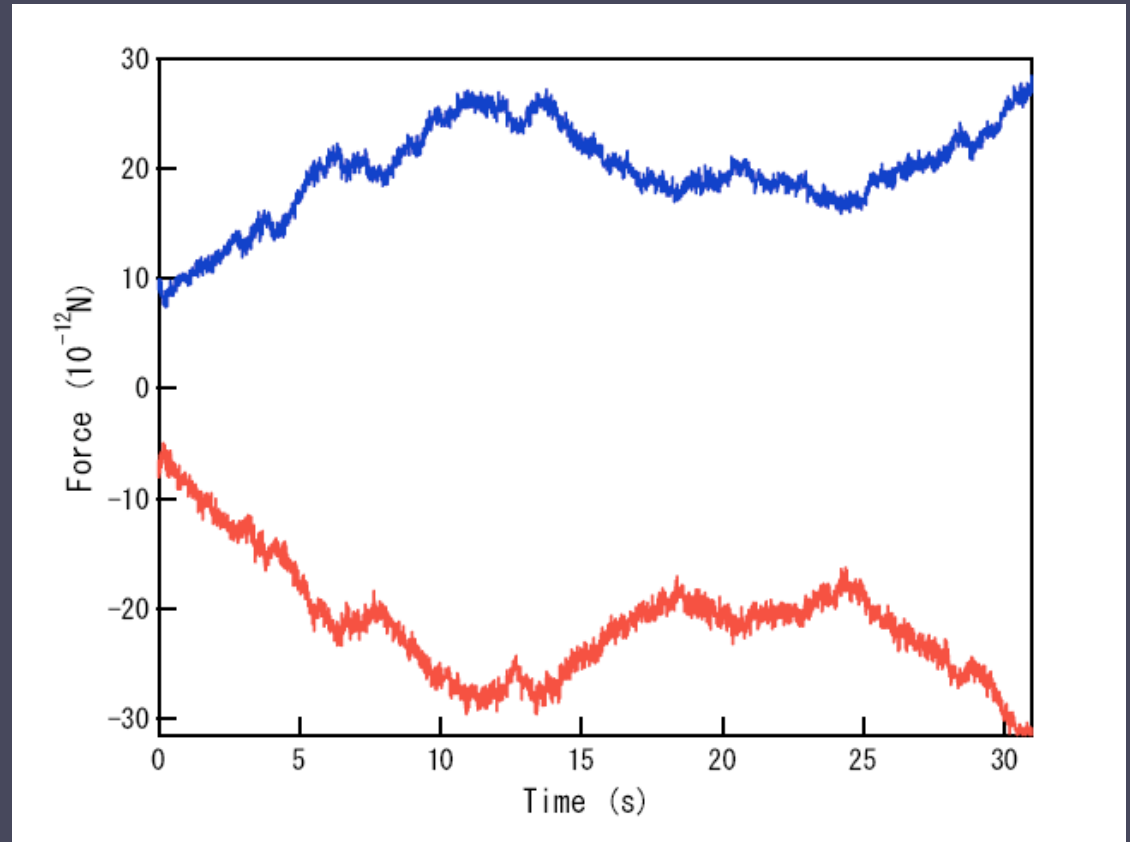
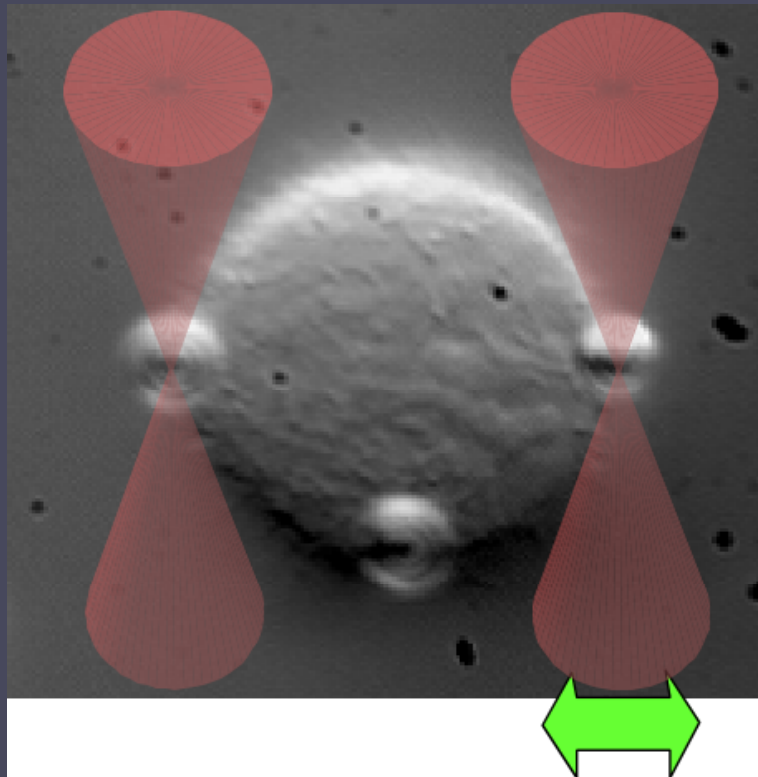
- 3T3 fibroblasts
- Mechanoresponsive cells in connective tissue



