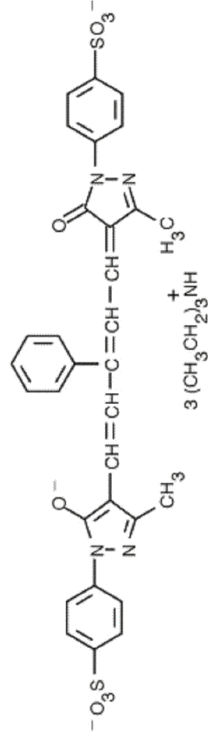
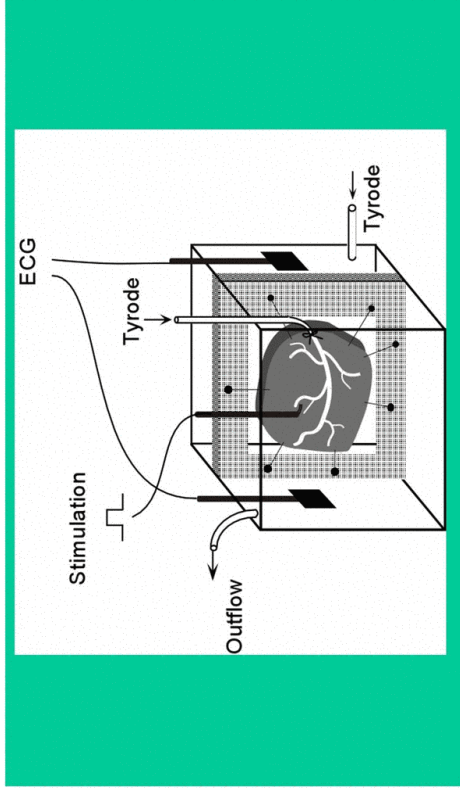


