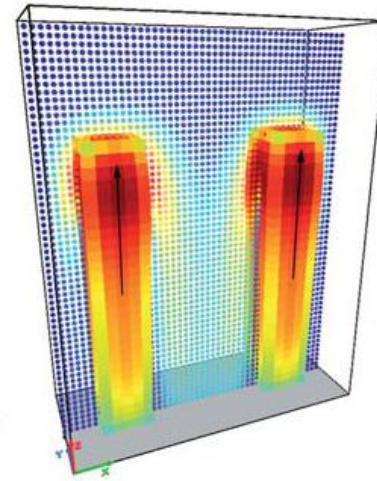
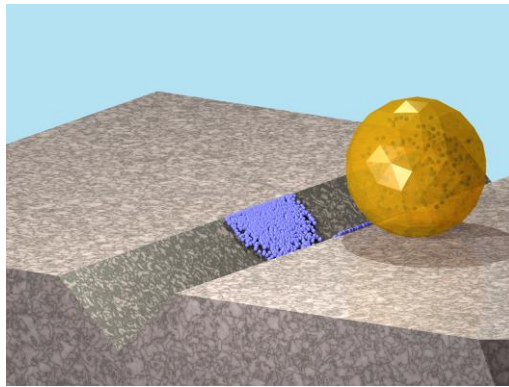


Multi-scale Modeling of Biomimetic Systems: Designing Synthetic Leukocytes and Artificial Cilia

Pratyush Dayal, Amitabh Bhattacharya,
Olga Kuksenok, German Kolmakov



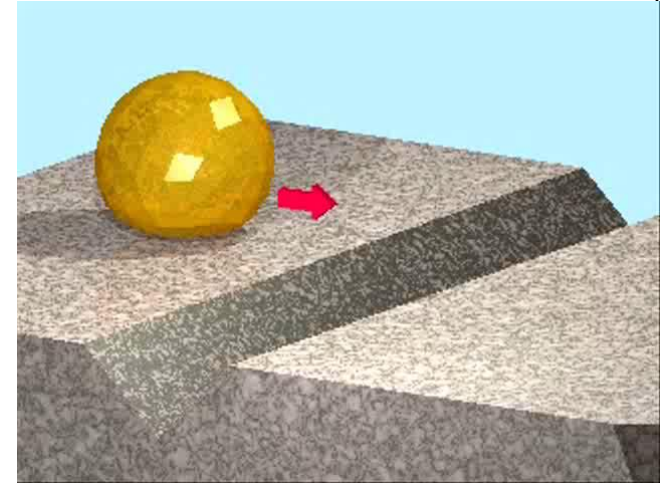
Anna C. Balazs

Chemical Engineering Department
University of Pittsburgh, Pittsburgh, PA

● Design Challenges

□ Integrate interactions among all species

- ☞ Micron and millimeter-sized soft elements
- ☞ Nanoparticles
- ☞ Fluids

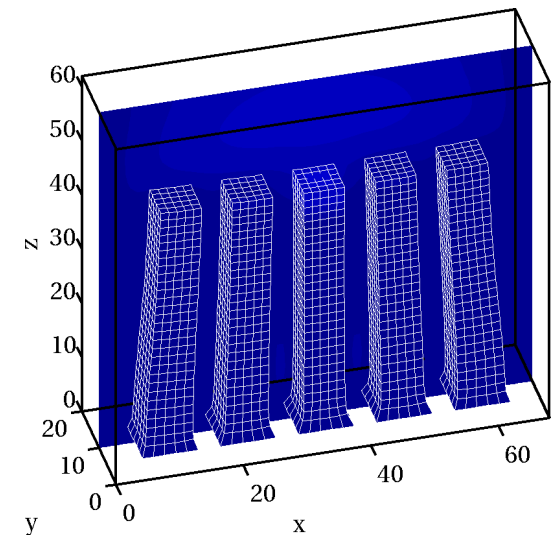


□ Capture dynamic behavior of all species

- ☞ Motion of microscopic compliant objects
- ☞ Diffusion of sub-micron species
- ☞ Fluid flow

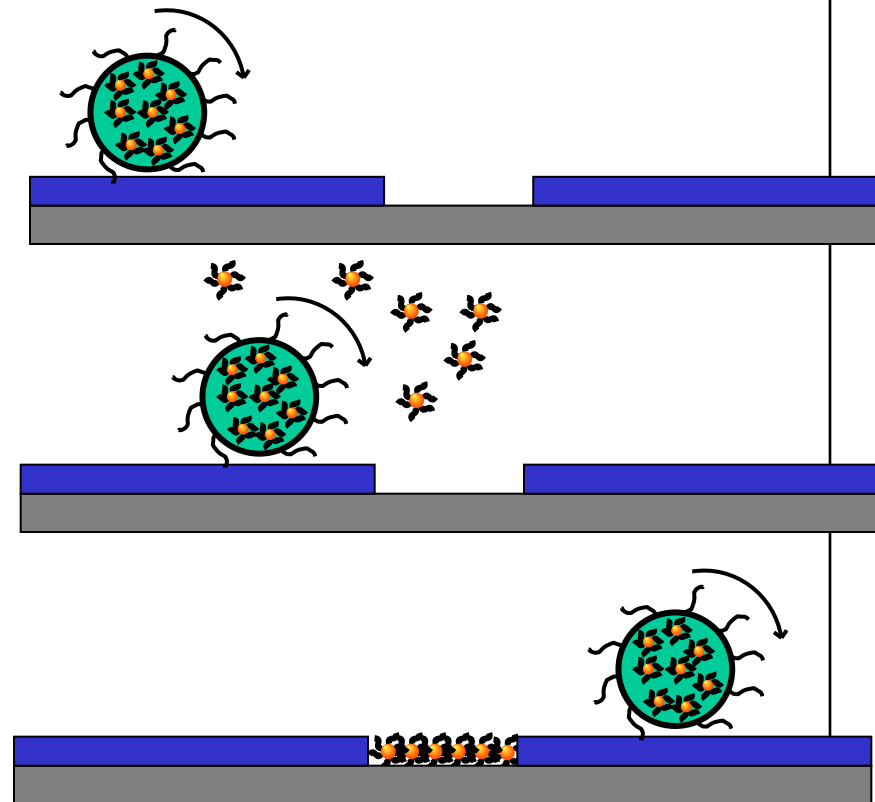
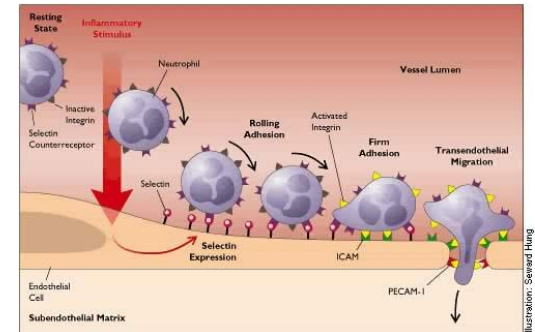
□ Provide useful guidelines for experiments

- ☞ Determining ideal materials to observe predicted behavior



Example 1: Design “Leukocytes” to Heal Synthetic Systems

- ❑ Create synthetic cells with similar features
 - ☞ Can sense & respond to damage
 - ☞ Extend lifetime & sustainability of system
- ❑ “Cell”: nanoparticle-filled microcapsule
- ❑ Drive capsules to move along damaged surface
 - ☞ Contains nano- or micro-crack
- ❑ Localize at crack
- ❑ Trigger release of particles
- ❑ Move on to next crack
 - ☞ Create “repair and go”



● Design Synthetic “Cells” with Biomimetic Functionality

❑ Cells utilize complex biochemical machinery

☞ Multiple, interacting components

❑ Goal: achieve biomimetic functionality using purely synthetic components

❑ Focus on microcapsules

☞ Same size as cells

❑ Can encapsulate various species

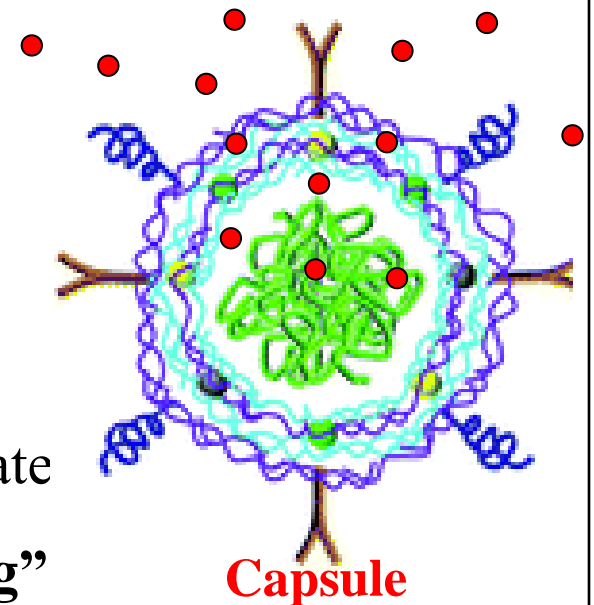
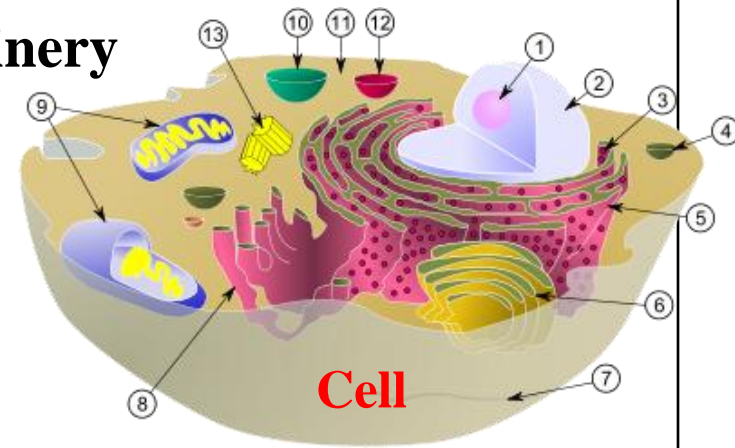
☞ Species diffuse out of porous capsule

☞ Set up communication with exterior

❑ Can functionalize outer surface of capsule

☞ Capsules can “sense” properties of substrate

❑ Function of interest: response to “wounding”



● Model: Hybrid Computational Approach

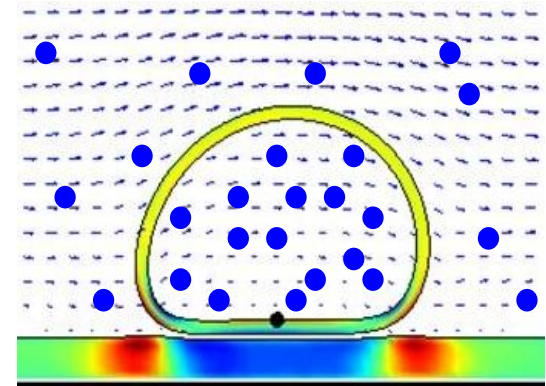
❑ Microcapsule: fluid-filled elastic shell

❑ Serves as model for

☞ Biological cells (leukocytes)

☞ Polymeric microcapsules

❑ Encapsulates nanoparticles



❑ Develop hybrid approach for capturing following interactions:

☞ Capsule-substrate

☞ Lattice Spring model

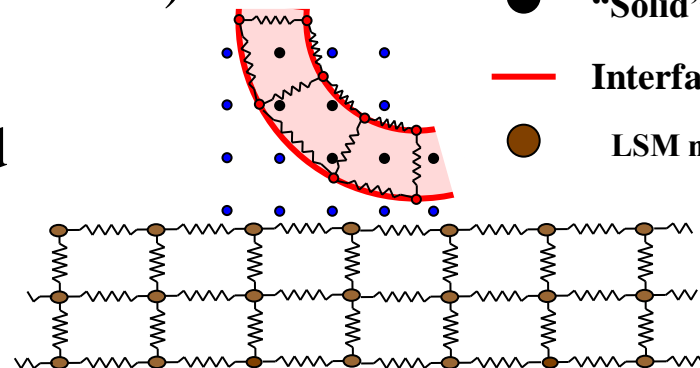
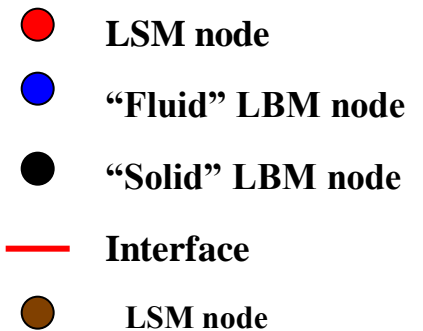
☞ Shell-fluid (encapsulated & external)