## probing cells with two optical traps

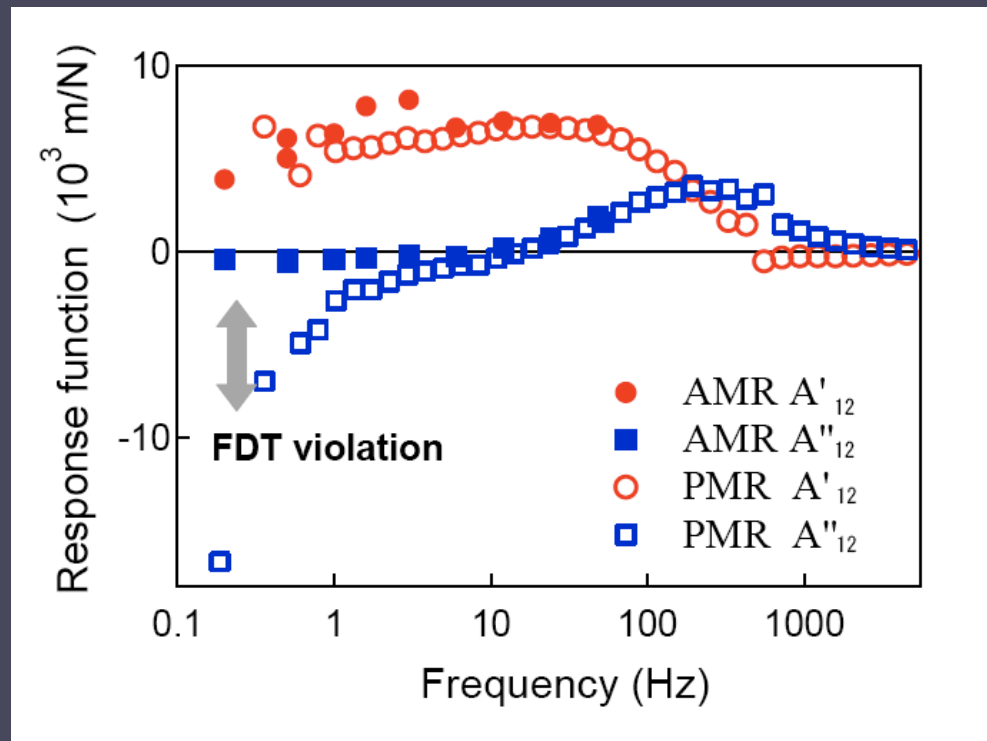


# anti-correlated fluctuations of a trapped cell

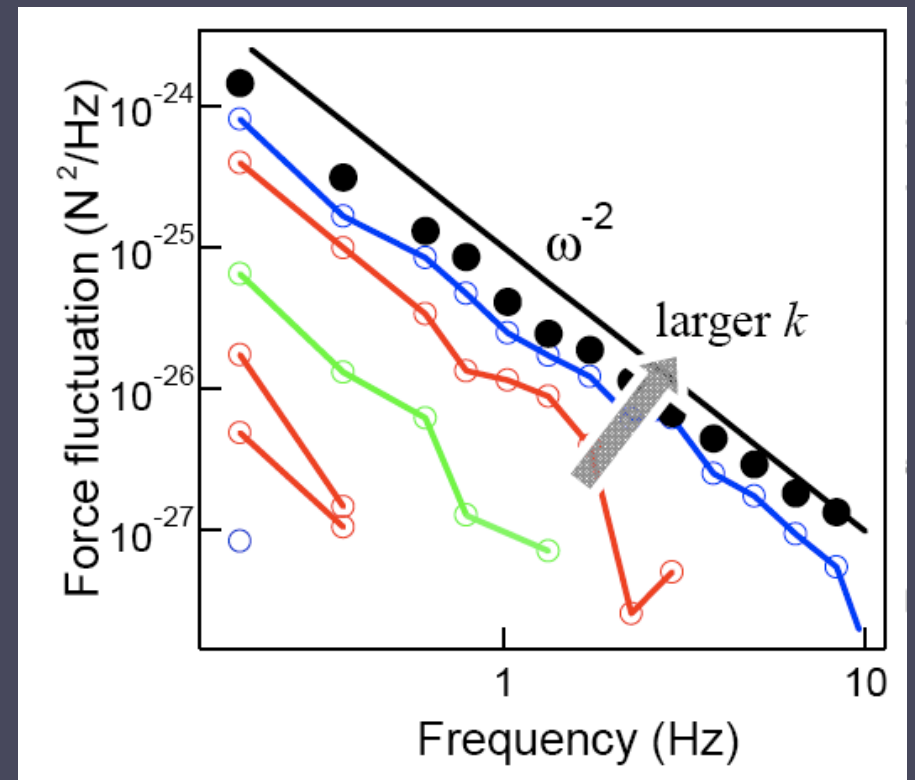


# spectrum of anti-correlated fluctuations of a trapped cell

response function