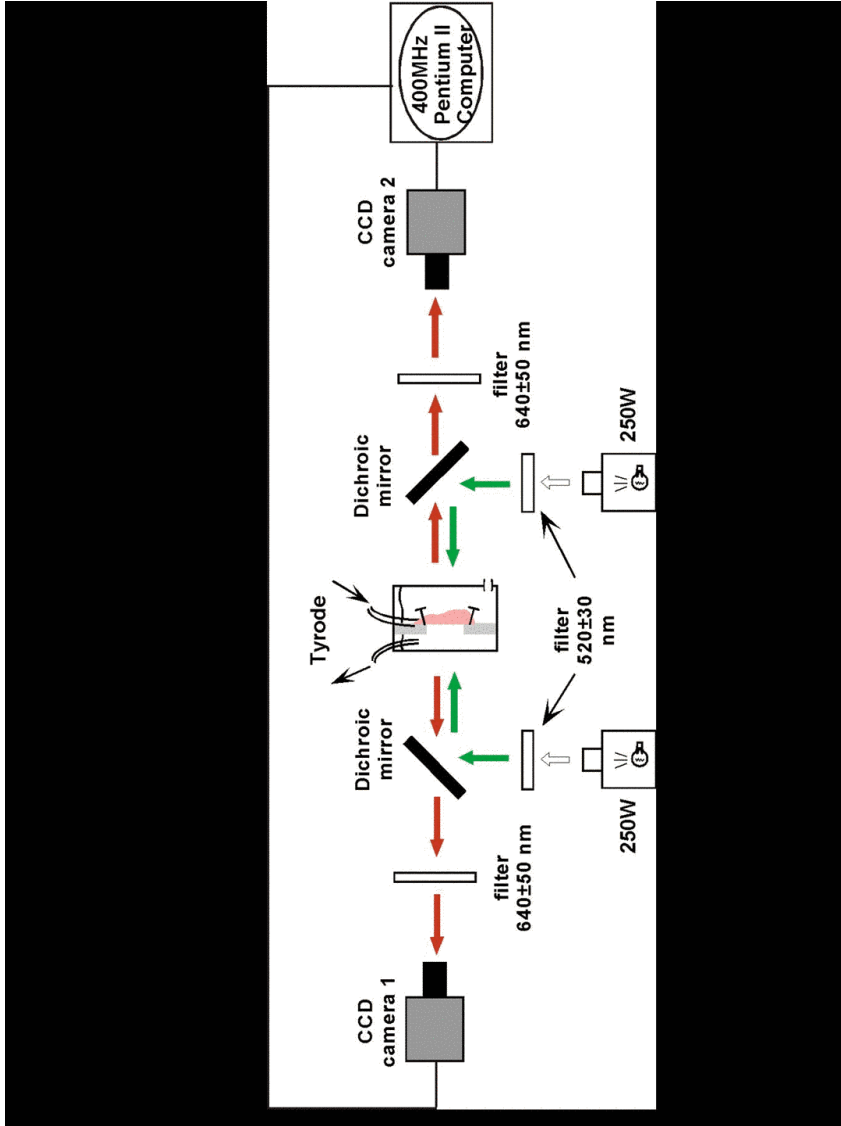
# OPTICAL MAPPING OF INTRAMURAL WAVE PROPAGATION

Arkady Pertsov  
*SUNY Upstate Medical University*

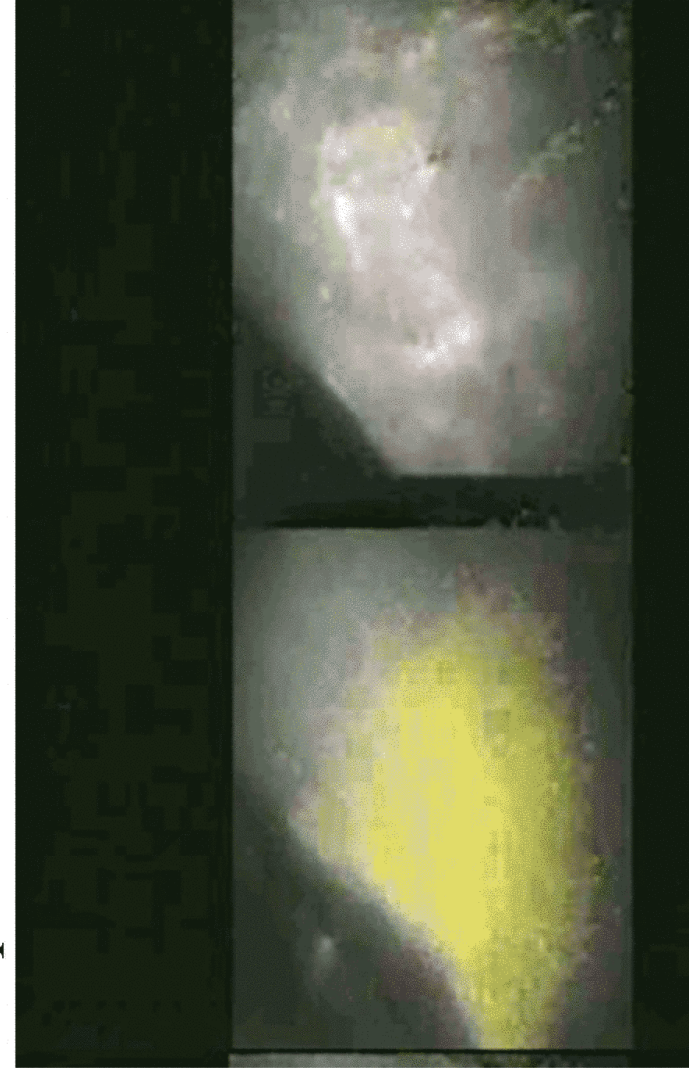


## Experimental evidence



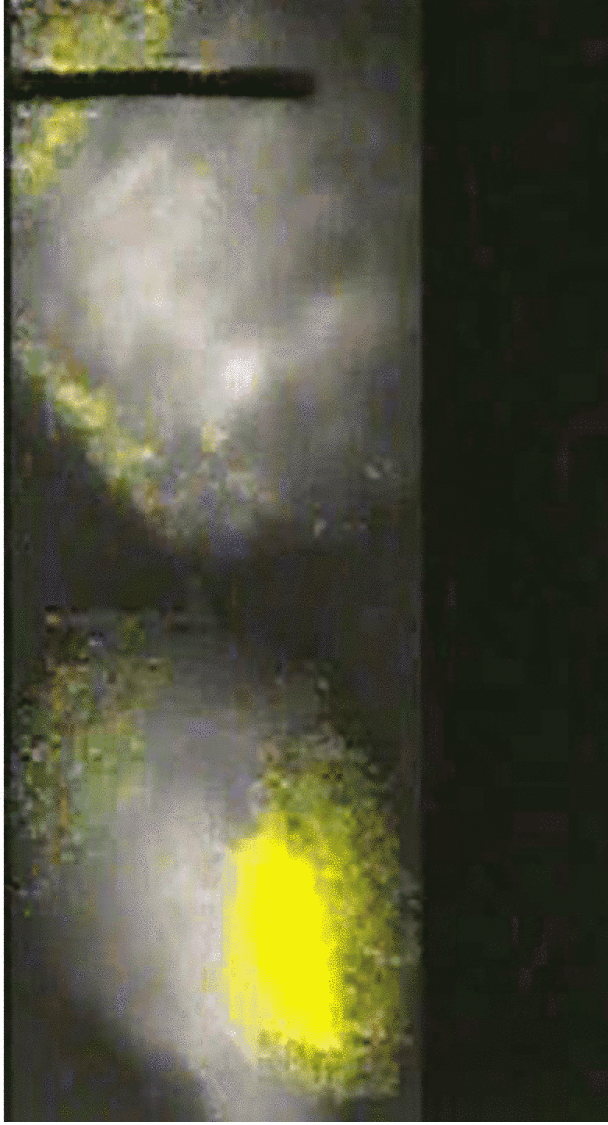


epicardium                      endocardium

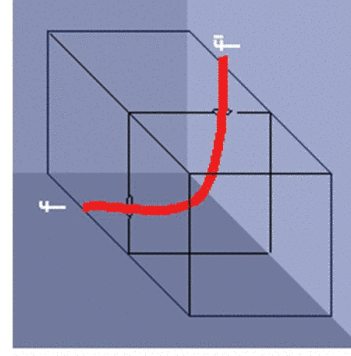
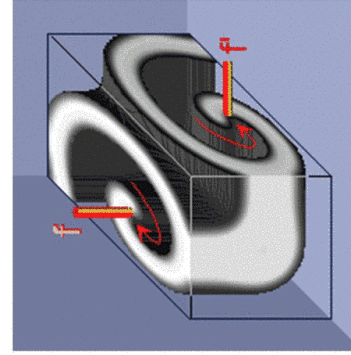


epicardium

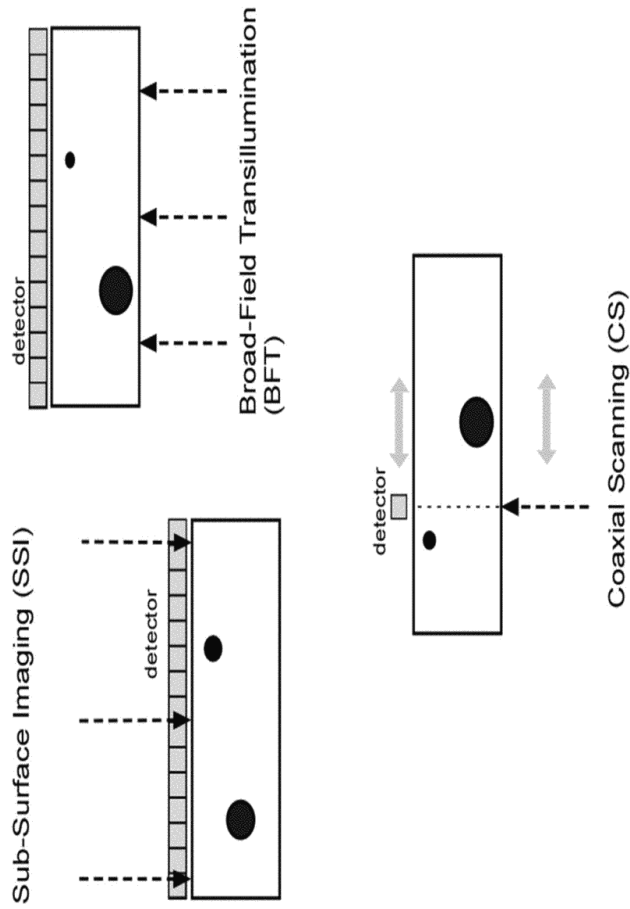
endocardium



L-shaped filament



# Optical Mapping Methods



## Hybrid model

Light absorption  
and scattering

+  
Action potential  
propagation

=  
Voltage-dependent  
Optical signal

$$D \nabla^2 \Phi(\vec{r}) - \mu_a \Phi(\vec{r}) + Q(\vec{r}) = 0$$

$$Q(\vec{r}) \sim \beta \cdot V_m(\vec{r}) \cdot \Phi_e(\vec{r})$$

## Calculating the PSF in a slab of thickness L (1)

- Analytical solution based on Dirichlet boundary conditions:

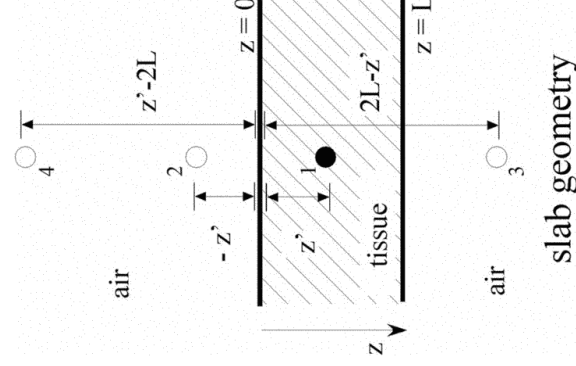
$$psf(R, z') = \frac{1}{2\pi} \int_0^\infty \frac{\xi J_0(\xi R) \sinh \eta(L - z')}{\sinh \eta L} d\xi$$

$$\eta = \sqrt{\xi^2 + \left(\frac{\mu_a}{D}\right)^2}$$

- Computationally efficient approximation based on hyperbolic functions

## Calculating PSF in a slab of thickness L (2)

Solution based on the **method of images** allows for use of different boundary conditions (Dirichlet, Robin, ...).



3D-information from the  
conventional epi-fluorescence  
mapping

$$\frac{\Delta F}{F} \sim \Delta V_m$$

$$\frac{\Delta F}{F} \sim \int_V \Delta V_m dV$$

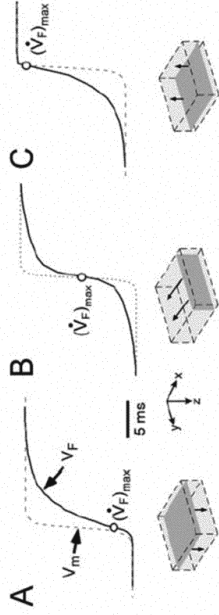


FIGURE 4 OAP upstroke morphology as a function of the direction of transmural propagation (see diagrams below each plot). (A) Propagation away from the recording surface; (B) propagation perpendicular to the recording surface; and (C) propagation toward the recording surface. Open circles on the OAP upstrokes indicate the Fenton-Karma ionic model locations of  $(V_F)_{max}$ . Electrical upstrokes are indicated by dashed lines.

Biophysical Journal 85(4) 2673-2683



Torrent-Guasp F. The cardiac muscle. Juan March Foundation. 1973.