☞ Lattice Boltzmann model

☞ Particle-fluid & particle-solid

☞ Tracer particles

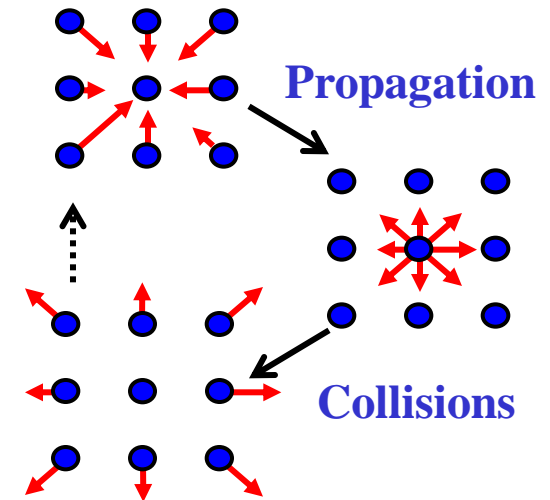
☞ Brownian dynamics



Model for Elastic Shell in Fluid

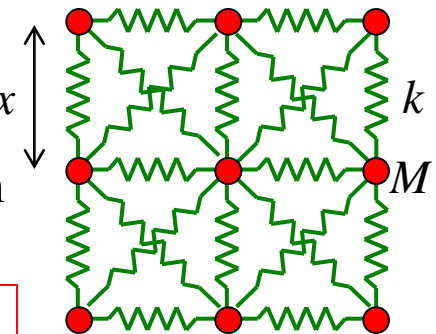
□ Lattice Boltzmann model (LBM) – solver for Navier-Stokes equations

- ☞ Fluid particles move along lattice
- ☞ Collisions allow particles to reach equilibrium
- ☞ Hydrodynamic fields obtained from velocity moments of the distribution function



□ Lattice spring model (LSM) – solver for continuum elasticity equations

- ☞ Network of harmonic springs connecting mass points
- ☞ 3D: 18 springs connecting nodes on a regular lattice Δx
- ☞ Integrate Newton equation of motion: Verlet algorithm



□ Coupling of LB and LSM

- ☞ At the fluid-solid boundaries

$$\text{Poisson ratio} = 1/4$$

$$\text{Young's modulus } E = \frac{5k}{2\Delta x}$$

$$\text{Solid density } \rho_s = \frac{M}{(\Delta x)^3}$$

A. Alexeev *et al.*, *Macro.* **38**, 10244 (2005)

Repair-and-Go System

□ Amphiphilic microcapsules

- ☞ Hydrophilic exterior
- ☞ Hydrophobic interior

□ Adhesion between capsule and substrate

- ☞ Modeled via Morse potential

$$U(r) = \varepsilon_0 \left(1 - \exp \left(- \frac{r - a}{r^*} \right) \right)^2$$

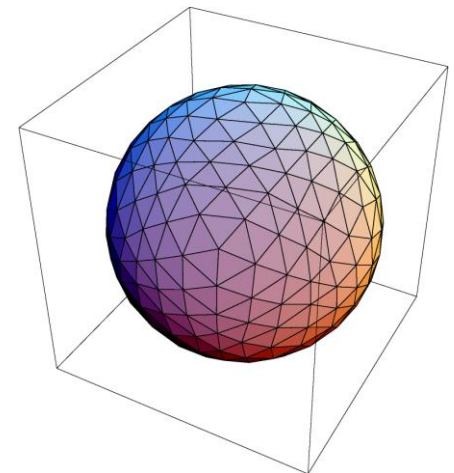
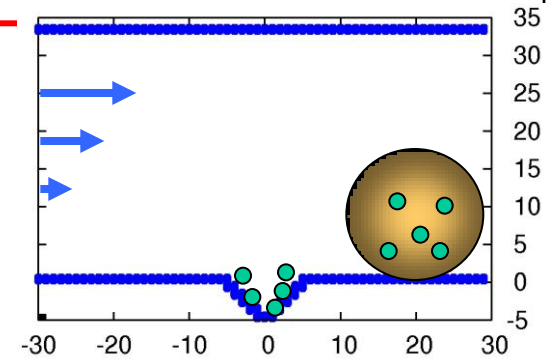
□ Capsules encase hydrophobic nanoparticles

- ☞ Dispersed in oil phase

□ Capsule driven by imposed shear flow

- ☞ Move over hydrophilic, cracked surface

□ Interior surface of crack hydrophobic



$N = 2$ layers \times 122

$D = 10\Delta x$, $\Delta x \approx 1.5$

$r^* = D/10$

Crack width = D

● Nanoparticle Dynamics

□ Dynamics within capsule

$$d\mathbf{r} = \mathbf{u} dt + \sqrt{2D} d\mathbf{W}(t)$$

☞ Equivalent to convection-diffusion for NP density

$$\frac{\partial n}{\partial t} = (\mathbf{u} \nabla) n + D \Delta n$$

□ “Tunneling” toward crack wall

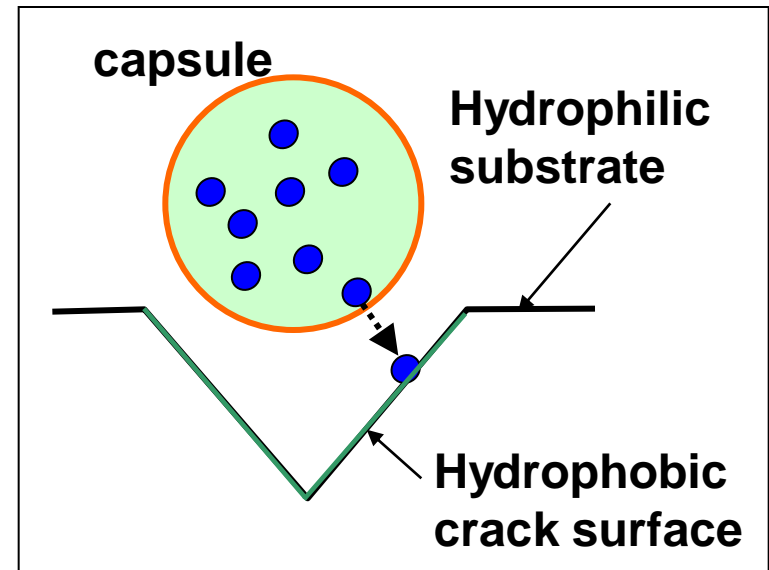
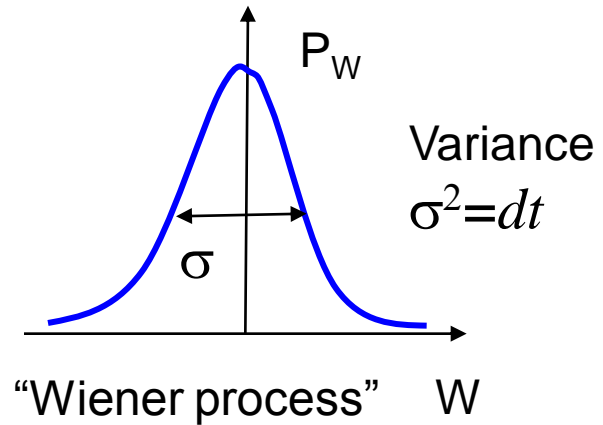
$$k = t_{tun}^{-1} e^{-r/r_{tun}}$$

$$w_{tun} = 1 - e^{-k\Delta t}$$

$r_{tun} \sim R^*$; R^* = range of adhesion force

□ If particle tunnels through

☞ Becomes stuck at crack walls



● Motion of Capsules

❑ Effect of imposed shear flow

❑ Low shear:

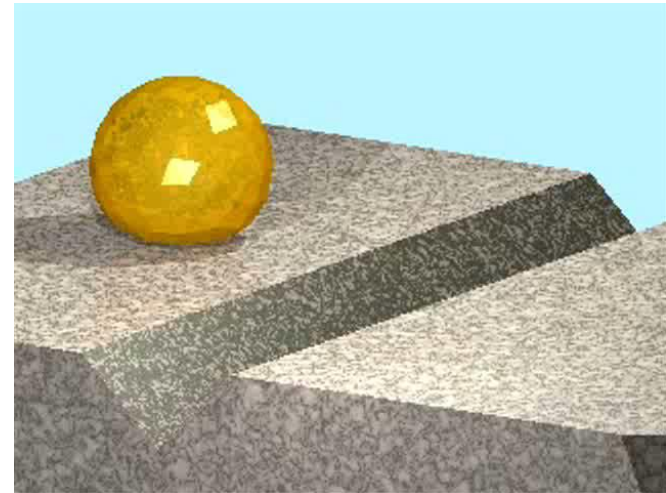
☞ Captured in crack—(1)

❑ Moderate shear:

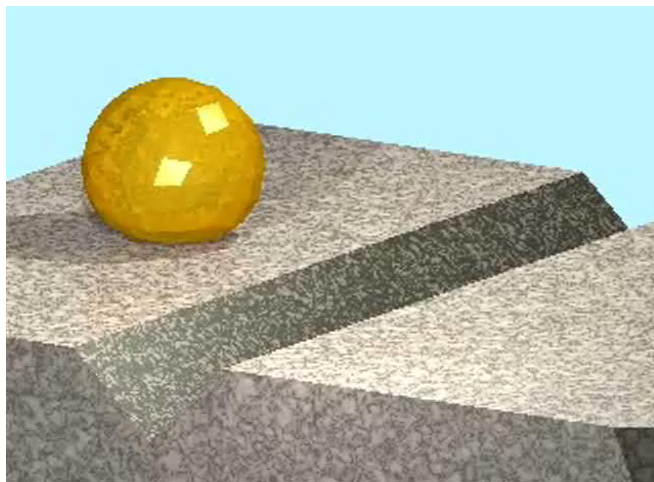
☞ Move along substrate—(2)

❑ High shear:

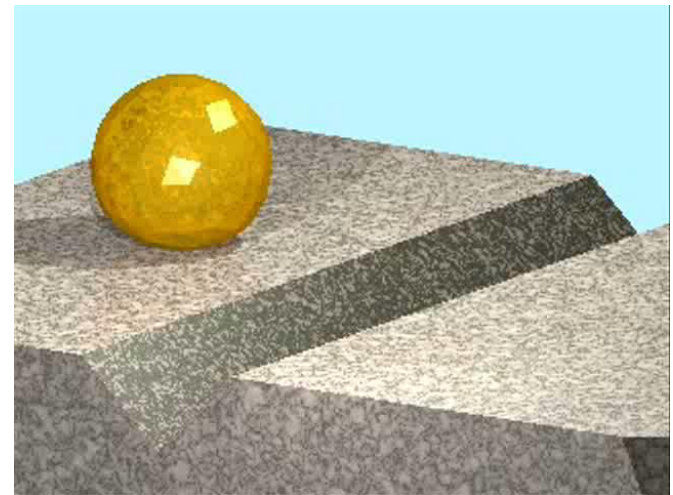
☞ Fly away due to lift force—(3)



(1)



(2)



(3)

Phase Map for Capsule Motion

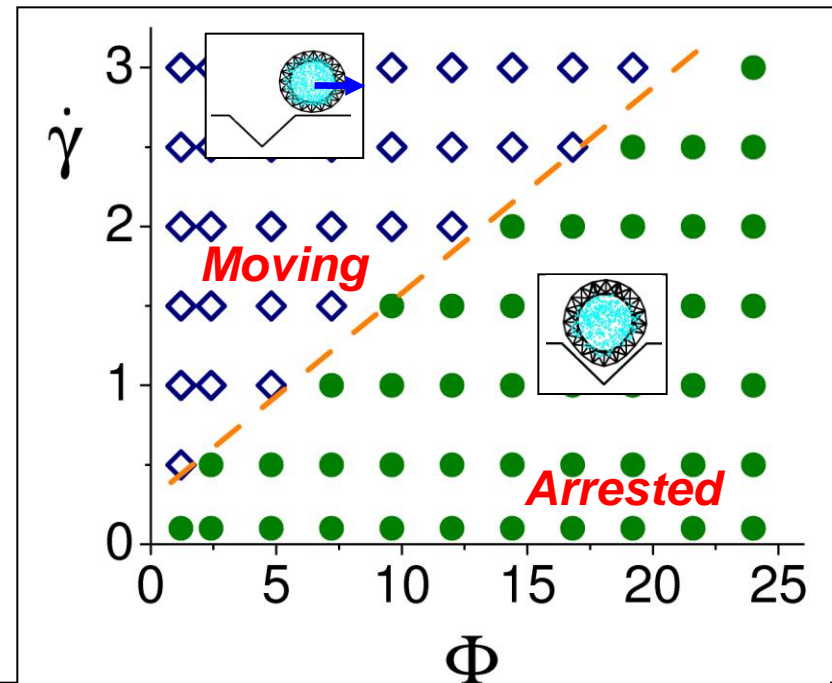
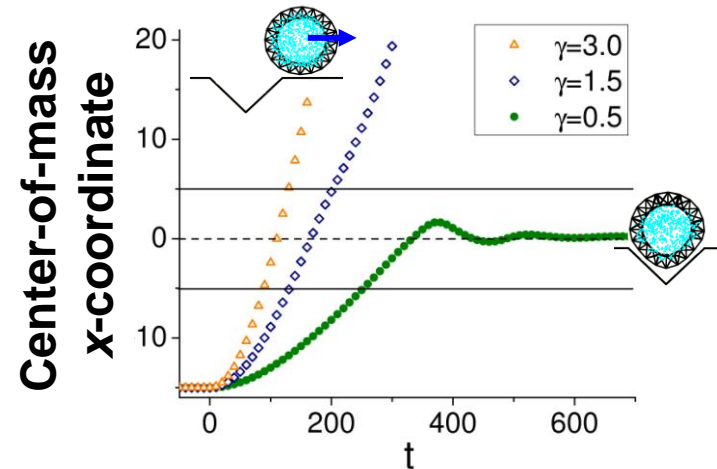
Dimensionless capsule-surface adhesion strength

$$\Phi = \frac{\text{attraction strength}}{\text{capsule stiffness}} = \frac{\varepsilon_0 N}{ERr^{*2}}$$