force fluctuation spectrum





# non-equilibrium part of fluctuations from active and passive measurement

from AMR



FDT

$$P_{th}(\omega) = 2k_B T A''_{ij} / \omega$$

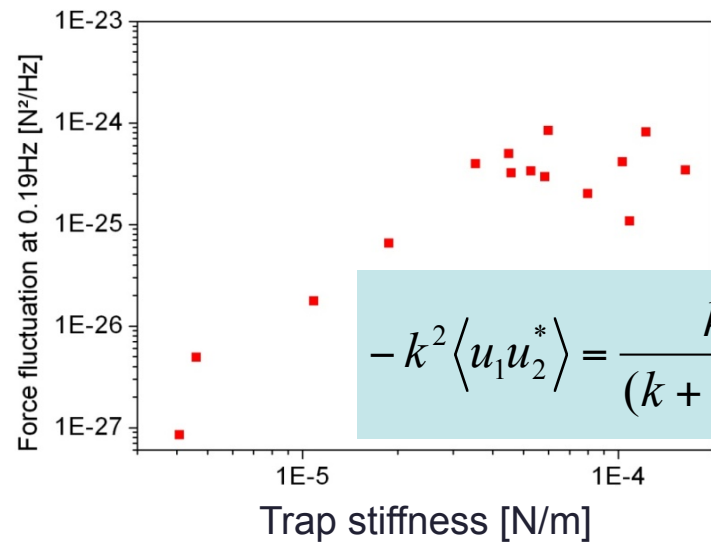
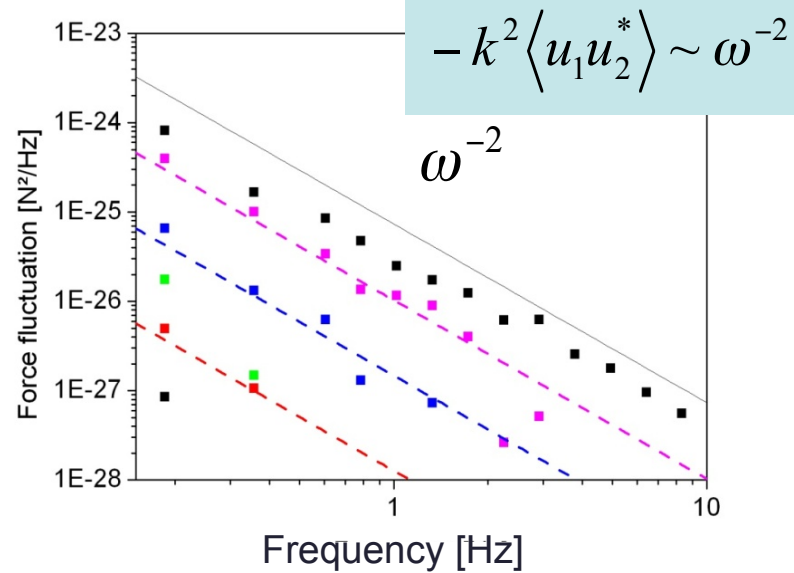
from PMR