Circulation Research August 5, 2005

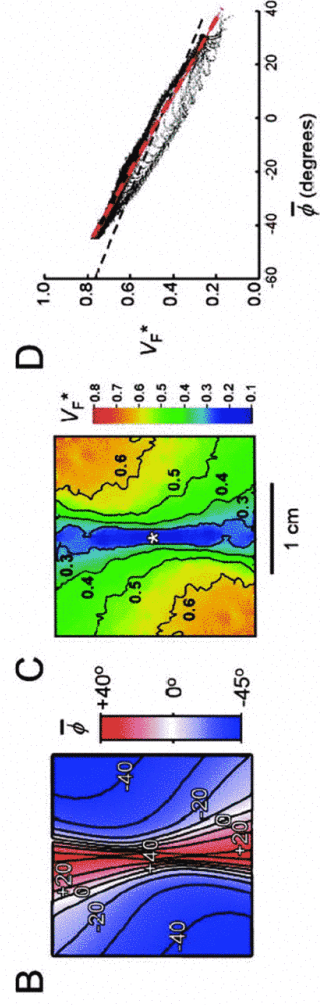
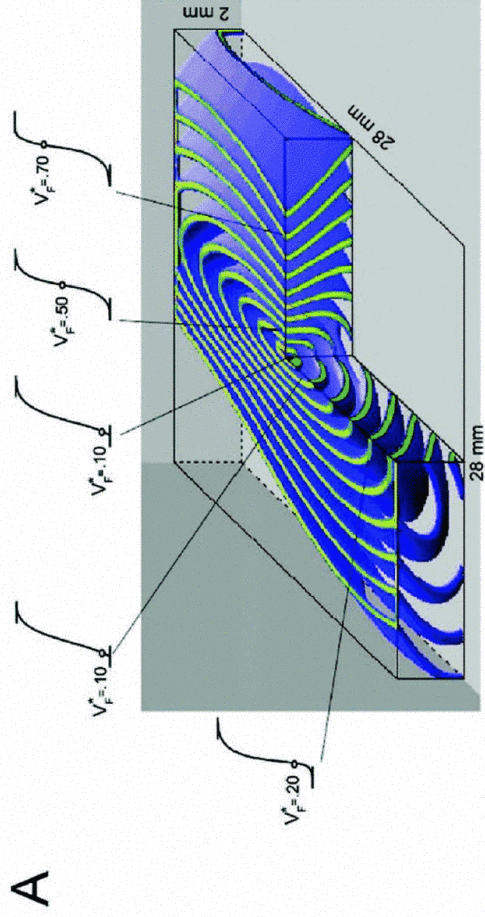
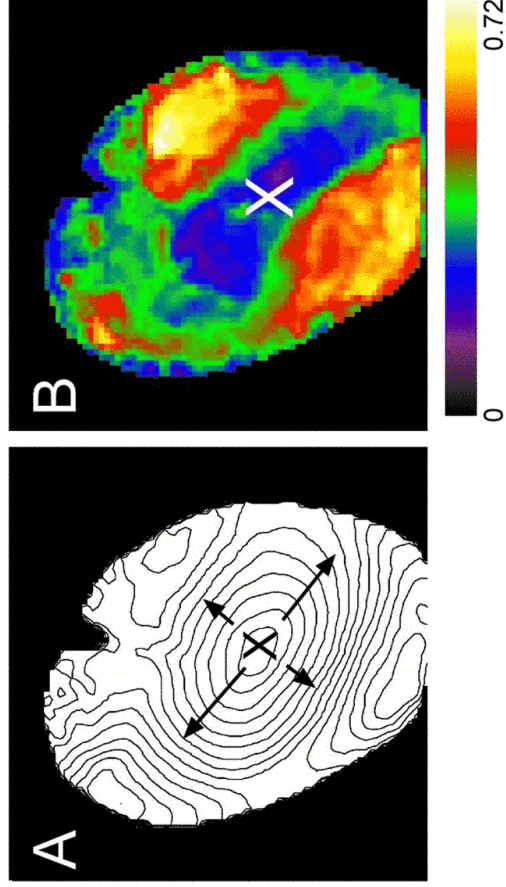


Figure 3. Subsurface wavefront orientation and spatial variation in OAP upstroke morphology after epicardial point stimulation. A, Simulated epicardial and transmural (cutaway) isochrone maps (interval, 5 ms). The corresponding OAP upstrokes at 5 different sites are shown (left and top). Open circles on the OAP upstrokes indicate the location of  $V_F^*$ . B, Map of the optically weighted mean angle,  $\bar{\phi}$ , for this simulation (isosines of  $\bar{\phi}$  are indicated). C, Corresponding  $V_F^*$  map, with isosines of  $V_F^*$  indicated. D, Plots showing the relationship between  $V_F^*$  vs  $\bar{\phi}$  at all corresponding pixels in the  $\bar{\phi}$  and  $V_F^*$  maps in B and C, respectively. The thick dashed red line is the linear regression of  $V_F^*$  vs  $\bar{\phi}$ . For comparison, the thin black dashed line shows the linear regression of  $V_F^*$  vs  $\bar{\phi}$  for steady-state waves fronts (from Figure 1C).



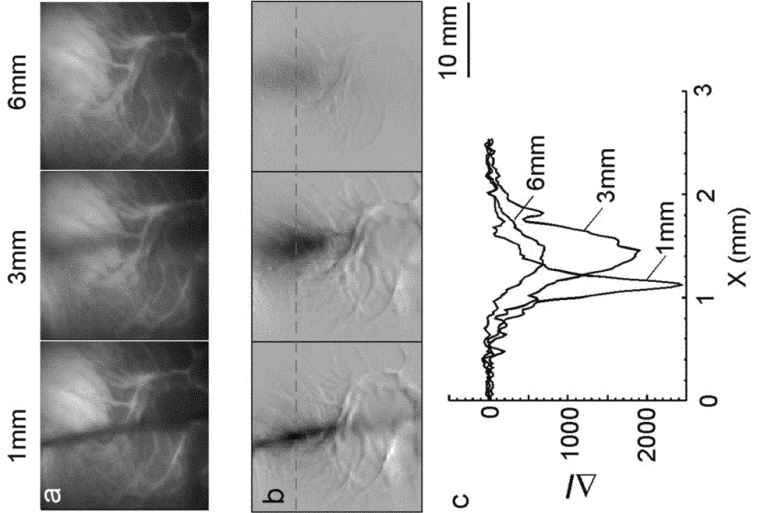
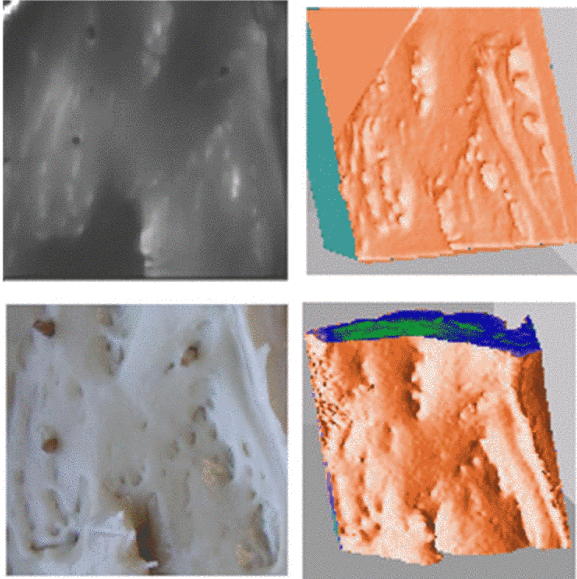
## Guinea pig LV

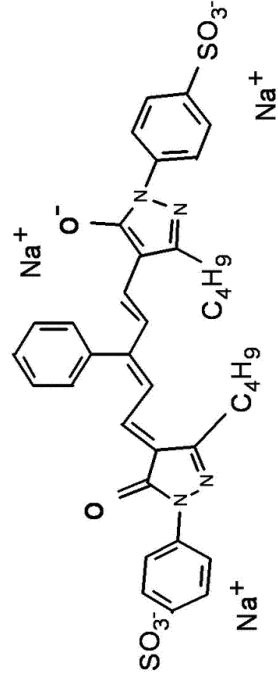


## Transillumination

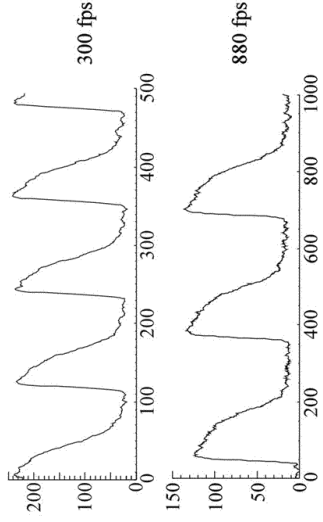
extracting information from  
deep inside myocardial wall

visualization of scroll wave filaments

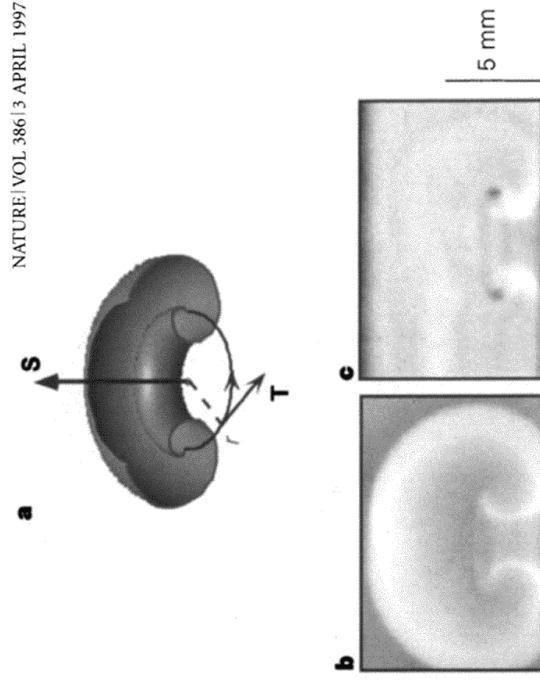




Absorption voltage-sensitive dye JPW 1150.