- ☞ E – Young's modulus
- ☞ R – capsule radius
- ☞ ε_0 – capsule-surface interaction
- ☞ r^* – interaction cut-off length
- ☞ N – number of gel nodes

G. Kolmakov et al

ACS Nano, 4 (2010) 1115-1123



● Deposition of Nanoparticles

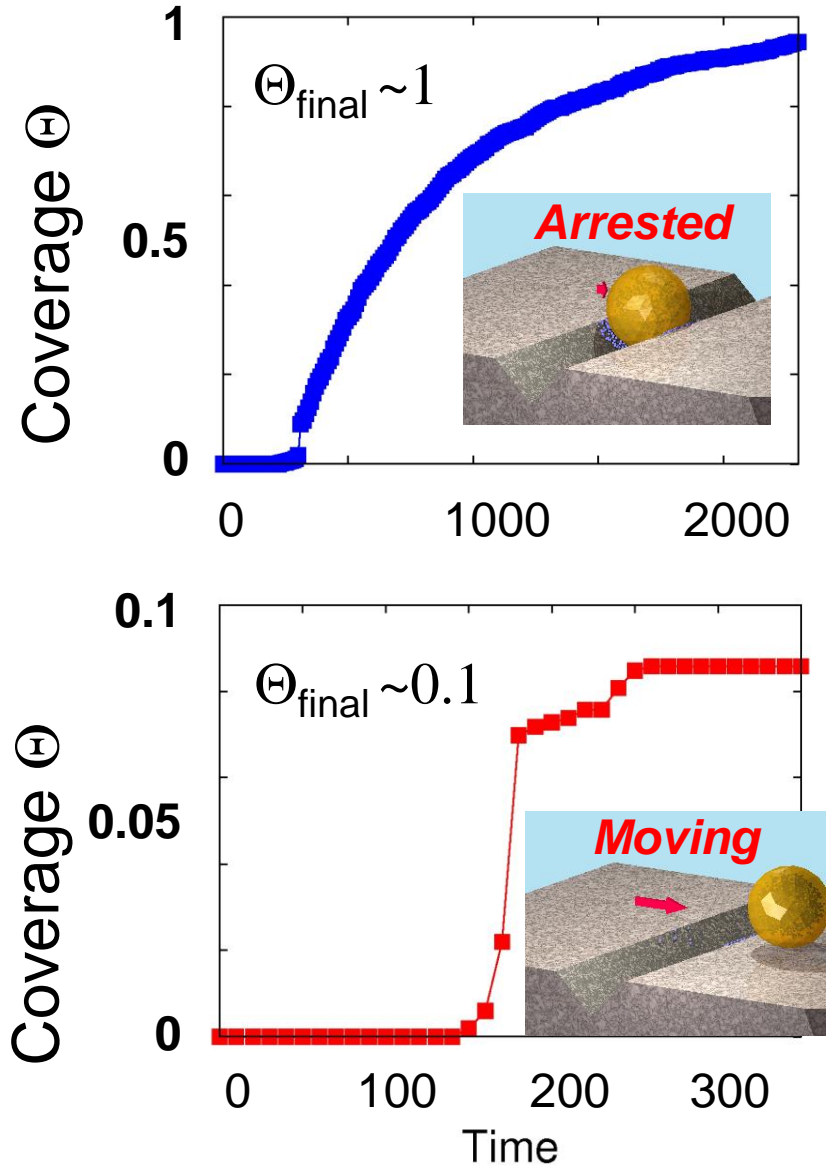
- ❑ **Capsule releases NPs on crack surface**
- ❑ **At low shears and strong adhesion:**
 - ☞ Arrested capsule
 - ☞ Virtually full coverage of crack surface by NPs

$$\Theta_{\text{final}} = N_{\text{NP}}/N_{\text{NP}}^{(\text{max})} \sim 1$$

- ❑ **At high shear and weak adhesion:**

- ☞ Moving capsule
- ☞ Partial coverage

$$\Theta_{\text{final}} \sim 0.1$$



● Arrested Capsule

□ Deposition of NPs on crack surface

$$N_{NP}^{(caps)}(t) = N_{NP}^{(caps)}(0) \exp(-t/\tau_d)$$

☞ τ_d – characteristic deposition time

☞ Coverage at $t \gg \tau_d$

$$\Theta = 1 - \exp(-t/\tau_d) \rightarrow 1$$

□ Value of τ_d depends on

☞ Adhesion strength

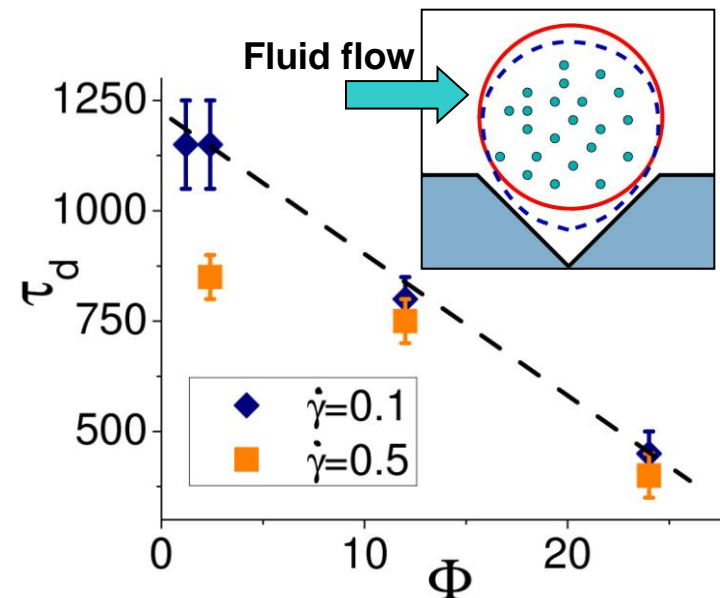
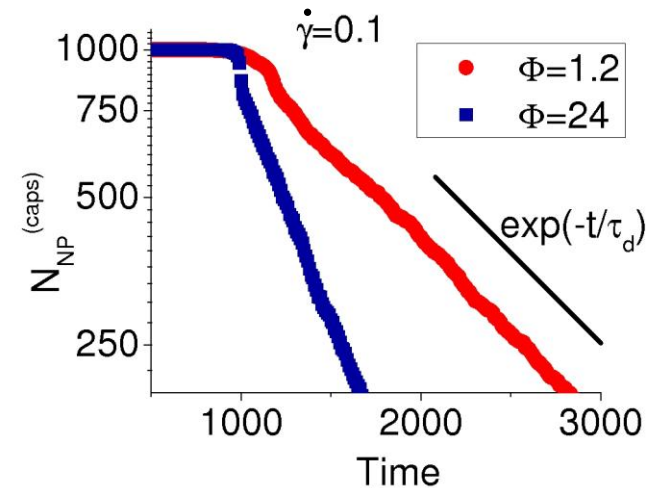
☞ Deform capsule by adhesion

☞ Shear rate at weak adhesion

☞ Deform capsule by fluid flow

□ But want repair and go

☞ Need capsule to leave crack

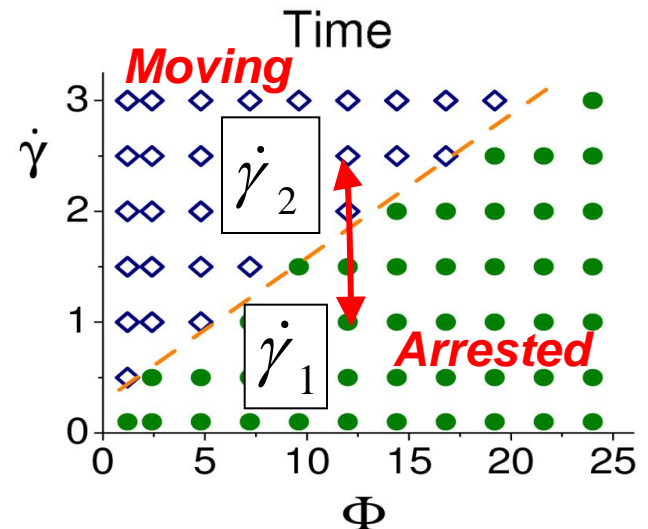
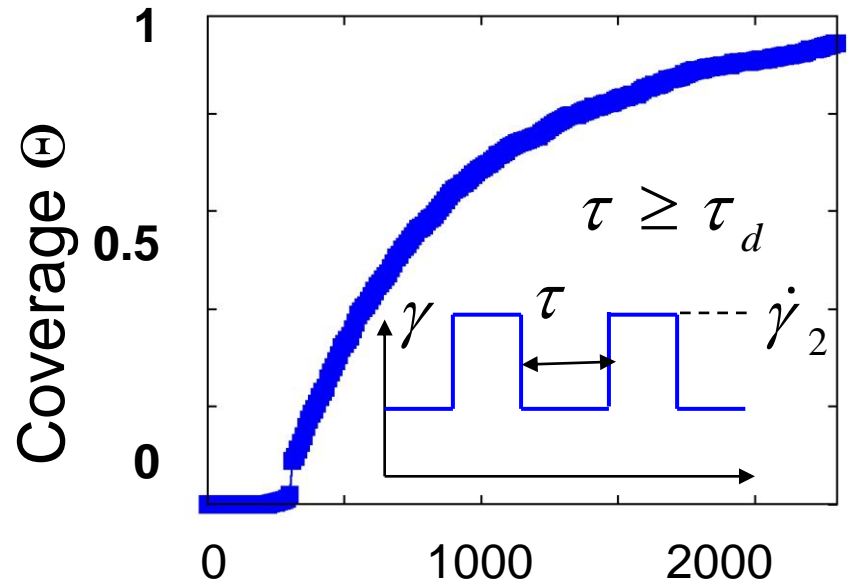
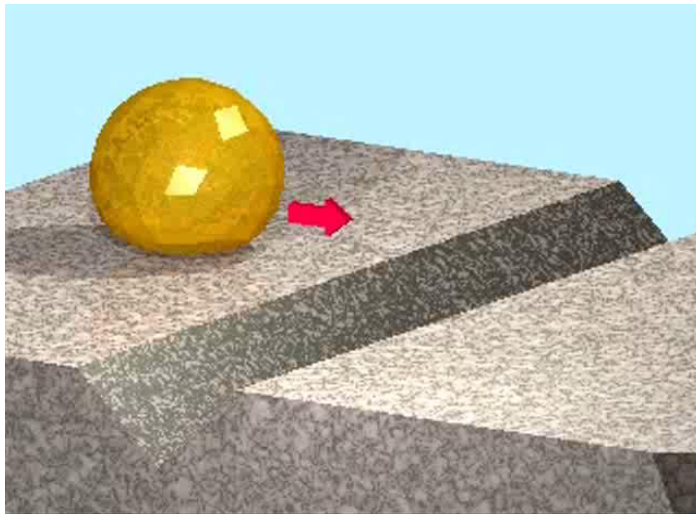