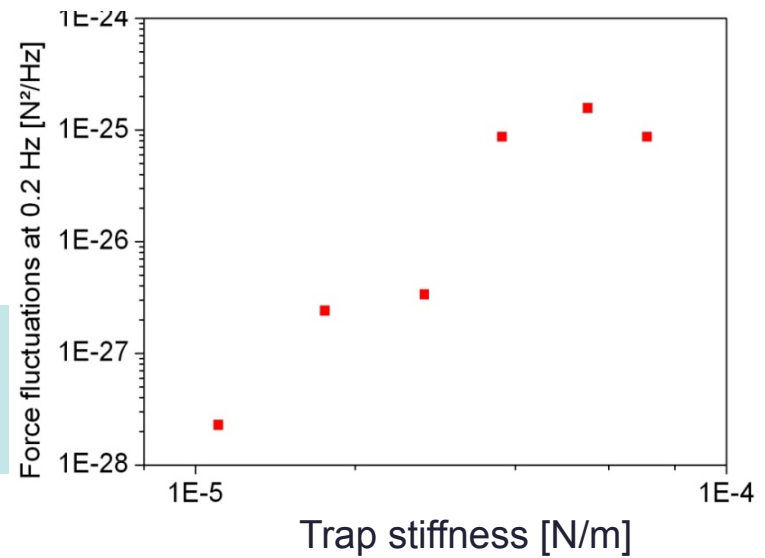
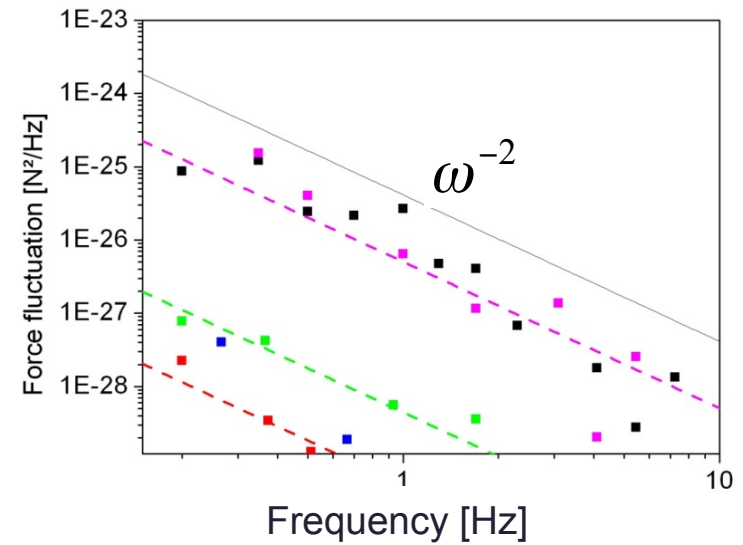
$$P_{act}(\omega) = \langle u_i u_j^* \rangle - 2k_B T A''_{ij} / \omega$$