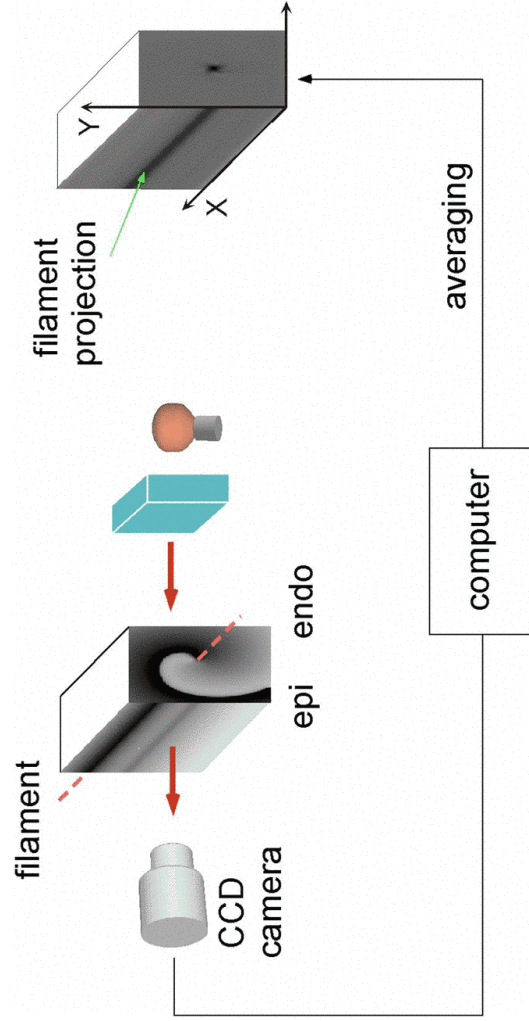


Transillumination signals obtained using JPW 1150

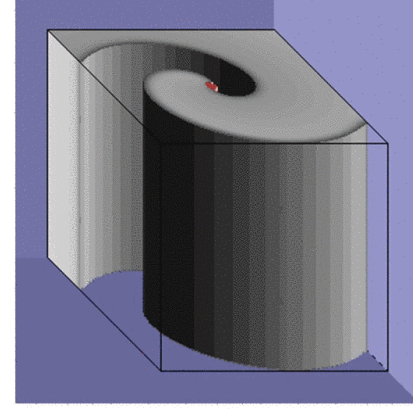


**Figure 1 a.** Schematic cross-section of a scroll ring. The dark circle of radius  $r$  in the centre is the filament of the ring, about which the wave rotates (the spiral on the right rotates clockwise). The unit tangent vector  $\mathbf{T}$  is in the direction of the local

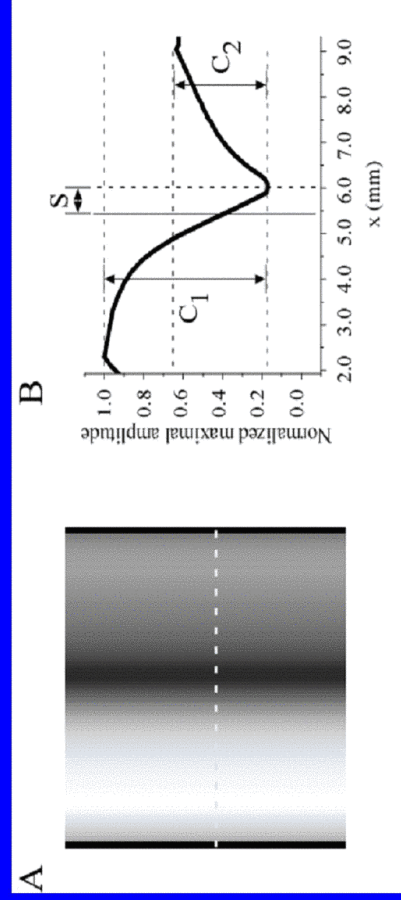
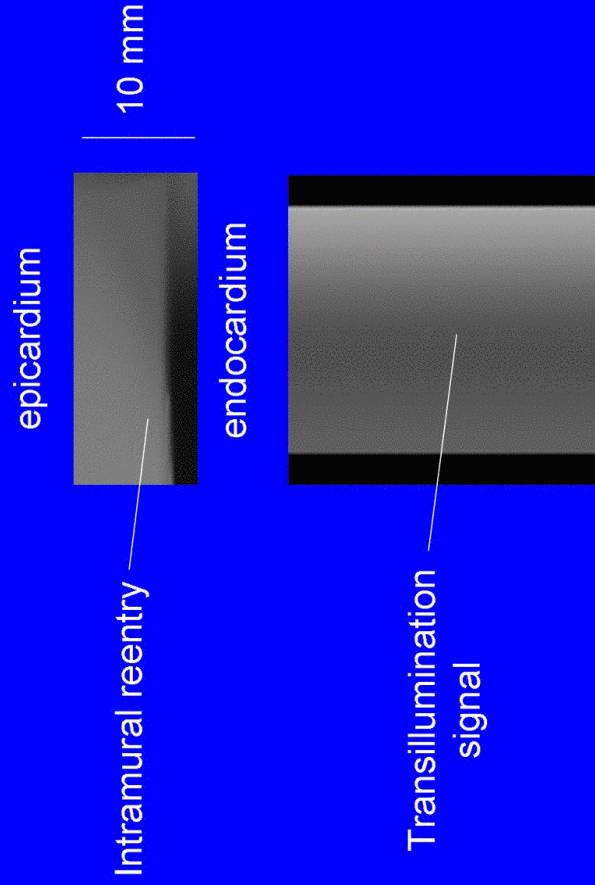
Michael Vinson<sup>†</sup>, Sergey Mironov<sup>†</sup>, Scott Mulvey<sup>\*</sup> & Arkady Pertsov<sup>\*</sup>