● Possible Solution: Capsule in Pulsatile Flow

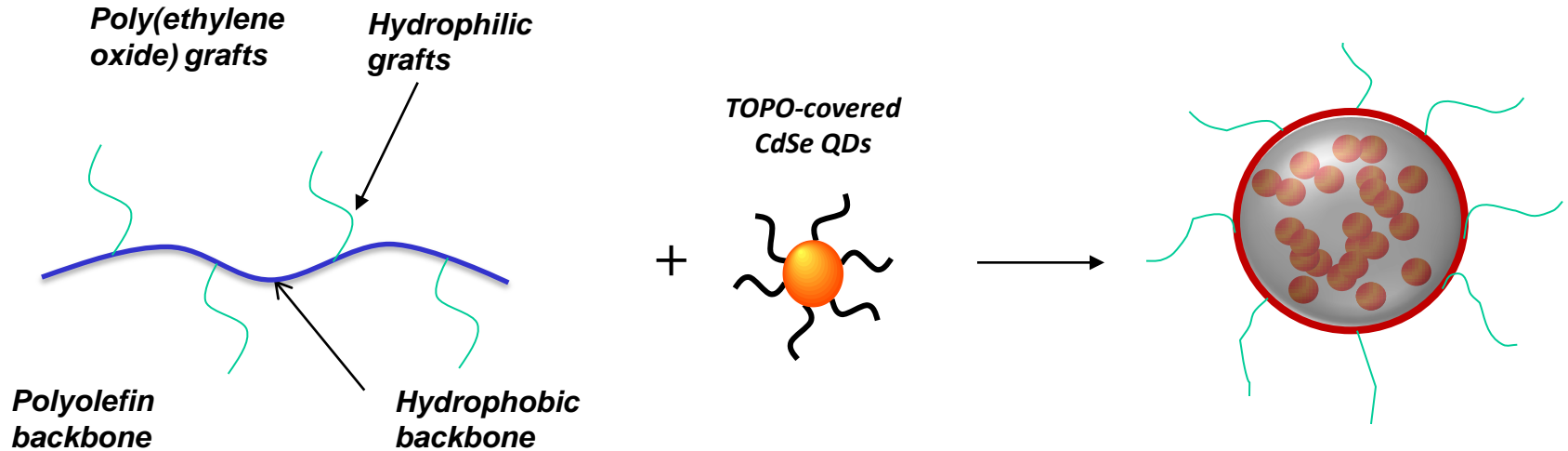
□ Motion of capsule

- ☞ Arrested at low shear period
 - ☞ Releases NPs
- ☞ Leaves crack at high shear period
 - ☞ Moves toward next crack

□ Resultant coverage $\Theta \sim 1$

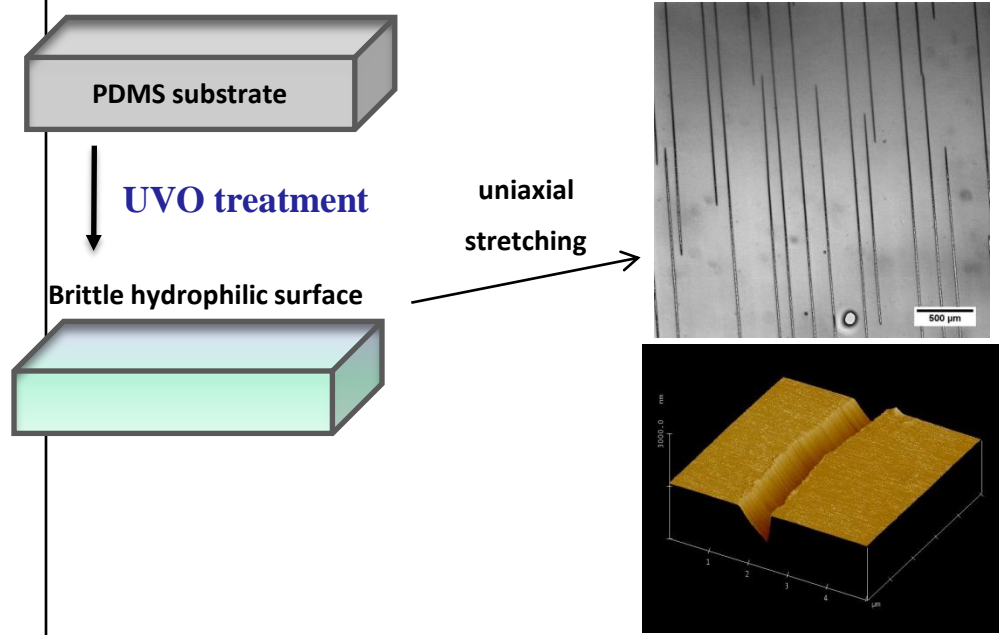


● Experiments: A. Crosby, T. Emrick, T. Russell, UMass

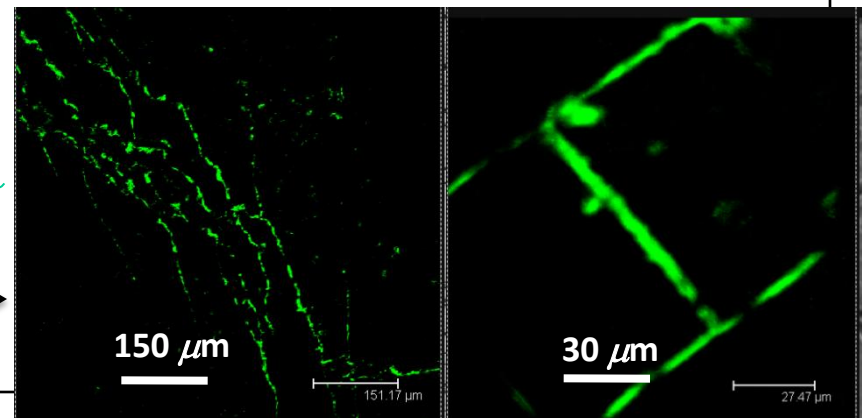
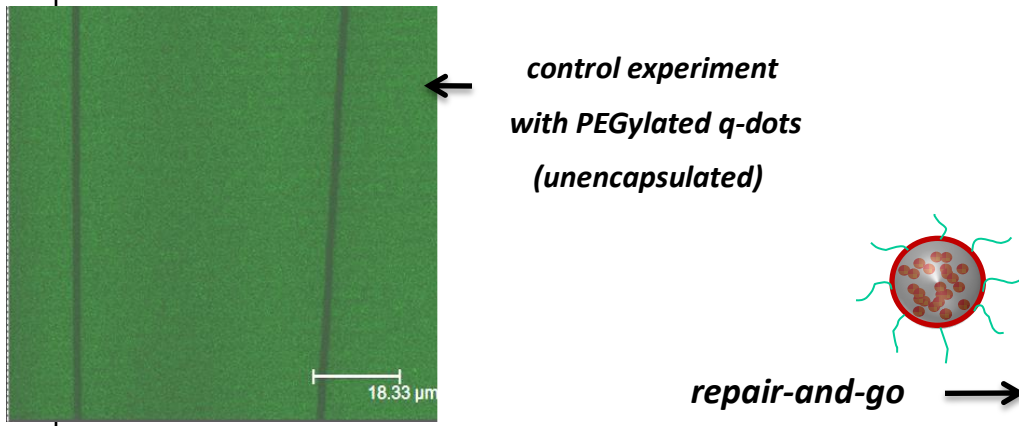


- ❑ **Microcapsule: formed from amphiphilic comb copolymer**
 - ☞ Hydrophilic teeth, hydrophobic backbone
- ❑ **Nanoparticles: quantum dots with hydrophobic coating**
- ❑ **In oil/water mixtures: form nanoparticle-loaded capsules**
 - ☞ Nanoparticles localized in encapsulated oil phase
 - ☞ Forms in one step
 - ☞ Capsule stable in water—hydrophilic teeth

● Crack Repair with Nanoparticle-loaded Capsules



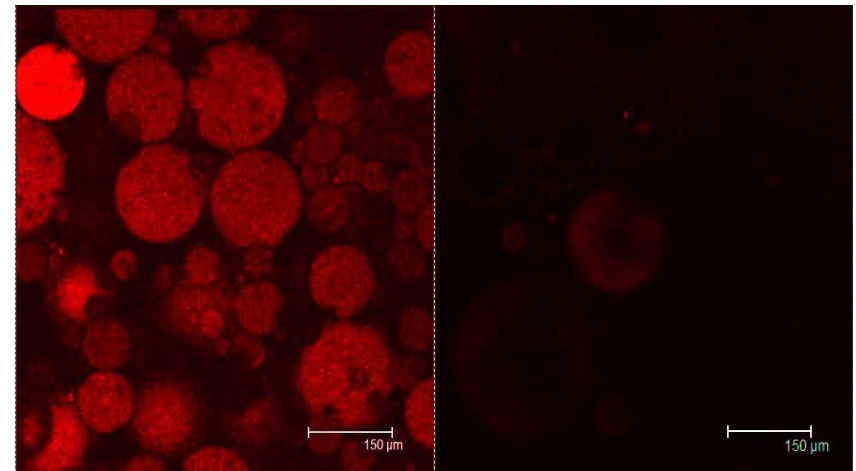
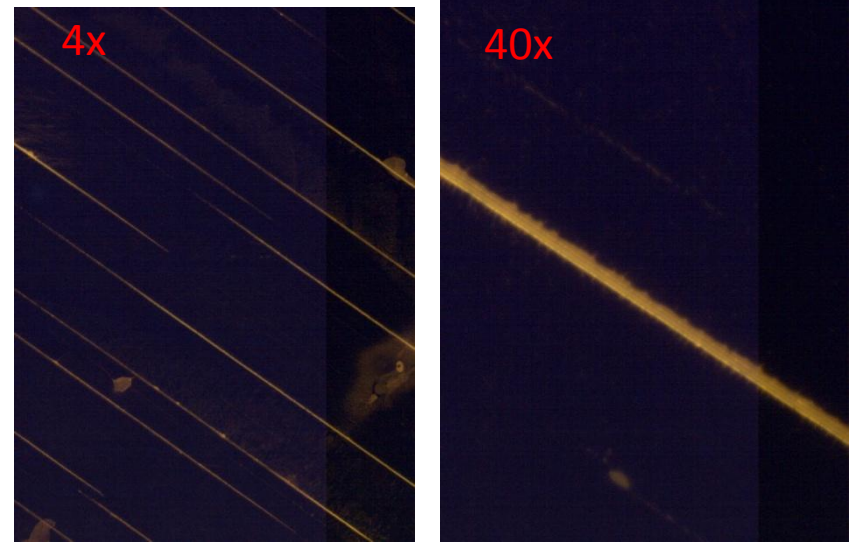
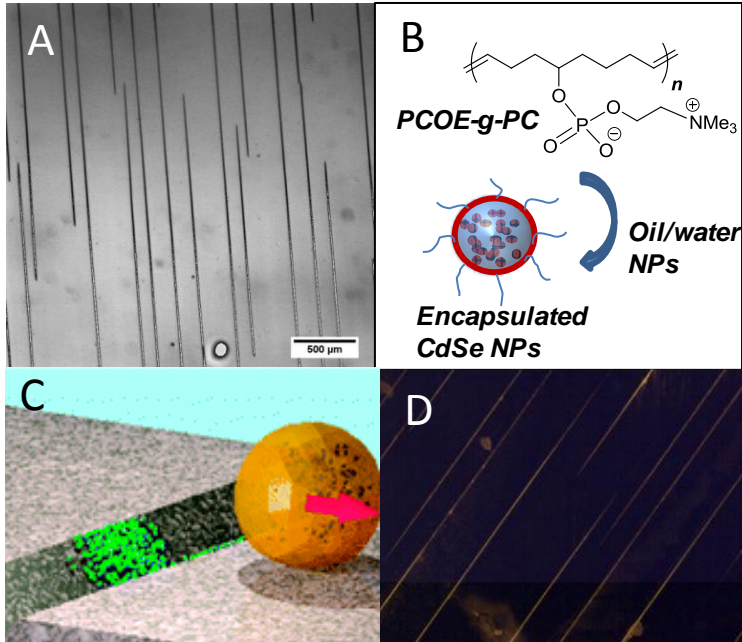
15 mL/min; ~15 psi back pressure, Pulsed intervals: flow and rest



Crosby, Emrick, Russell

● Site-specific Nanoparticle Deposition

Repair-and-go with PC-polyolefin microcapsules



K. Kratz et al. Nature Nanotechnology, 7 (2012) 87-90

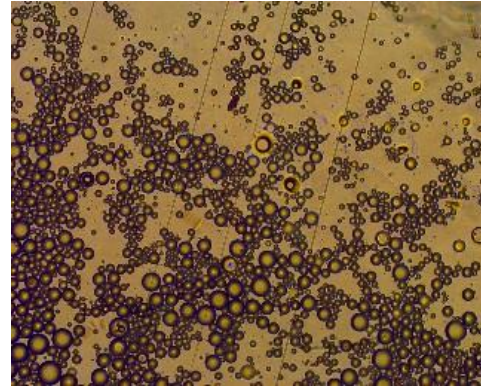
□ Bottom image

- ☞ Left—capsule before exp.
- ☞ Right—capsule after exp.
- ☞ Nanoparticles remain in crack

● Control Experiments

□ No nanoparticles in capsules

- ☞ No localization of capsules into cracks
- ☞ Capsules labeled with rhodamine



80 μm



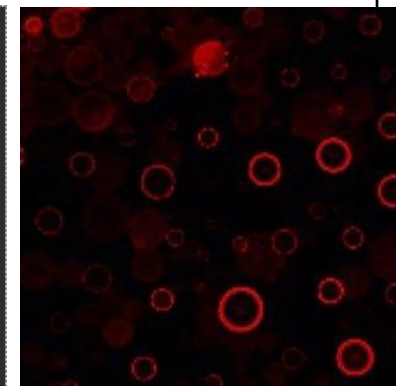
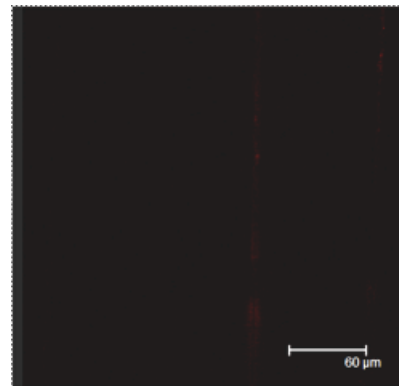
20 μm