# force fluctuations

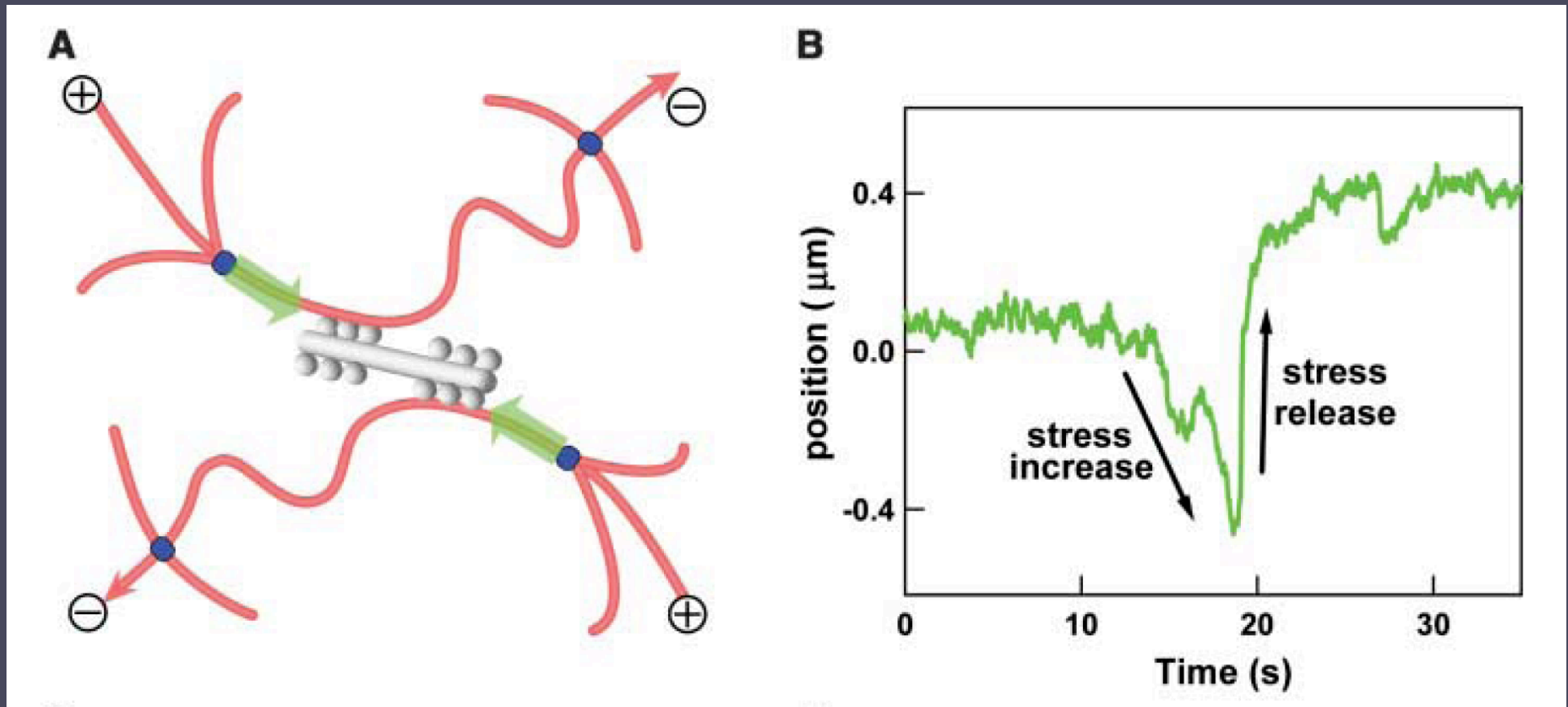
osteocytes



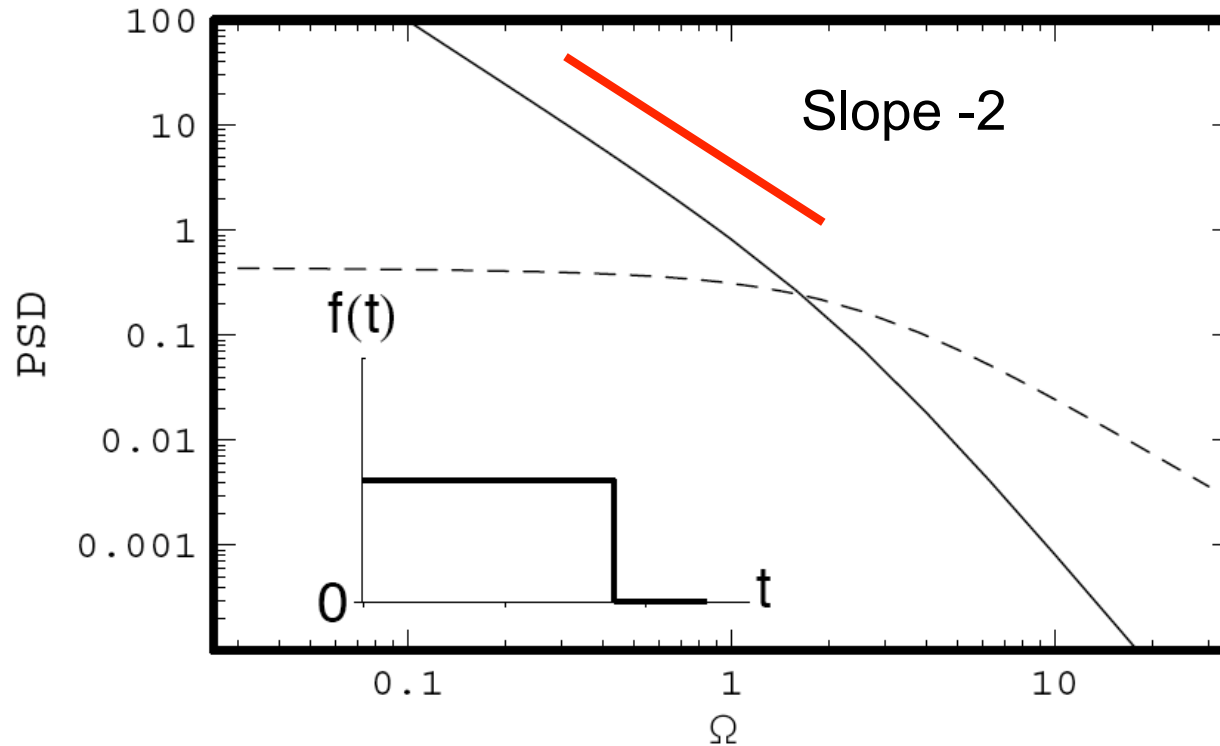
fibroblasts



motors generate contractile stress/strain:  
slow build-up, sudden (catastrophic) release