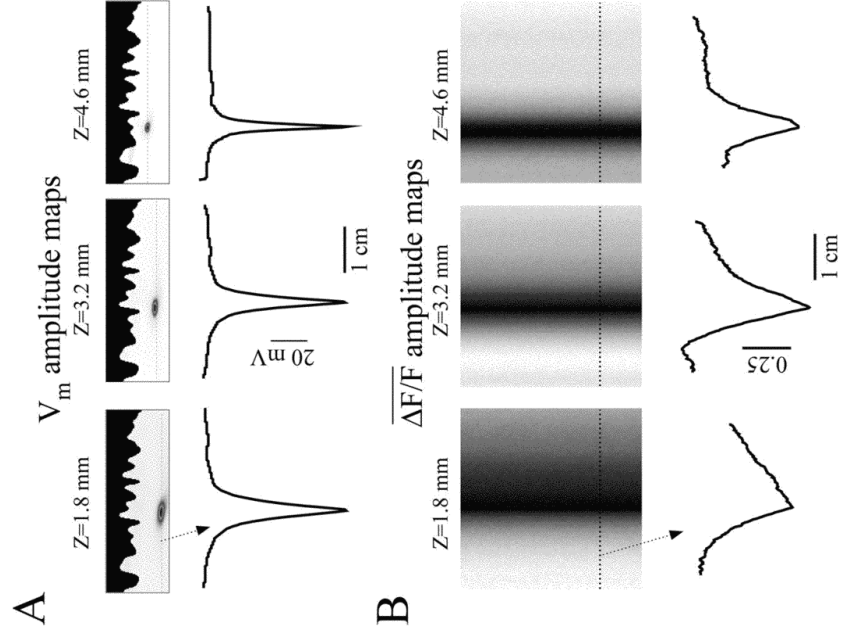


## Intramural scroll wave

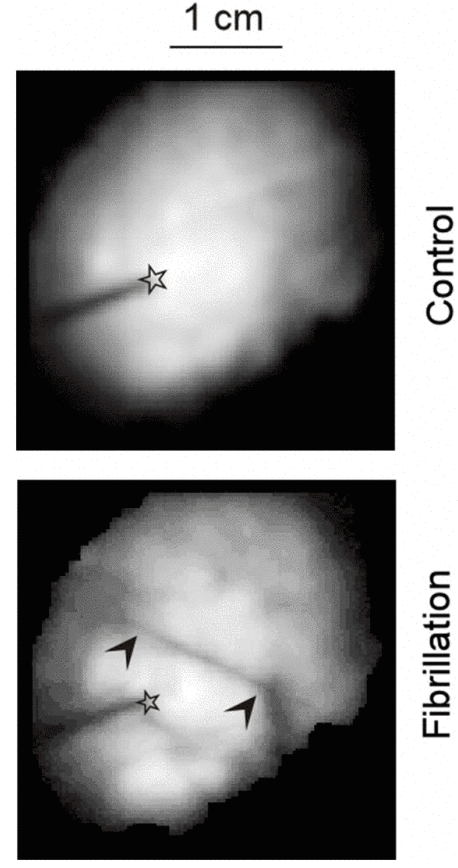


# Hybrid model (LRd + optical diffusion)



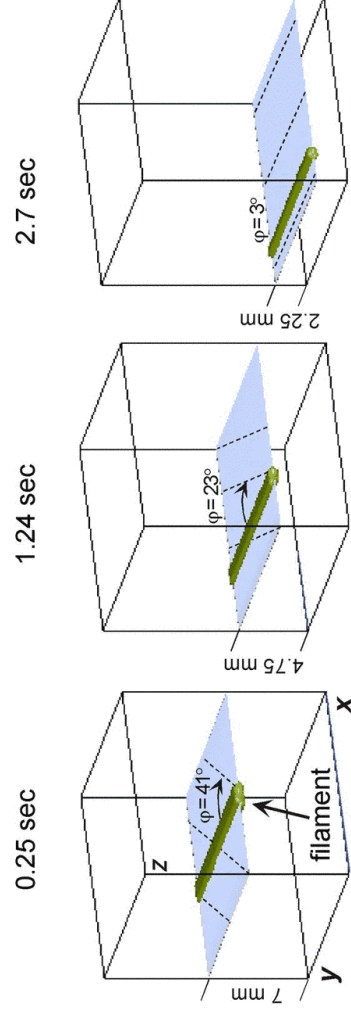


**Filament reconstruction  
(sheep, RH-155 staining)**

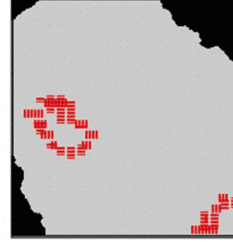
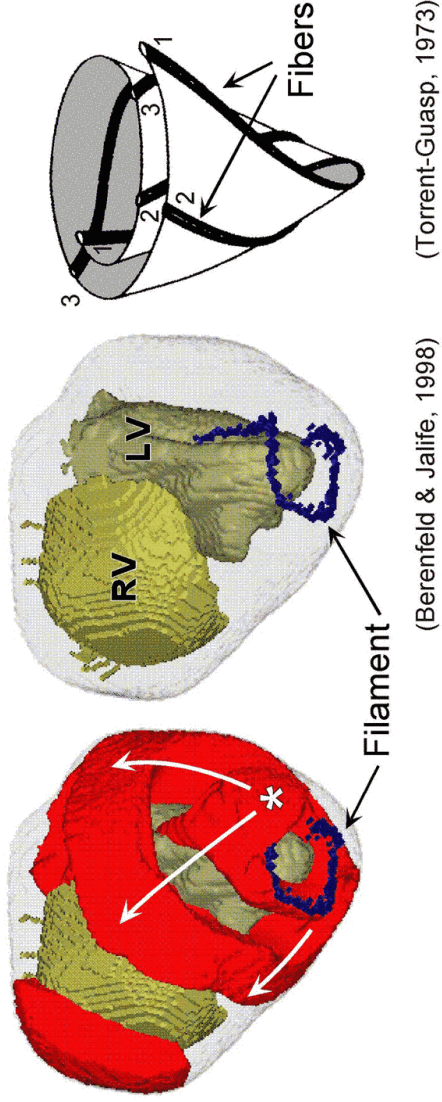


- Filaments tend to stabilize along muscle fibers (effect is model independent)

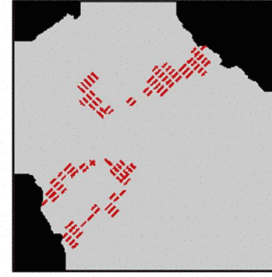
### Coupling Mediated Alignment



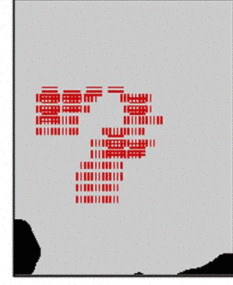
# Scroll Wave in Whole Heart Model



DF = 5.5Hz, (15 cycles)



DF = 6.6Hz, (17 cycles)



DF = 4.7Hz, (20 cycles)

5mm



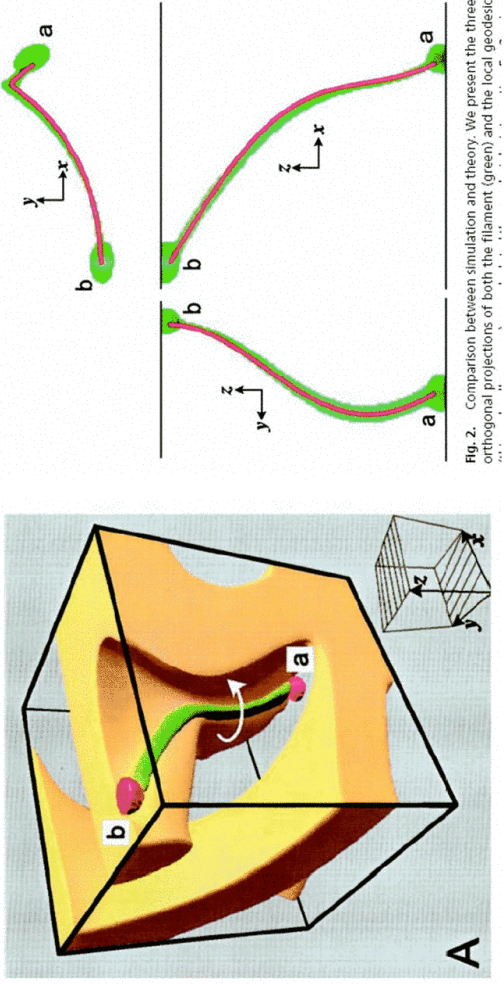
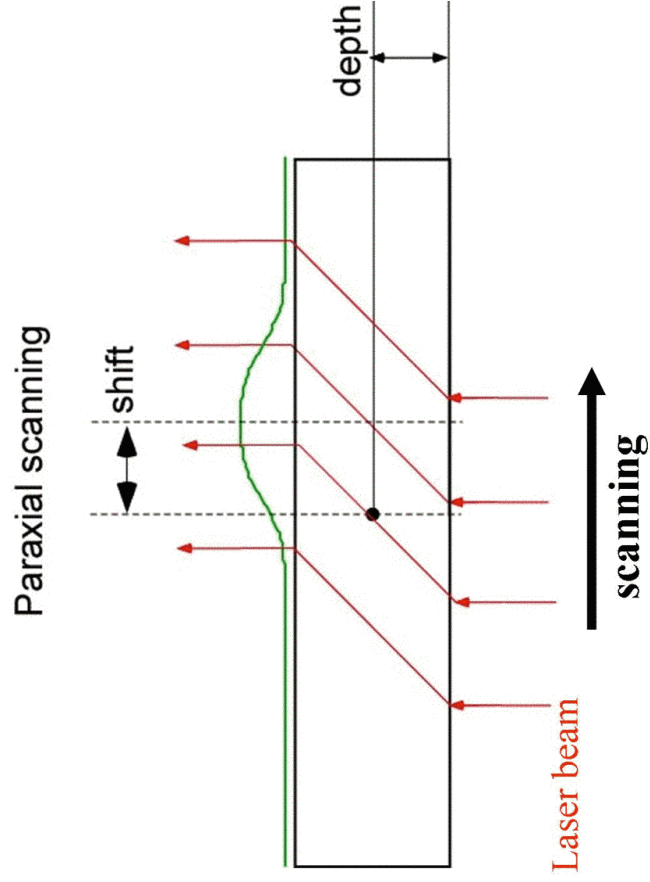