□ No capsules—free particles

- ☞ In water and PEG-coating, particles bound everywhere on surface
- ☞ In toluene and hydrophobic coating, non-selective deposition

□ No difference in surface energies

- ☞ Oxidation of surface after cracking
 - ☞ No hydrophobic domains
- ☞ No surface deposition of particles
 - ☞ Remain in capsules



● Example 2: Design Artificial Chemo-responsive Cilia

□ Cilia in respiratory system

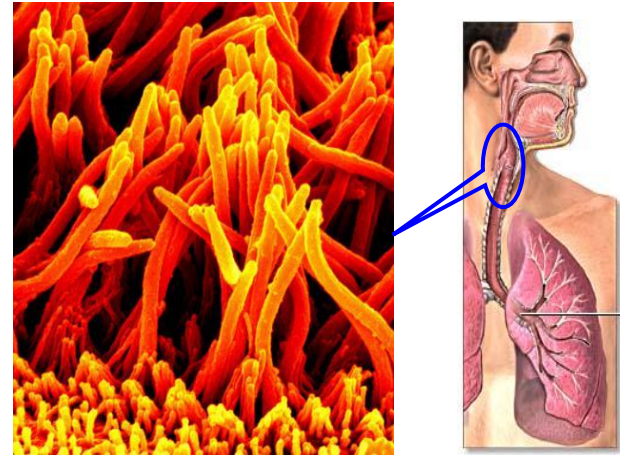
- ☞ Exhibit collective motion
 - ☞ Metachronal waves
- ☞ Can expel particulates

□ Design artificial cilia

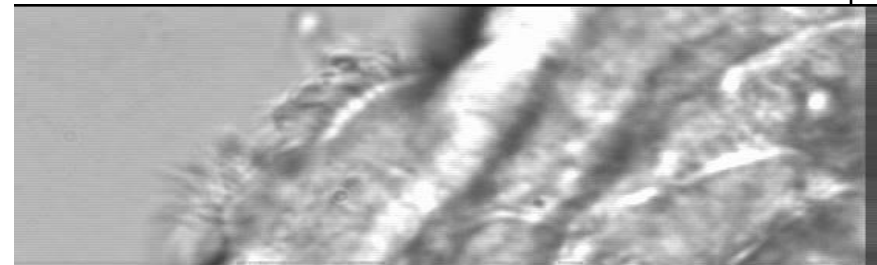
- ☞ System undergoes collective motion

□ Devise BZ cilia

- ☞ Control collective behavior using light
 - ☞ Regulate transport of particles in microfluidic devices



Shah *et al* *Science* 2009, **325**, 1131

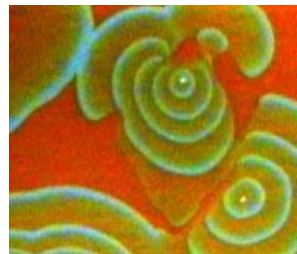


users.umassmed.edu/michael.sanderson/

● Enabling Material—BZ Polymer Gels

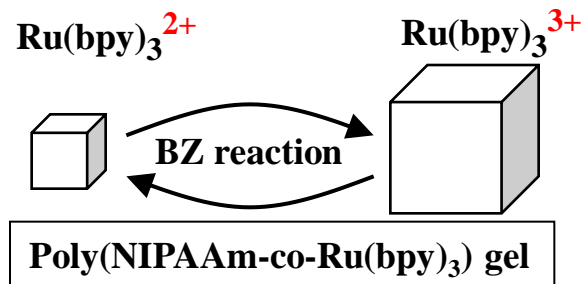
□ BZ reaction in solution

- ☞ Exhibits rich dynamical behavior



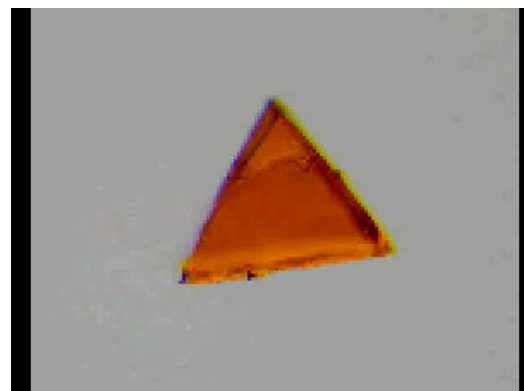
□ BZ in gel causes periodic, *autonomous* swelling/deswelling

- ☞ Catalyst grafted to polymer:

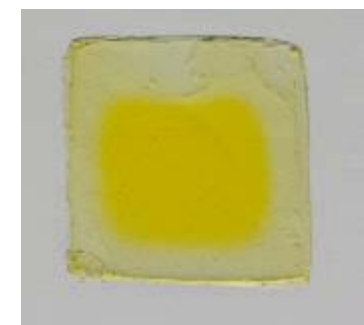


R. Yoshida *et al*, *JACS*, 1996, **118**, 5134.

- ☞ Yellow: swollen polymer
- ☞ Orange: contracted polymer



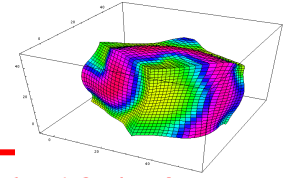
☞ Small sample (~ 1 mm)



☞ Larger: 3 x 3 mm

I. Chen et al,
Soft Matter, 2011, **7**, 3141

● Model for Chemo-responsive Gels in 3D



□ Evolution equations:

V.V.Yashin et al, JCP, 2007, 126, 124707

O. Kuksenok et al. PRE (2008)

$$\frac{\partial \phi}{\partial t} = -\nabla \cdot (\phi \mathbf{v}^p)$$

ϕ, \mathbf{v}^p volume fraction & velocity of polymer

$$\frac{\partial v}{\partial t} = -\nabla \cdot (v \mathbf{v}^p) + \varepsilon G$$

v concentration of oxidized catalyst

$$\frac{\partial u}{\partial t} = -\nabla \cdot (u \mathbf{v}^s) - \nabla \cdot \mathbf{j}^s + F$$

u, \mathbf{v}^s concentration & velocity of activator

$\mathbf{j}^s = -(1 - \phi) \nabla \frac{u}{1 - \phi}$ diffusion of u in system

☞ Reaction kinetics : modified Oregonator model

$$F = (1 - \phi)^2 u - u^2 - f v (1 - \phi) \frac{u - q(1 - \phi)^2}{u + q(1 - \phi)^2}; \quad G = (1 - \phi)^2 u - (1 - \phi)v$$

☞ Relaxational dynamics:

☞ Neglect total velocity

$$\nabla \cdot \hat{\sigma} \sim \zeta(\phi)(\mathbf{v}^p - \mathbf{v}^s)$$

$\hat{\sigma}$ stress tensor

$\zeta(\phi)$ friction coeff.

$$\phi \mathbf{v}^p + (1 - \phi) \mathbf{v}^s \equiv 0$$

Model for Chemo-responsive Gels in 3D

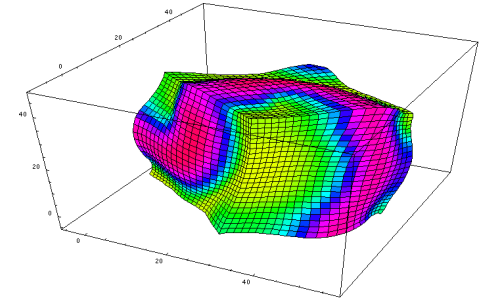
Define energy density of deformed gel

$$U = U_{el}(I_1, I_3) + U_{FH}(I_3)$$

↳ Elastic energy $U_{el} = \frac{c_0 v_0}{2} (I_1 - 3 - \ln I_3^{1/2})$

↳ Interaction energy $U_{FH} = \sqrt{I_3} [(1 - \phi) \ln(1 - \phi) + \chi_{FH}(\phi) \phi(1 - \phi) - \chi^* v(1 - \phi)]$

↳ c_0 is crosslink density, $\chi^* > 0$: hydrating effect of oxidized catalyst



Use 3D gLSM model

↳ Calculate velocities of node \mathbf{n} of element \mathbf{m}

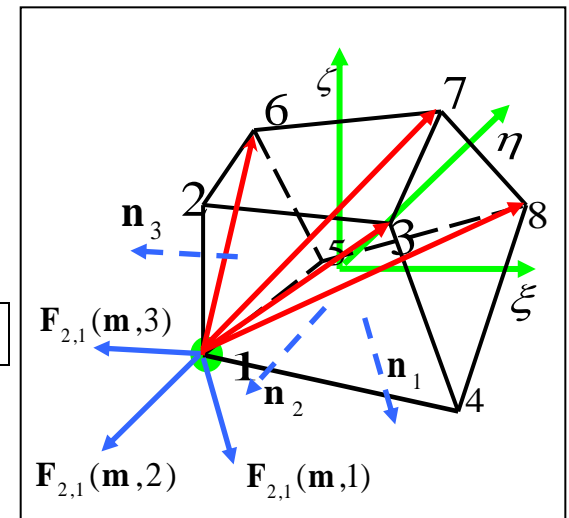
$$\frac{d\mathbf{r}_n(\mathbf{m}, t)}{dt} = M_n(\mathbf{m}, t) [F_{1,n}(\mathbf{m}, t) + F_{2,n}(\mathbf{m}, t)]$$

Spring-like

From pressure

↳ Update $v(\mathbf{m}, t)$ and $u(\mathbf{m}, t)$

↳ Combination of finite elements & finite difference techniques



3D gLSM: Compare Simulations and Experiment

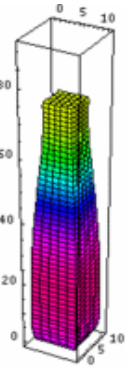
□ Small cubic samples

- ☞ Oscillations uniform though the sample
- ☞ In-phase synchronization of chemical & mechanical oscillations
- ☞ Similar to experiments *R. Yoshida et al, J.Phys.Chem, 104, 2000*



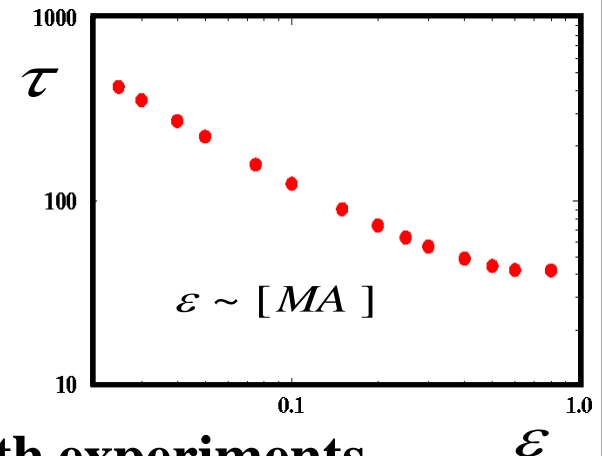
□ Long rectangular samples attached to wall

- ☞ Traveling wave propagates from wall towards free end
- ☞ Similar to experiments *R. Yoshida et al, Chaos, 9,1999,*



□ Effect of $\varepsilon \sim [MA]$ on period of oscillations

- ☞ Increase in [MA] decreases period
- ☞ At higher ε transition to steady-state
- ☞ Similar to experiments *D. Suzuki et al, J.Phys.Chem. B 112, 2008*



□ Simulations are in qualitative agreement with experiments

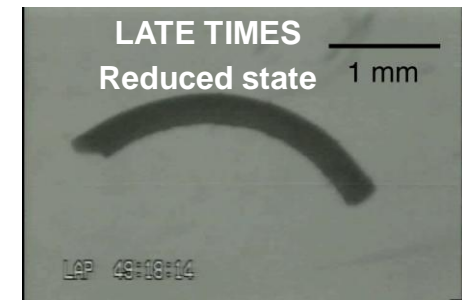
● Gels with Gradient in Crosslink Density

□ What can we learn from experiments?