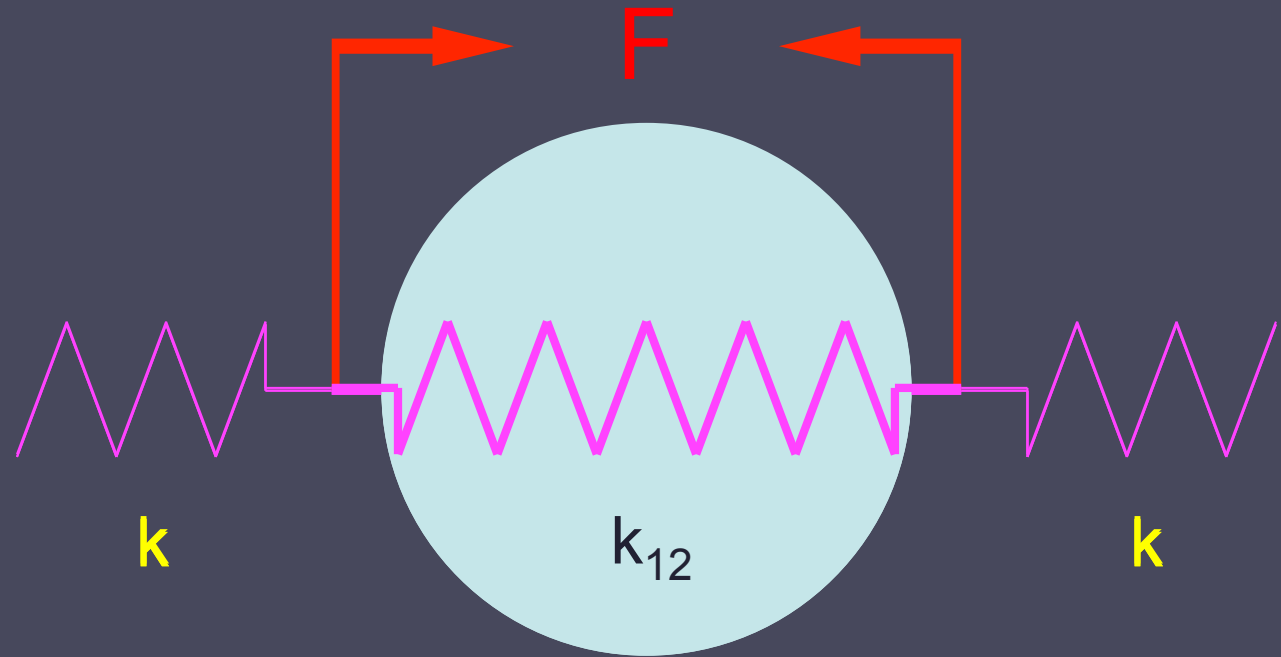
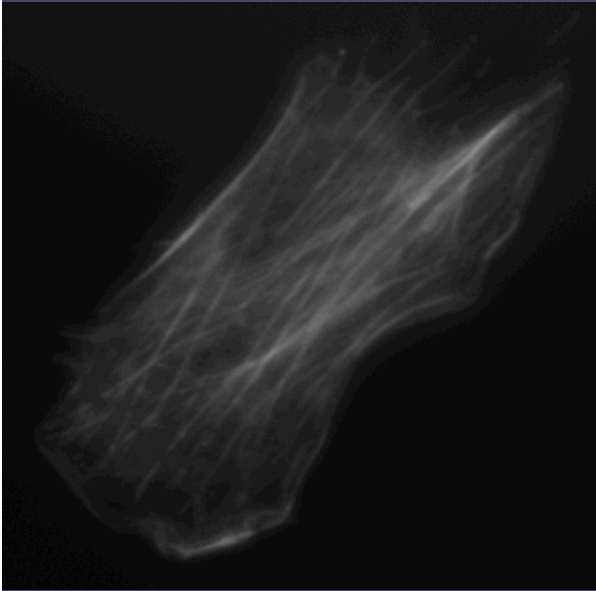


# PSD slope due to active fluctuations



$$\langle |u(\omega)|^2 \rangle \propto \langle |f(\omega)|^2 \rangle / |G(\omega)|^2 \propto |\omega G|^{-2}$$