Fig. 2. Comparison between simulation and theory. We present the three orthogonal projections of both the filament (green) and the local geodesic

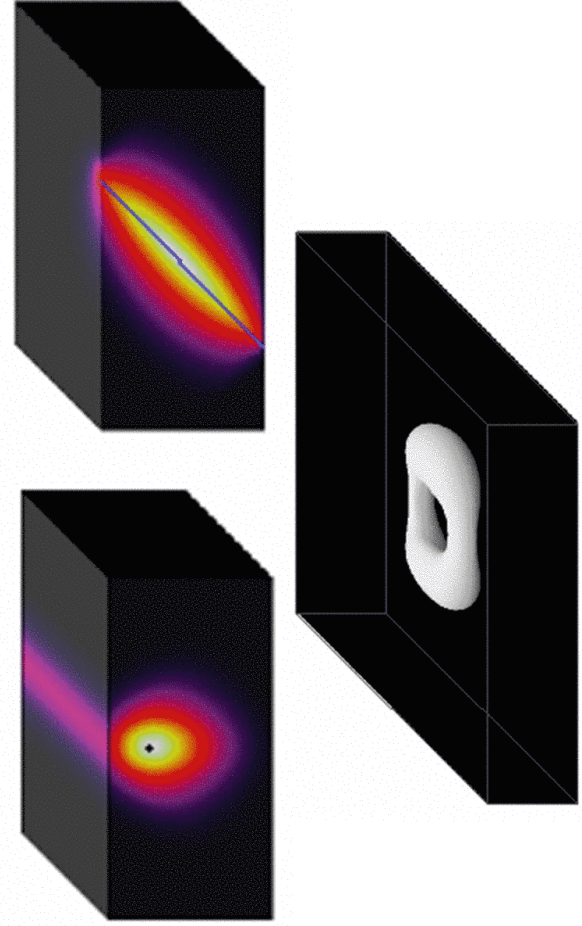
PLoS | June 11, 2002 | vol. 99 | no. 12 | 8017

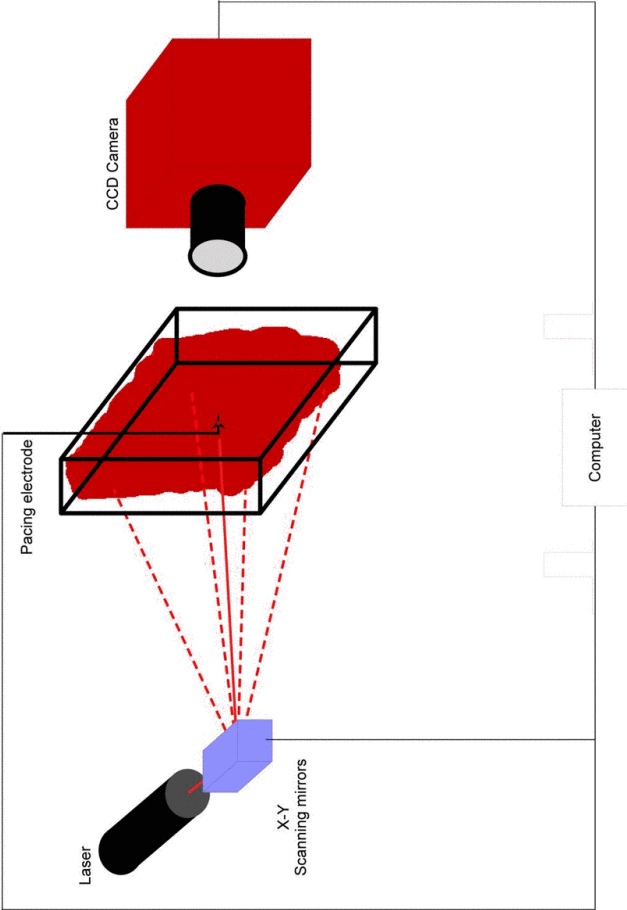
# Paraxial Scanning

extracting depth information

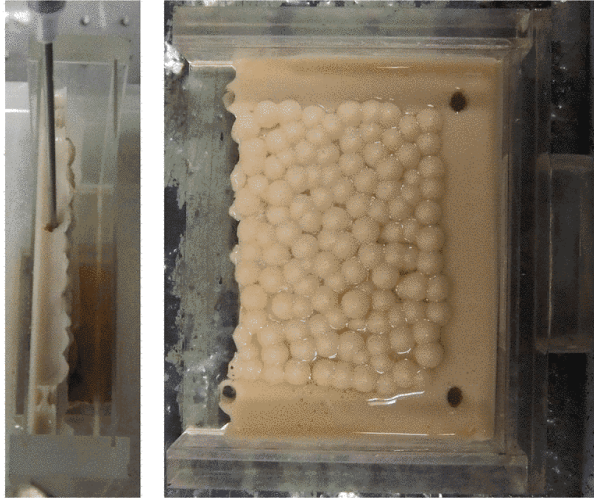
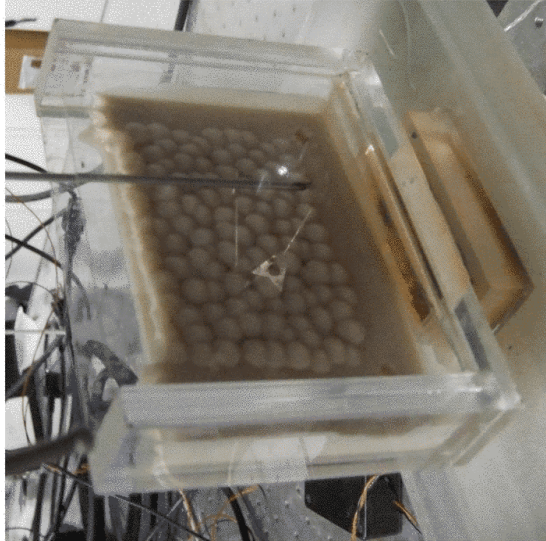


### Reconstruction of the filament

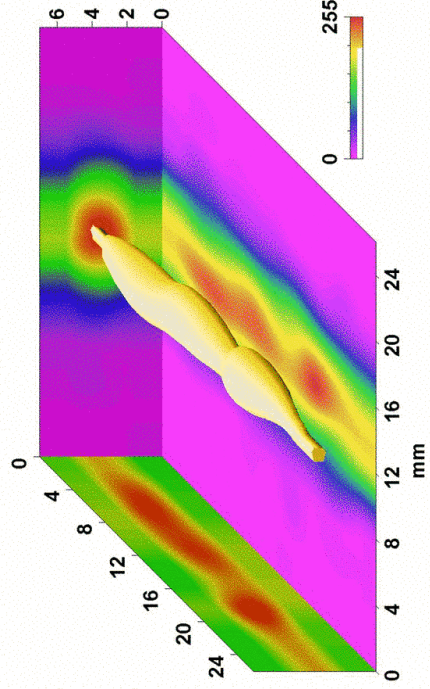




# Phantom experiments

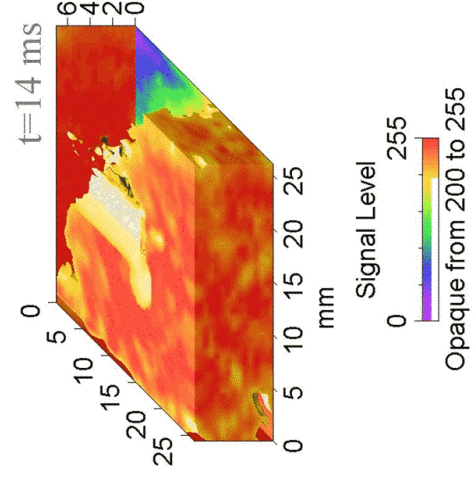


# Reconstruction



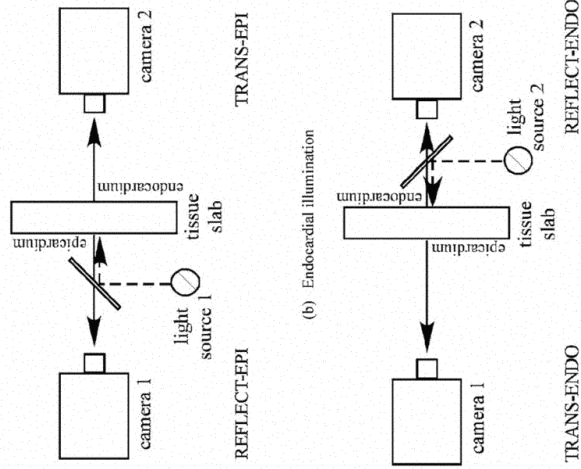
- Scanned area: 40x40 mm
- Reconstructed area: 26x26 mm
- No of points:169
- Object diameter: 2 mm