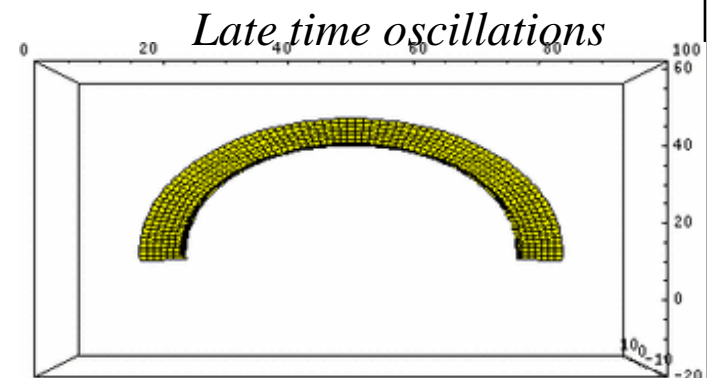
*Images are provided
by R. Yoshida et. al.*

*Kuksenok, Yoshida,
Balazs
J Mat. Chem.
21 (2011) 8360*



- ☞ Bending is smaller at early times and increases with reaction time
- ☞ Amplitude of motion of gel's ends increases with reaction time
- ☞ Sample seen to slowly move "up"

□ Simulations show qualitative agreement with experiments



Modify gLSM: Introduce Diffusion/Reaction in Solution

Activator (u) produced inside the gel only

- Diffuses to/from gel's surfaces
- Concentration in outer solution decays
 - Due to disproportionation reaction

$$\frac{du}{dt} = \nabla^2 u - u^2$$

O. Steinbock et al, Science 1995, 269, 1857

Diffusivity of u :

- Equal in solvent & outer solution

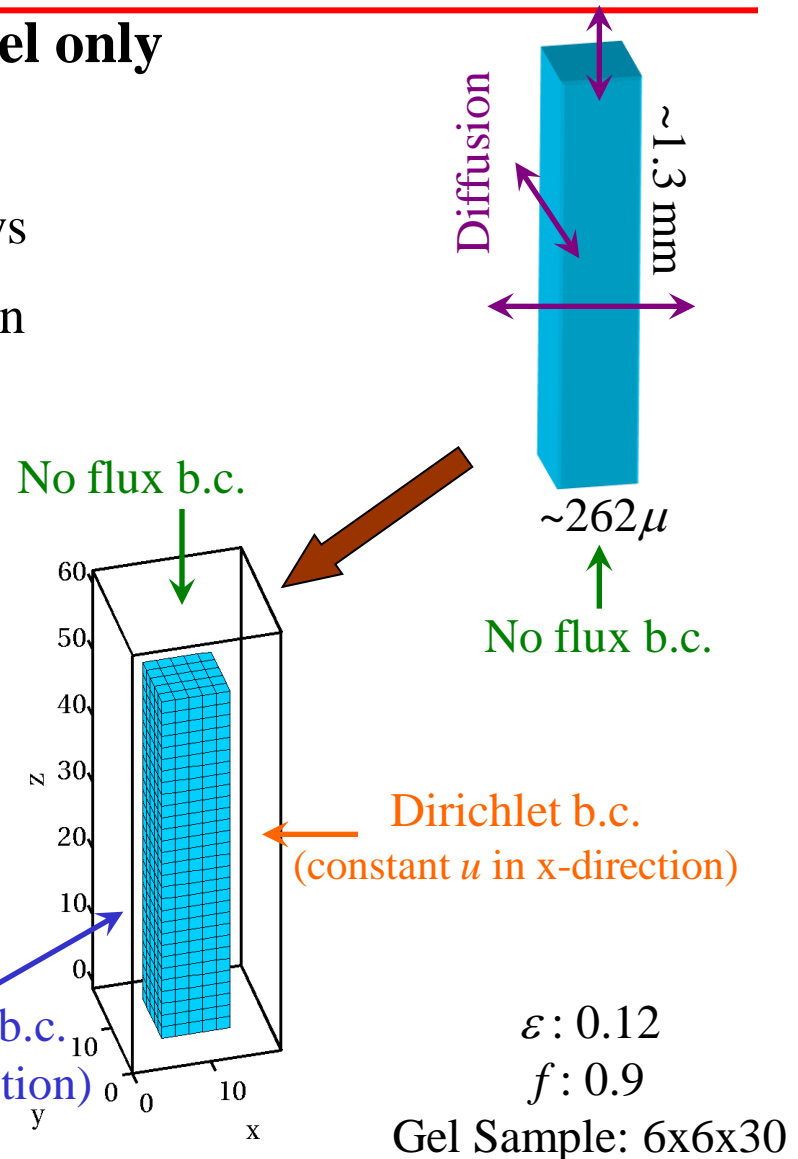
$$D = 2 \times 10^{-9} \text{m}^2/\text{s}$$

R. Yoshida et al, J. Phys. Chem. A 2001, 105, 3667

- Unit of length: $\sim 25 \mu$

- Unit of time: $\sim 0.3 \text{ s}$

P. Dayal et al, J. Mater. Chem. 2012, 22, 241



Dependence of Frequency of Oscillations on u

□ Frequency increases with increase in u at fluid boundaries

☞ Sample size: $8 \times 8 \times 8$

☞ Frequency ~ 0.032 - 0.055 Hz

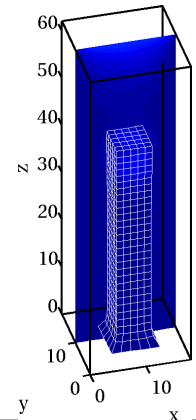
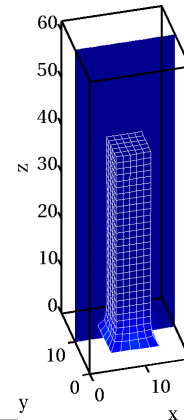
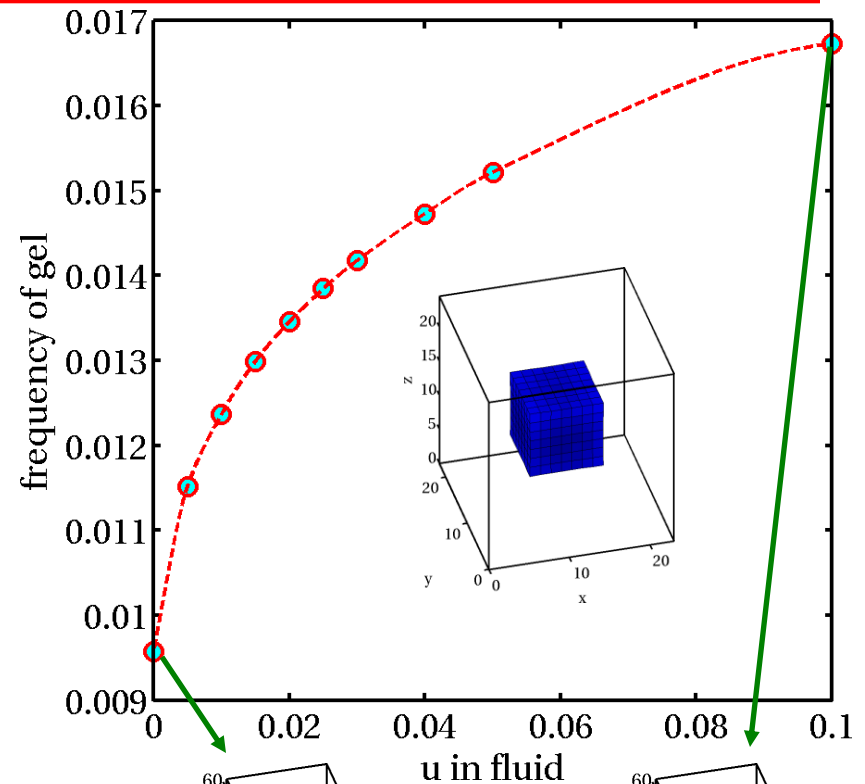
□ For longer samples

☞ Each node is an oscillator

□ Area of higher frequency dominates

☞ Sets directionality of wave propagation

☞ From higher u to lower u



Y. Kuramoto, *Chemical Oscillations, Waves, and Turbulence*

A. S. Mikhailov and A. Engel, *Phys. Lett. A* 117, 257 (1986)

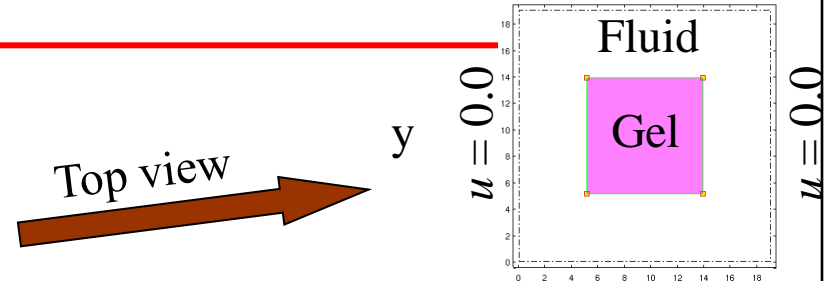
B. Blasius and R. Tonjes, *Phys. Rev. Lett.* 95, 084101 (2005)