# from displacement fluctuations in traps to force fluctuations

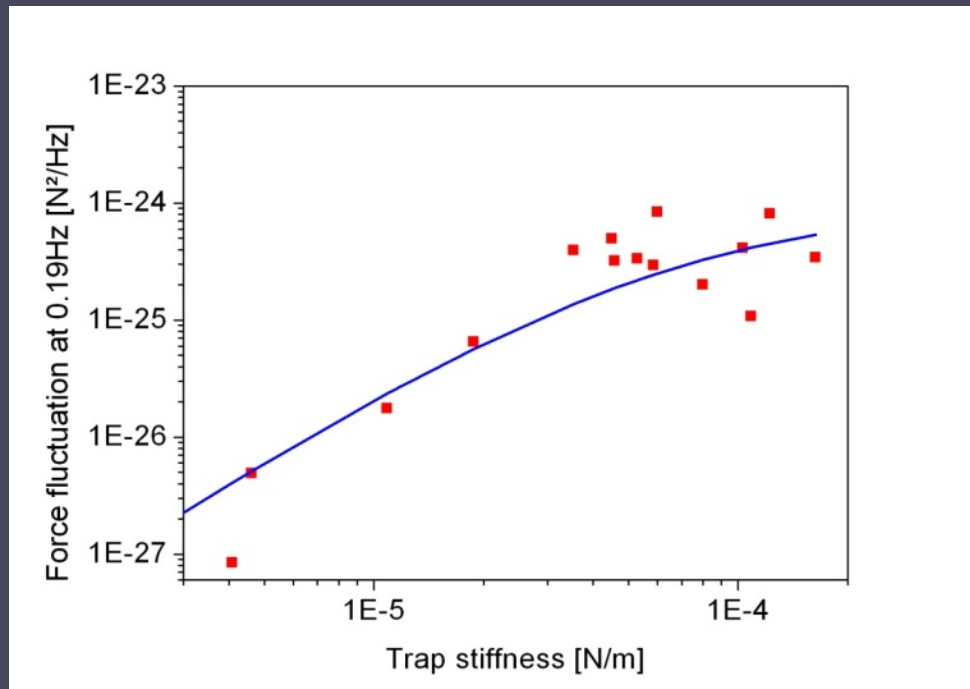


$$u_1 = -u_2 = -F / (k + 2k_{12})$$

$$-k^2 \langle u_1 u_2^* \rangle = \frac{k^2}{(k + 2k_{12})^2} \langle FF^* \rangle$$

# spring model

- internally generated forces deform cell and displace particles



- fitting  $k_{12}$  and  $\langle FF^* \rangle$

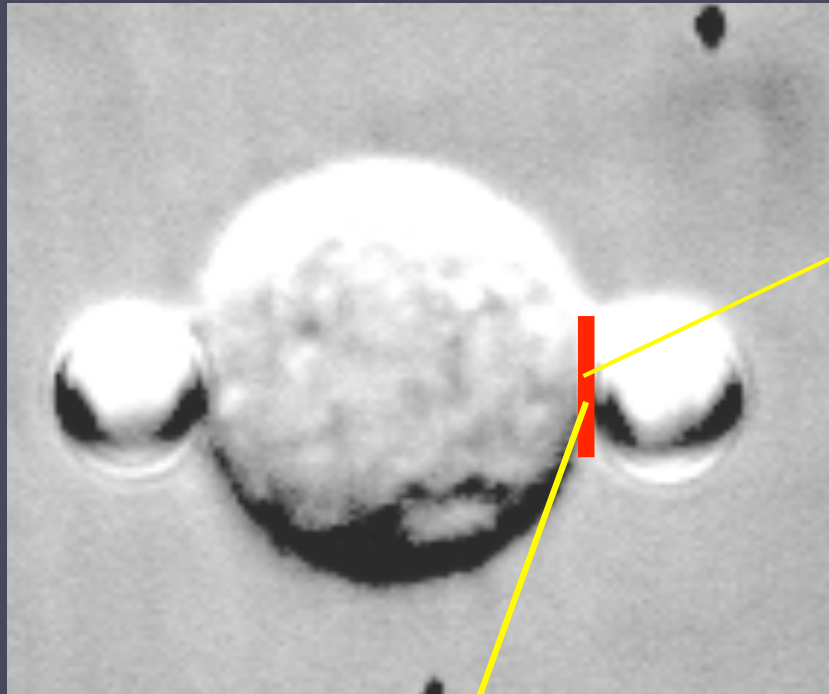
$$-k^2 \langle u_1 u_2^* \rangle = \frac{k^2}{(k + 2k_{12})^2} \langle FF^* \rangle$$