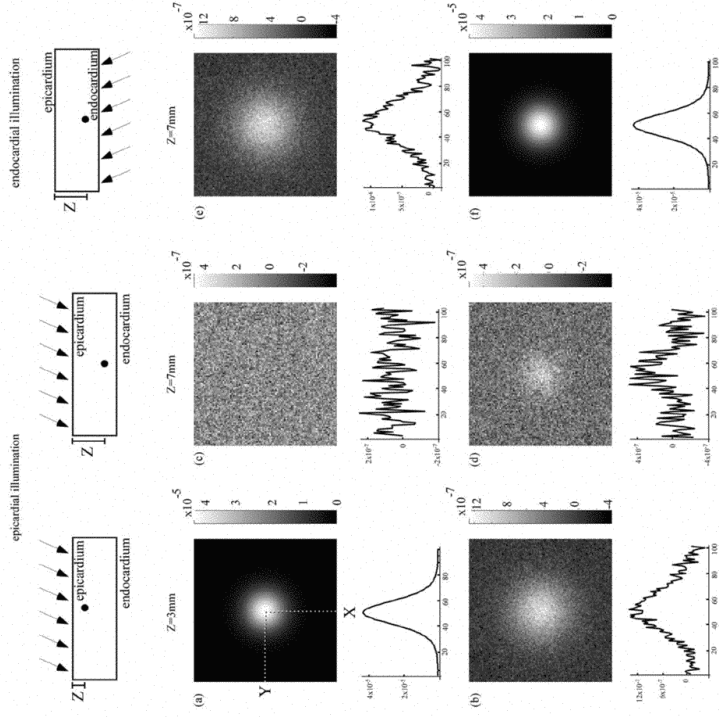
Porcine RV wall, epicardial pacing(BCL = 300 ms) stained with JPW-5034



# Alternating transillumination imaging of non-stationary propagation

## The idea of the method





Estimation of depth from integral reflection and transillumination signals

$$Z = \frac{1}{2} \left[ L - \delta \ln \left( \frac{J^{\text{refl}}}{J^{\text{trans}}} \right) \right].$$

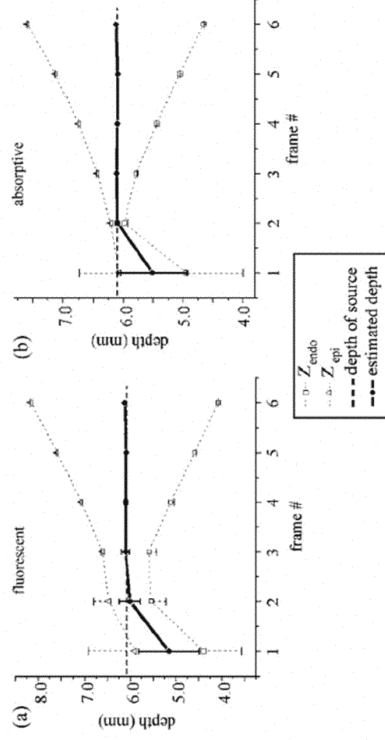


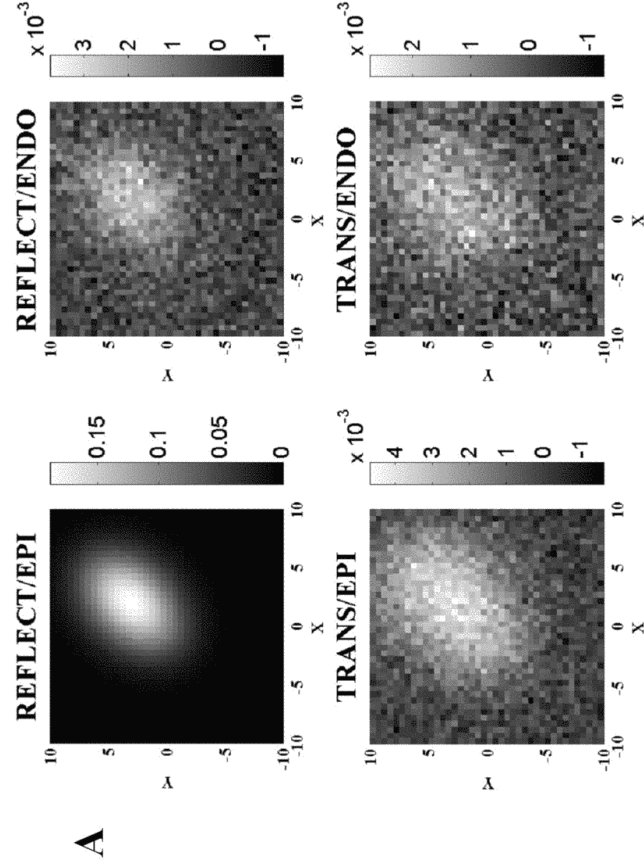
Fig. 5 Accuracy of localizing the excitation center of the expanding hollow ellipsoidal wave using the method of total signal ratios. The actual position of the excitation center (6 mm) is indicated by a dashed line, dotted lines show the calculated depths  $Z_{epi}$  and  $Z_{endb}$ , and the solid line shows the calculated position of the excitation center. The SD due to noise is indicated for each data point. (a) and (b) are for fluorescence and absorption imaging, respectively.

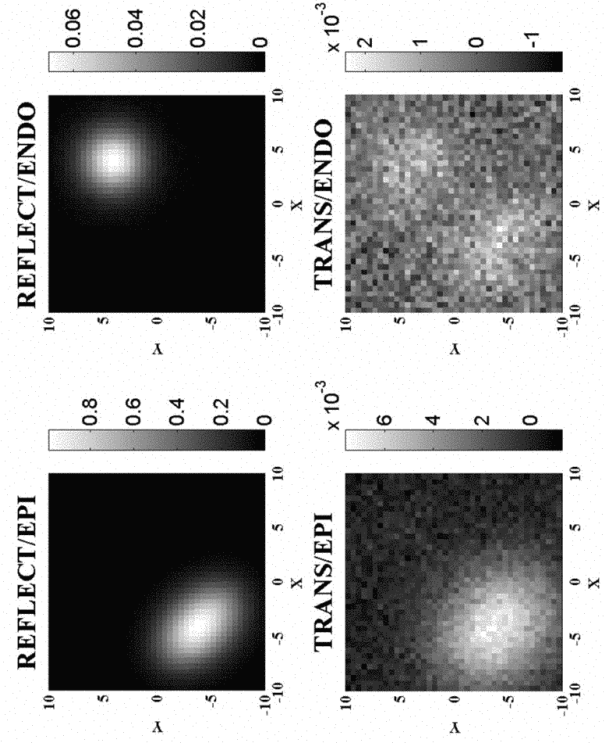
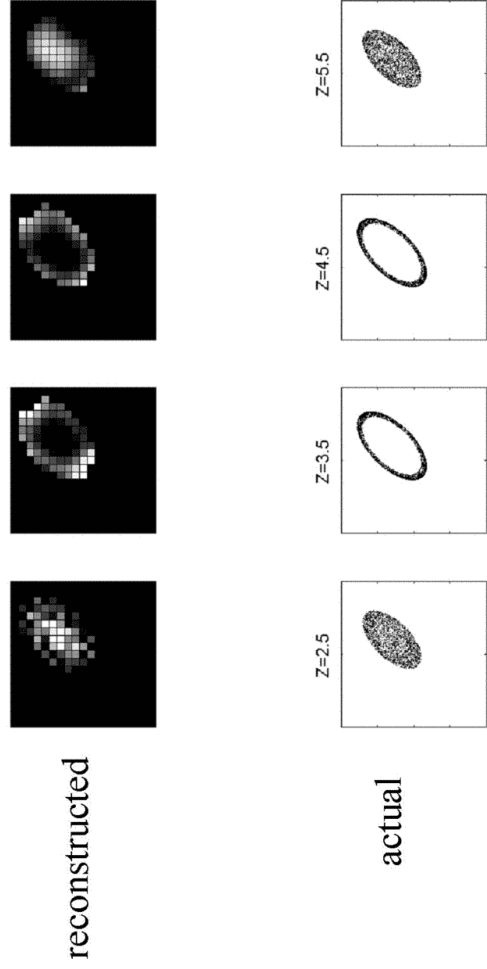
Journal of Biomedical Optics