● Wave Propagation in Single Cilium: Effect of Activator u

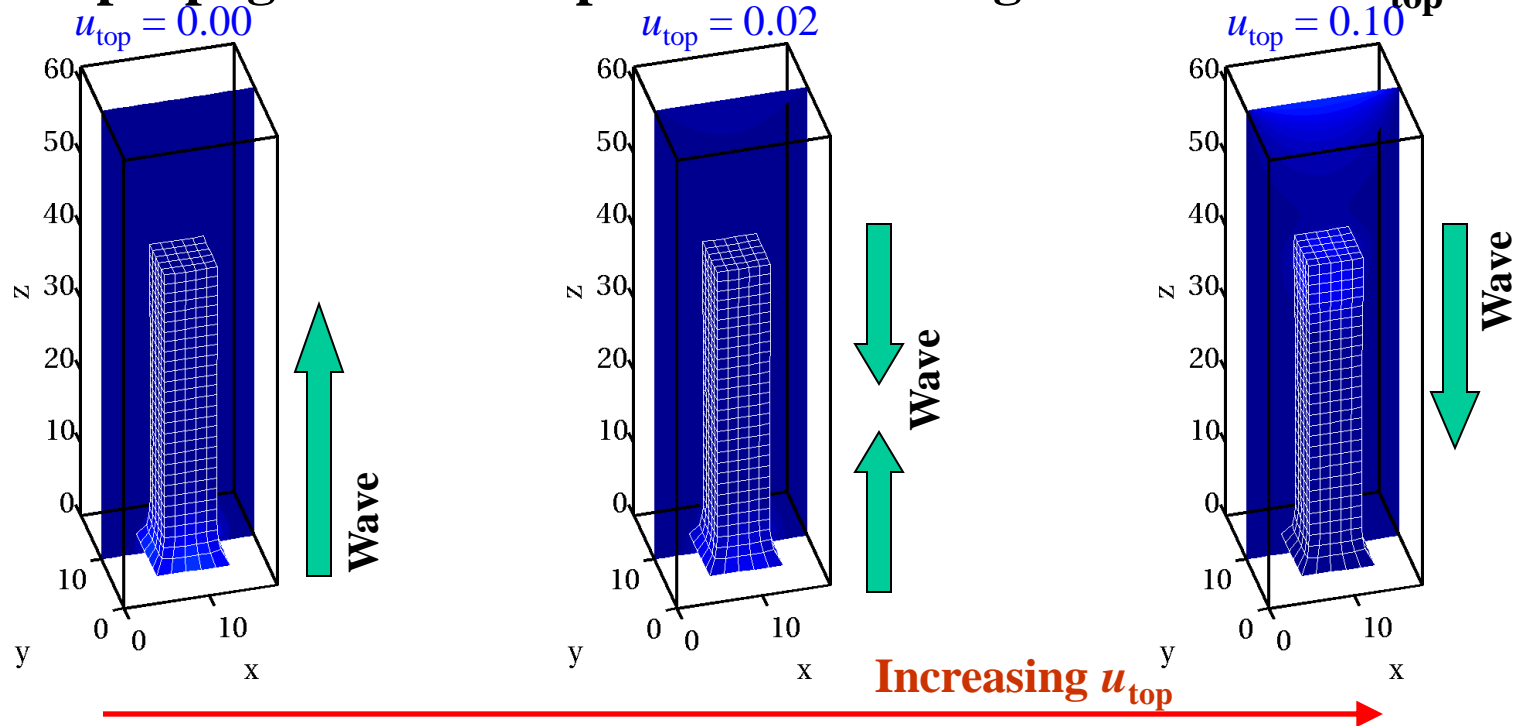
□ Boundary conditions

☞ $u = 0.0$ at $x = 0, L$

☞ $u = u_{\text{top}}$ at top of the fluid box



□ Wave propagates from top to bottom at higher values of u_{top}



P. Dayal et al, J. Mater. Chem. 2012, 22, 241

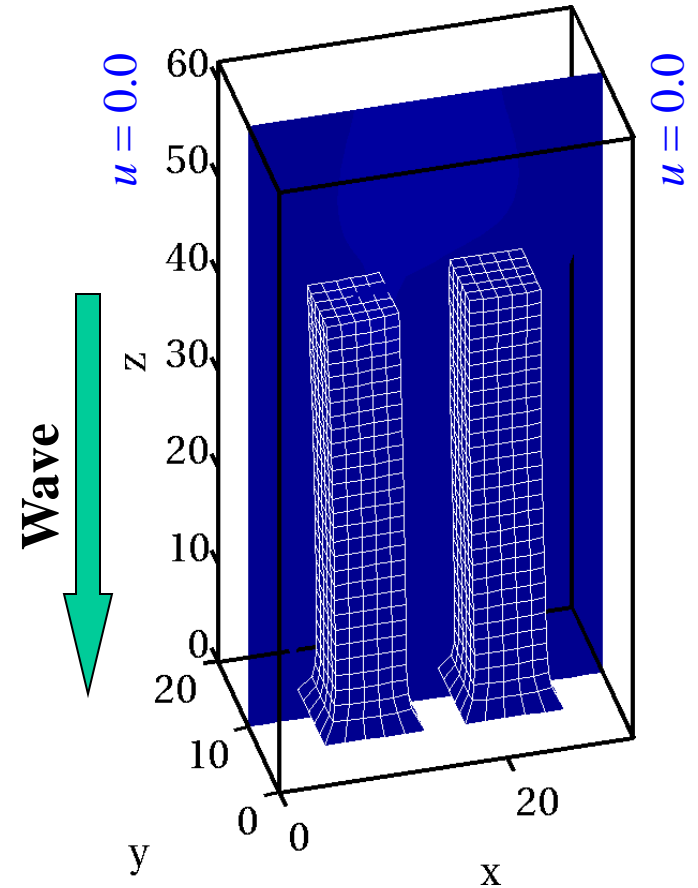
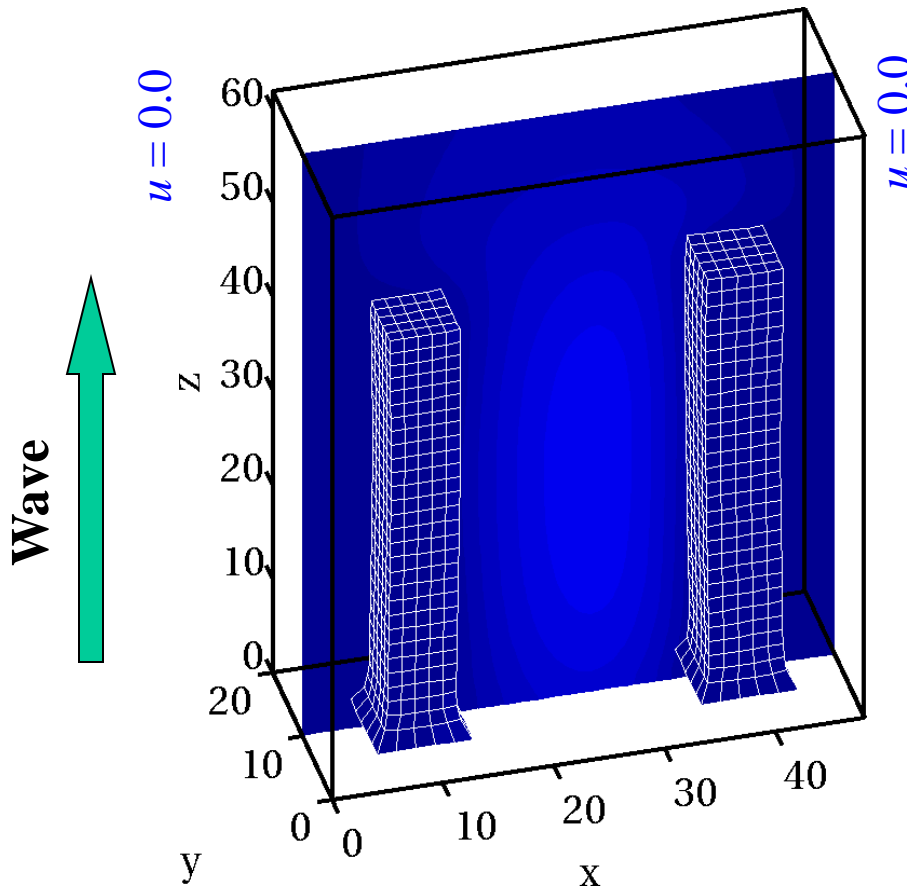
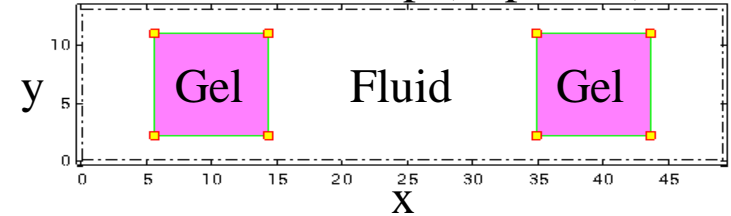
□ Activator concentration changes direction of wave propagation

Two Cilia: Effect of Spacing

Decrease spacing between cilia

- Change direction of wave propagation

Initial Setup (Top view)



● Two Cilia: Distribution of Activator u

□ Directionality of wave propagation

☞ Determined by local distribution of u

□ Cilia spaced close together

☞ Highest u concentration above cilia

☞ Wave propagates top-down

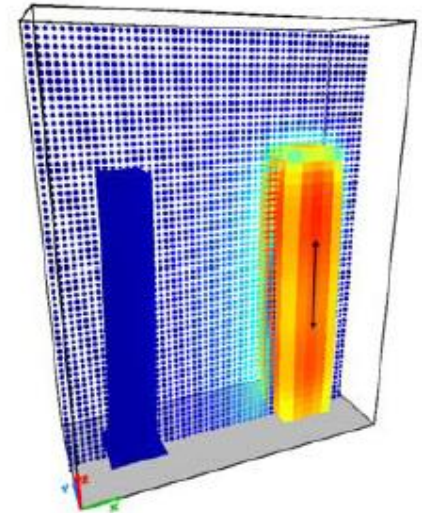
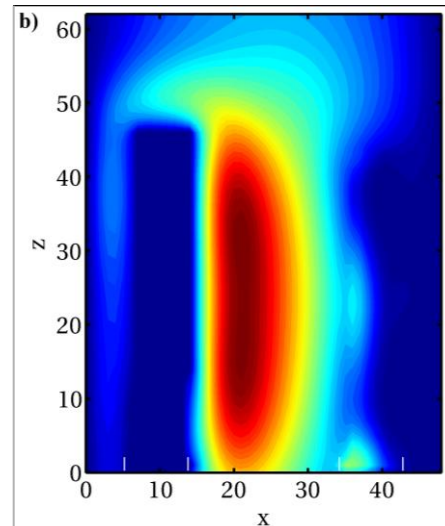
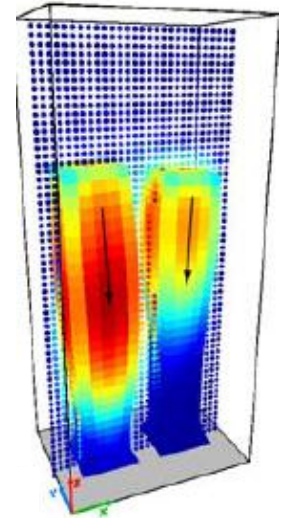
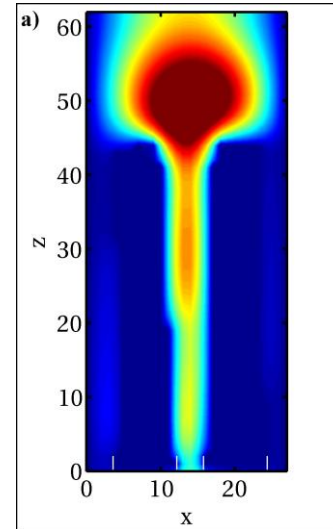
□ Cilia spaced further apart

☞ Highest u concentration between cilia
at midpoint of each gel

☞ Wave propagates from
center of each cilium

□ Control directionality of wave propagation

☞ By varying spacing



Communication Between Five Cilia

□ Boundary conditions

☞ $u = 0.0$ at $x = 0, x = L$

□ At early times

☞ Wave travels from bottom to top

□ At late times

☞ Wave travels from top to bottom

☞ Cilia bends towards center

☞ Highest concentration of u

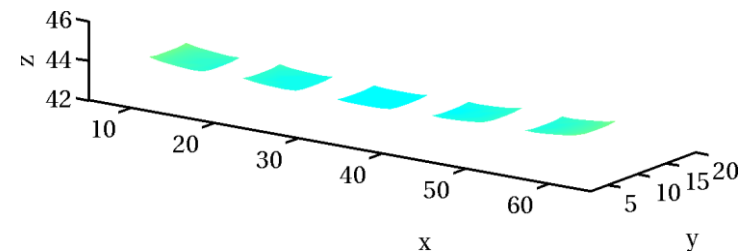
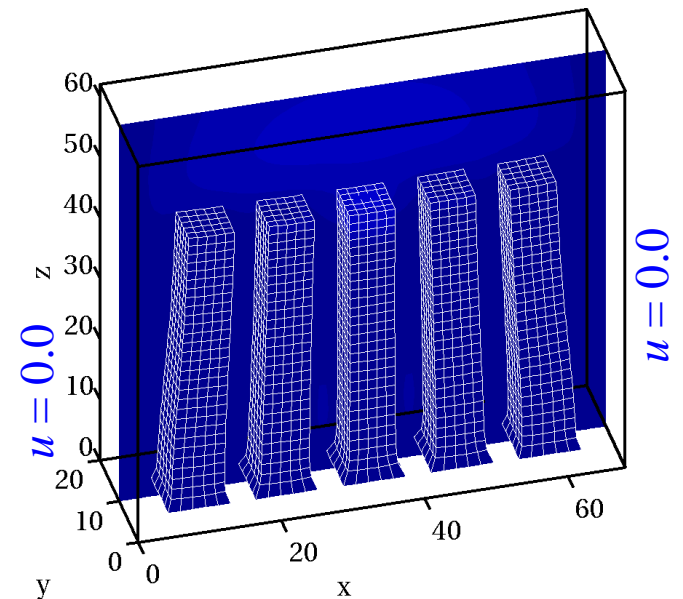
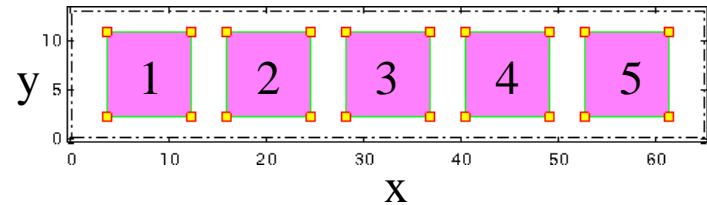
□ Multiple cilia exhibit collective behavior

☞ Wave in cilium 3 leads

☞ Higher concentration of u

☞ Oscillations are synchronized

Initial Setup (Top view)



● Exploit Photosensitivity of BZ Reaction

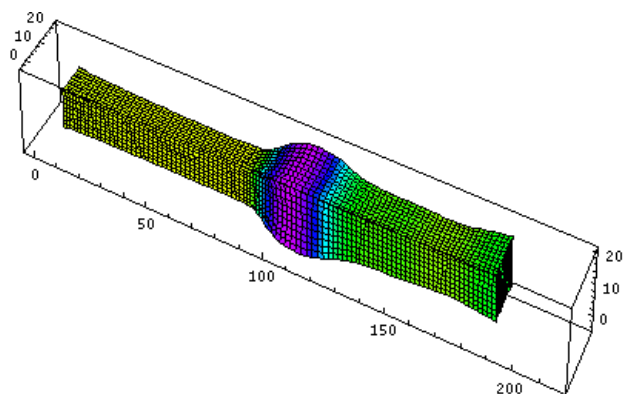
- ❑ Ruthenium-catalyzed BZ reaction photosensitive
- ❑ Introduce external light source of specific wavelength (~ 450 nm)

- ☞ Increases production of bromide ions
- ☞ Suppresses oscillations

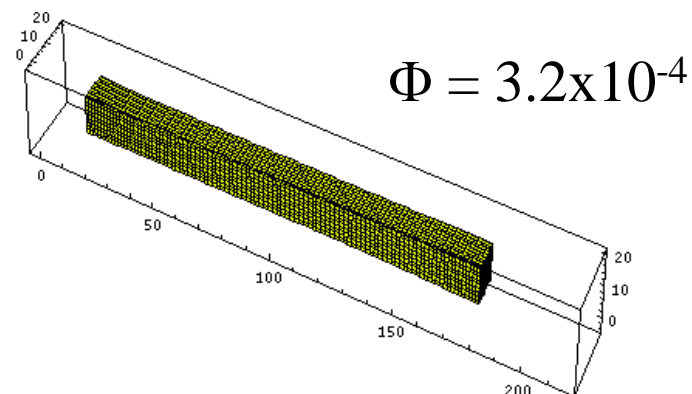
Krug, H.-J.; Pohlmann, L.; Kuhnert, L.
J. Phys. Chem. 1990, 94, 4862-4866.

$$F(u, v, \phi) = (1 - \phi)^2 u - u^2 - (1 - \phi) [fv + \Phi] \frac{u - q(1 - \phi)^2}{u + q(1 - \phi)^2}$$