$$k_{Osteo} \approx 4 \times 10^{-5} \text{ N / m}$$

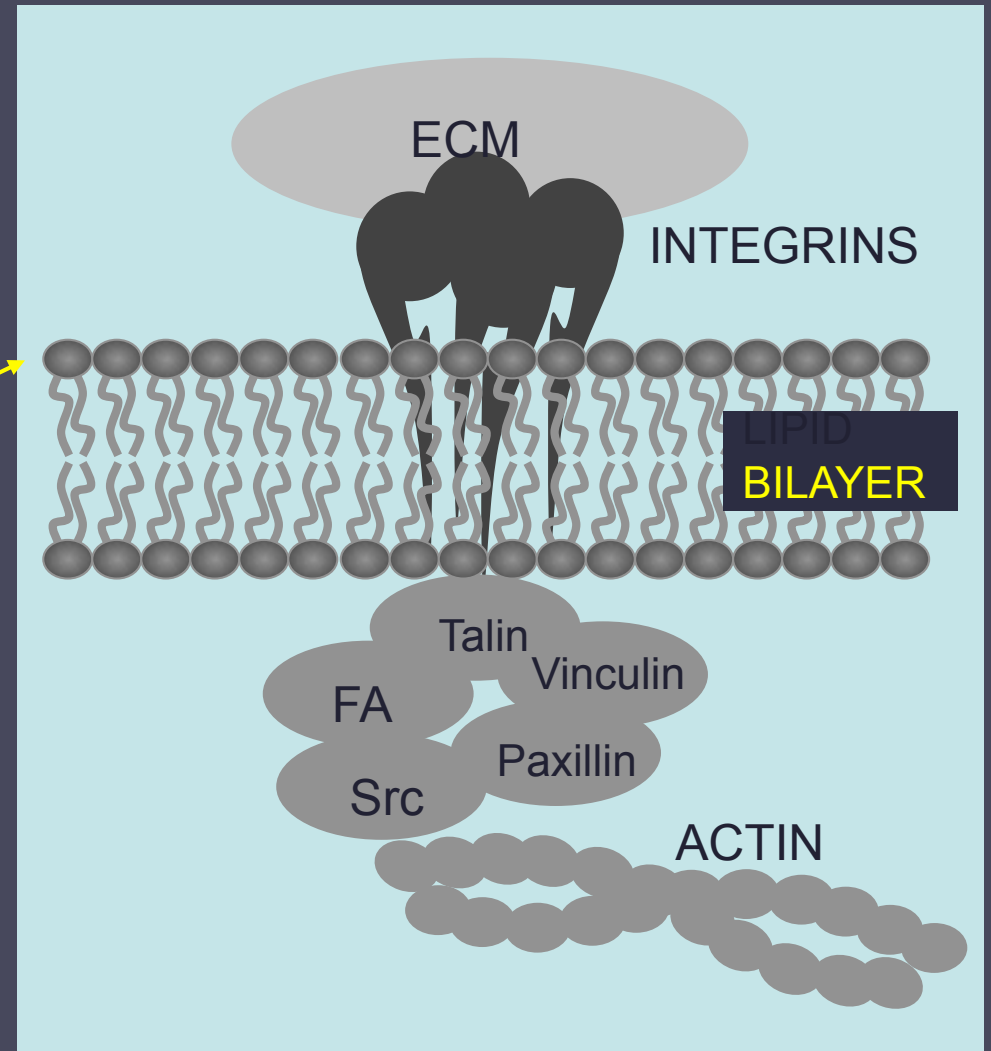
$$k_{Fibro} \approx 3 \times 10^{-5} \text{ N / m}$$

- results comparable to force-distance curve experiments

# mechanosensor : focal adhesion complex



total cellular force ??



“traction force” is applied to mechanosensor

# conclusions

- sampling of  $\mu\text{m}^3$  volumes with microrheology (bandwidth 0.1 Hz- 100kHz)
- active MR more tedious, but better data
- active and passive MR ideal to study non-equilibrium soft systems
- myosin-motor driven actin networks show clear non-equilibrium
- $\omega^{-2}$  spectrum of non-equilibrium fluctuations, stiffening by internal stress
- force fluctuations of cells can be tracked, also show  $\omega^{-2}$  spectrum
- van Hove correlation function distinguishes motors: far away/close by.

acknowledgements ->



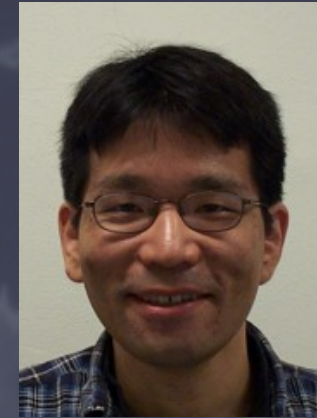
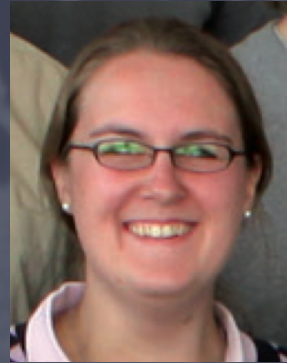


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