034007-7

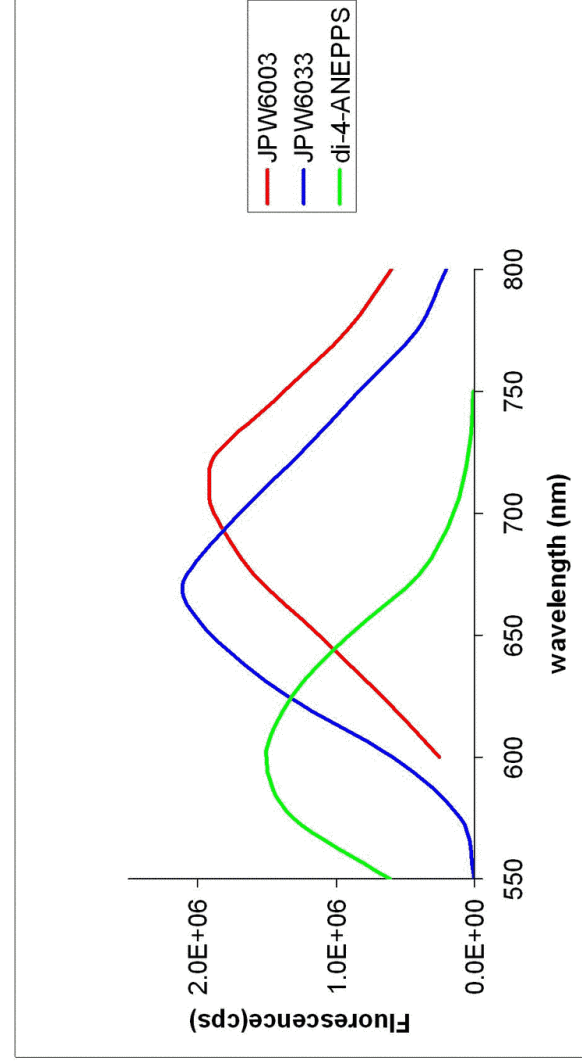
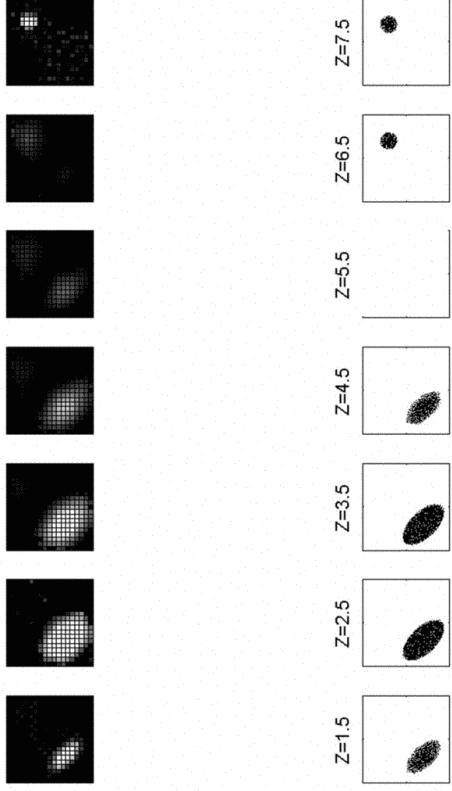
May/June 2006 • Vol. 11(3)

### Quadruplets of images produced by an ellipsoidal front









**Figure 1. Dye emission spectra in multilamellar lipid vesicles (spectrum of di-4-ANEPPS shown for comparison)**

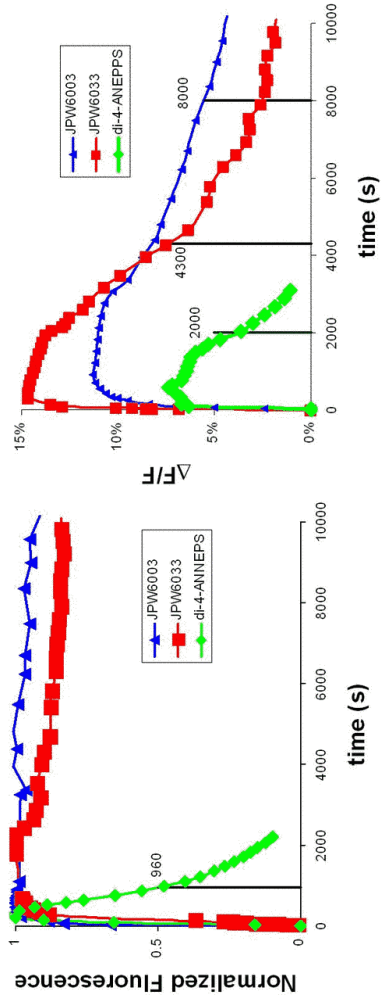


Figure 2. Dye loading and washout dynamics in rat in terms of total (left panel) and voltage-sensitive fluorescence (right panel). Pluronic F-127 was used to load the dye JPW6003 only. Vertical lines show washout half-time.

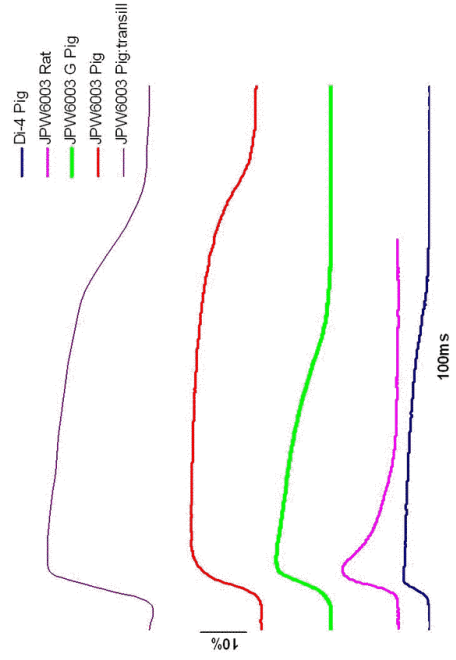


Figure 3. Fluorescence response of the new styryl dye JPW6003 in various cardiac tissues. Traces from bottom to top correspond to di-4-ANEPPS in pig, and JPW6003 in rat, guinea pig, and pig (epifluorescence and transillumination) respectively. washout dynamics in pig.

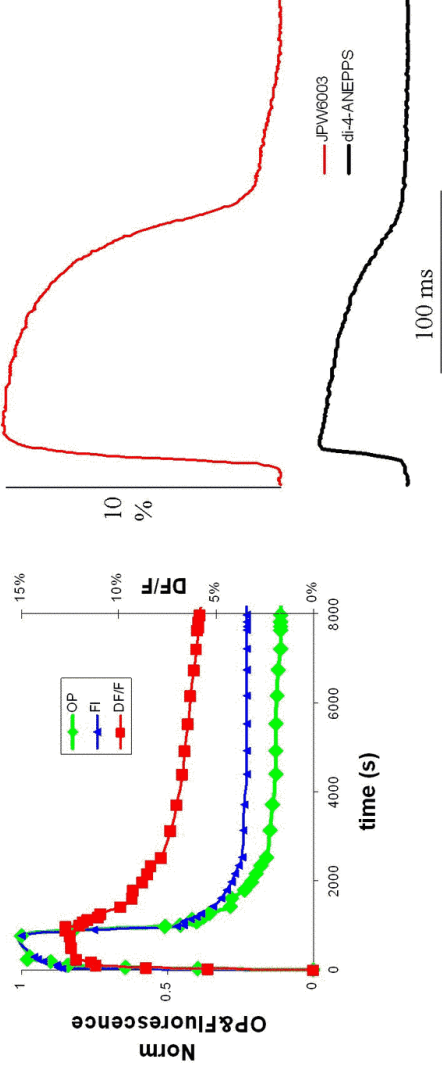


Figure 4. JPW6003 performance in blood perfused pig heart. Left panel shows dye loading and washout dynamics in terms of optical action potential amplitude, total and voltage-sensitive fluorescence. Right panel compares optical potential between JPW6003 and di-4-ANEPPS.

## Acknowledgements:

- Christopher Hyatt
- Sergey Mironov
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- Bogdan Mitrea
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- Alexey Zaitsev
- Christian Zemlin