- ❑ Without external light source



- ❑ With external light source



- ☞ Similar results seen experimentally

Shinohara *et al.*, *Angew. Chem. Int. Ed.* 2008, 47, 9039

Multiple Cilia: Effect of Light

□ Use light to alter dynamics

☞ Illuminate cilia 1-3

☞ $\Phi = 6 \times 10^{-4}$: Suppresses oscillations in isolated sample

□ Communication between cilia through fluid

☞ Light does not suppress oscillations in cilia 1-3

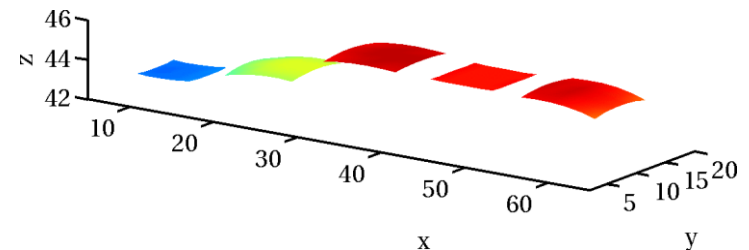
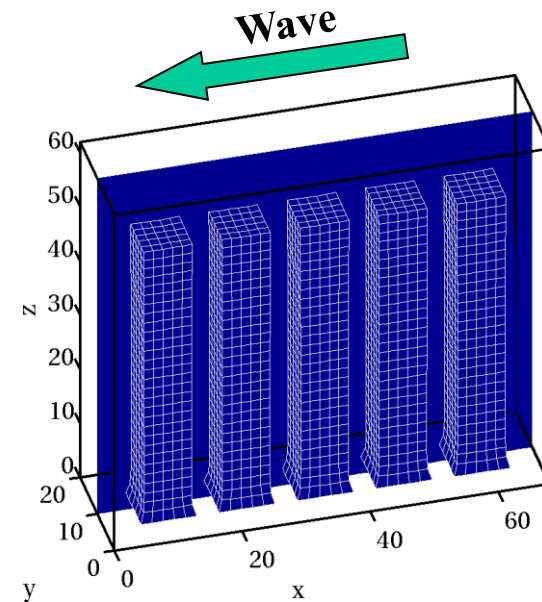
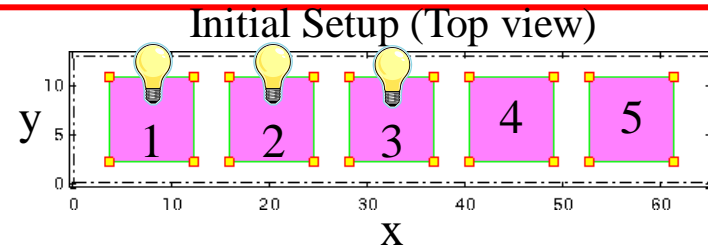
☞ Due to diffusion of u in fluid

☞ Wave originates in dark region

□ “Play” cilia like piano keyboard

☞ Address individual cilium

☞ Control collective behavior



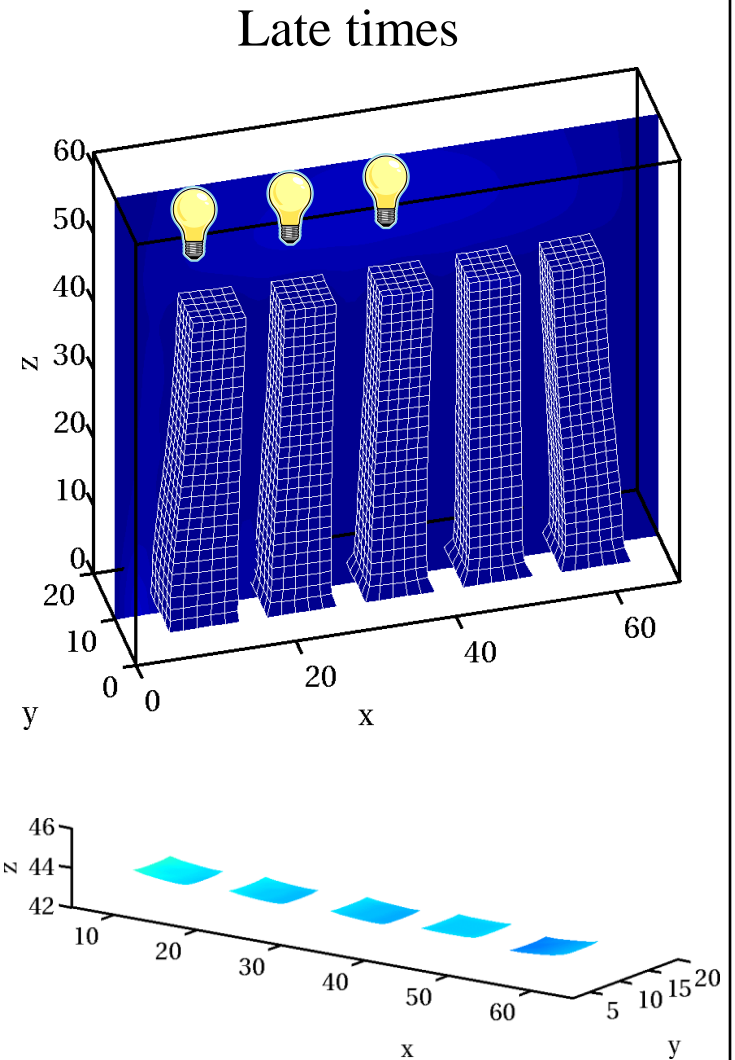
Summary

Multiple cilia exhibit collective behavior

- Oscillations synchronized
- Degree of bending determined by gradient in u
 - Cilium bends towards higher u
- Direction of wave propagation is controlled by distribution of u

Effect of light

- Provides means for remote and non-invasive control
- Changes frequency of oscillations
 - Dynamics can be controlled by non-uniform illumination



● Experimental Evidence for u -mediated Communication

- ❑ **BZ gels mechano-responsive**
 - ☞ Can drive non-oscillatory sample into oscillatory phase

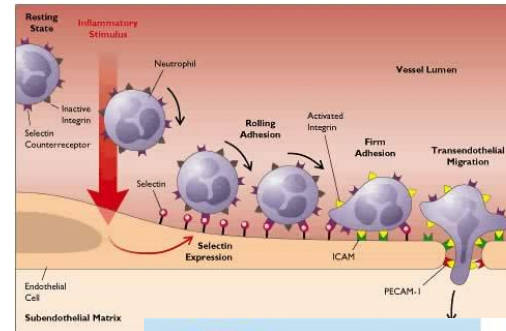
Kuksenok et al, *Soft Matter*, 5 (2009) 1835;
Soft Matter, 3 (2007) 1138; Chen, I.C., Van Vliet. K.J., et al
Adv. Func. Mat, 2012 (DOI:10.1002/adfm.201103036).
- ❑ **Exploit mechanical force as stimulus**
- ❑ **All pieces initially non-oscillatory**
- ❑ **Push on smile (through cover slip)**
 - ☞ Driven to pulsate
 - ☞ Releases u into surrounding solution
- ❑ **u diffuses to eyes**
 - ☞ Initiates oscillations in eyes
- ❑ **If eyes too far away**
 - ☞ Do not sense u
 - ☞ Do not wink



● Conclusions: Used Modeling to Design Biomimetic Systems

□ Leukocytes

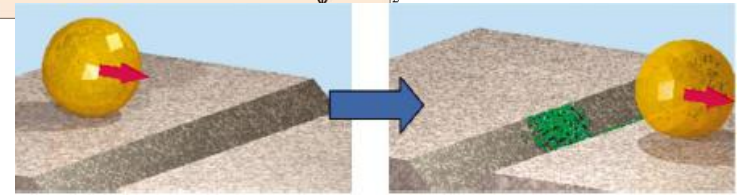
- ☞ Sense damage
- ☞ Migrate to damaged site
- ☞ Initiate repair



Leukocytes

□ Synthetic leukocytes

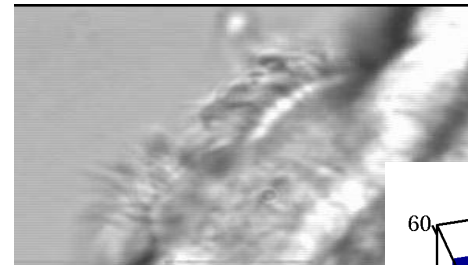
- ☞ Heal nanoscale cracks in substrates



K. Kratz et al. Nature Nano., 7 (2012) 87

□ Cilia

- ☞ Exhibit collective dynamics

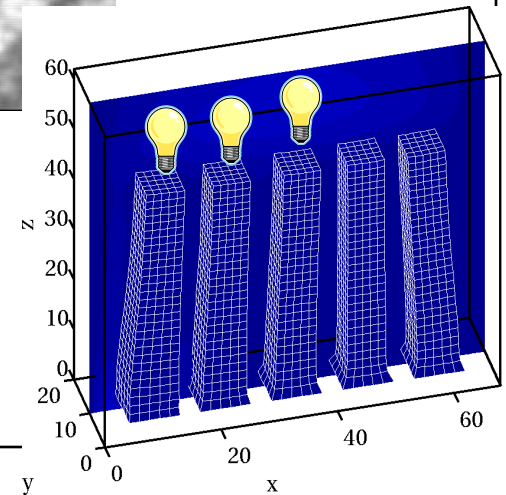


Cilia

□ Artificial cilia

- ☞ Communicate via diffusion of u
- ☞ Can be controlled by light
 - ☞ Regulate transport in microfluidic devices

P. Dayal et al, J. Mater. Chem. 22 (2012) 241



Model for Chemo-responsive Gels in 3D

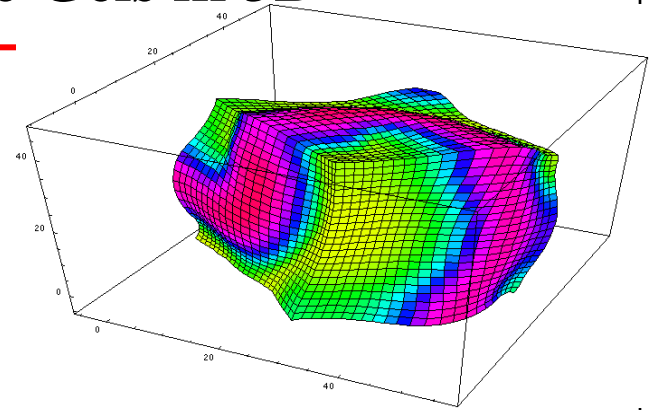
Define energy density of deformed gel

$$U = U_{el}(I_1, I_3) + U_{FH}(I_3)$$

↳ Elastic energy $U_{el} = \frac{c_0 v_0}{2} (I_1 - 3 - \ln I_3^{1/2})$

↳ Interaction energy $U_{FH} = \sqrt{I_3} [(1 - \phi) \ln(1 - \phi) + \chi_{FH}(\phi) \phi(1 - \phi) - \chi^* v(1 - \phi)]$

↳ c_0 is crosslink density, $\chi^* > 0$: hydrating effect of oxidized catalyst



Use 3D gLSM model

↳ Calculate velocities of node \mathbf{n} of element \mathbf{m}

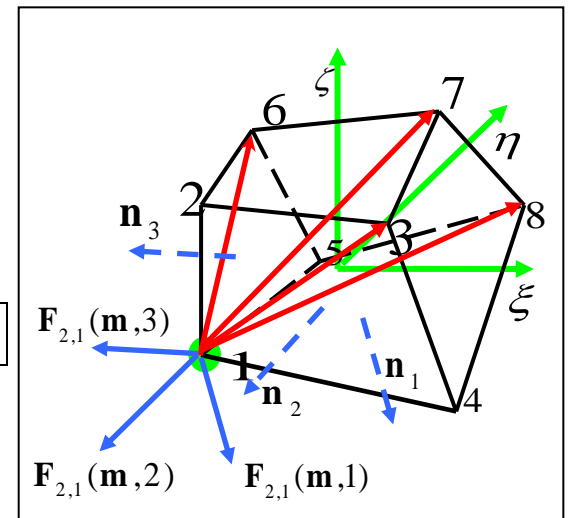
$$\frac{d\mathbf{r}_n(\mathbf{m}, t)}{dt} = M_n(\mathbf{m}, t) [F_{1,n}(\mathbf{m}, t) + F_{2,n}(\mathbf{m}, t)]$$

Spring-like

From pressure

↳ Update $v(\mathbf{m}, t)$ and $u(\mathbf{m}, t)$

↳ Combination of finite elements & finite difference techniques



O. Kuksenok et al. PRE (2008)

● Introduce Light

□ Focus on array of BZ gels attached to substrate

- ☞ Cilia communicate via diffusion of reagents
- ☞ Motion can be controlled by light

P. Dayal et al, J. Mater. Chem. 2012, 22, 241

□ Effect of visible light on BZ gels

- ☞ Enhances production of bromide ions
- ☞ Inhibits oscillations

$$I = 6.45 \text{ mW} ; \lambda = 436 \text{ nm}$$

S. Shinohara et al, Angew. Chem. 2008, 47, 9039

□ Modify reactive term in gLSM

- ☞ Additional flux of bromide ions

$$(\Phi \propto I)$$

