

# Deriving the Neural Code from Single Neuron Dynamics

Michael Famulare  
University of Washington  
Department of Physics

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[famulare@uw.edu](mailto:famulare@uw.edu)

# Acknowledgements

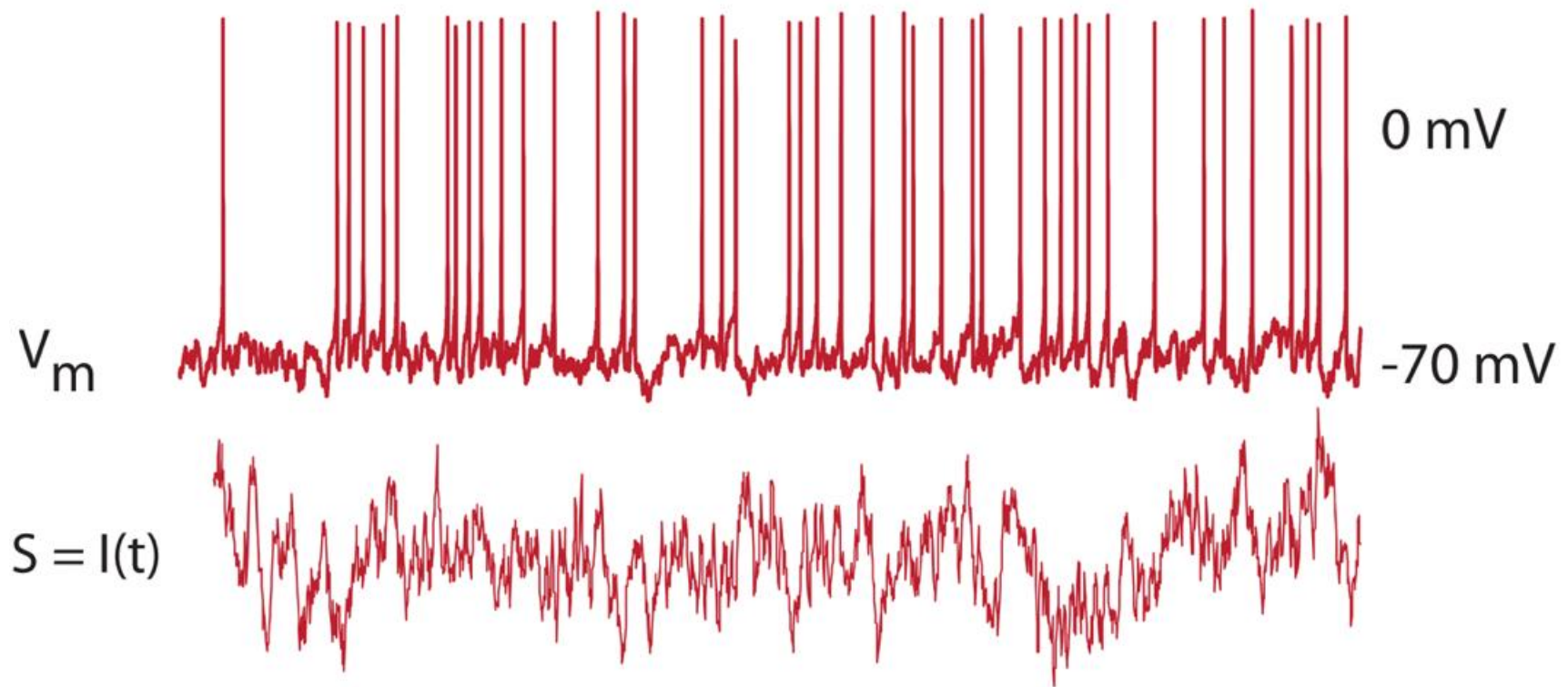
Adrienne Fairhall

Rebecca Mease

NSF

McKnight Foundation

# What does a spike represent?

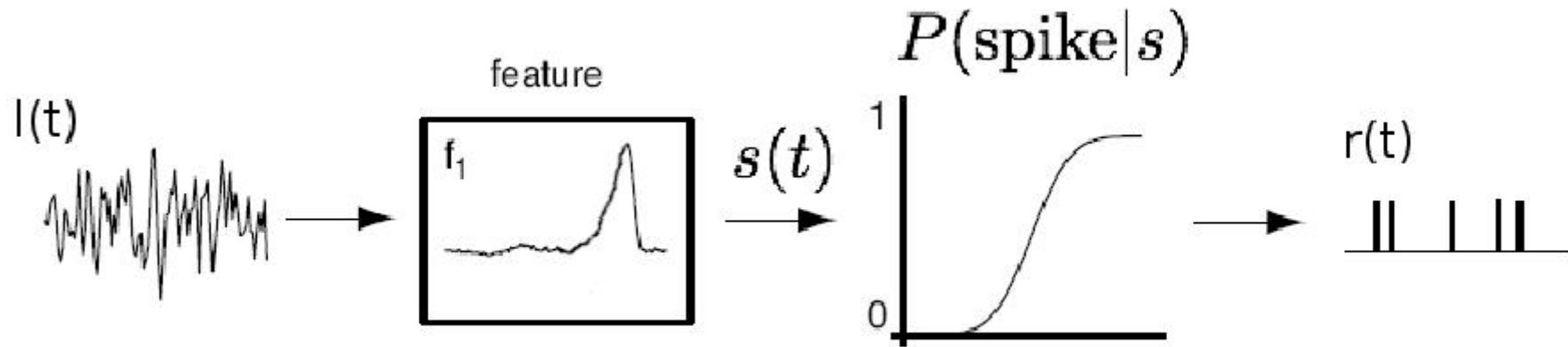


c/o R.  
Mease

1 second

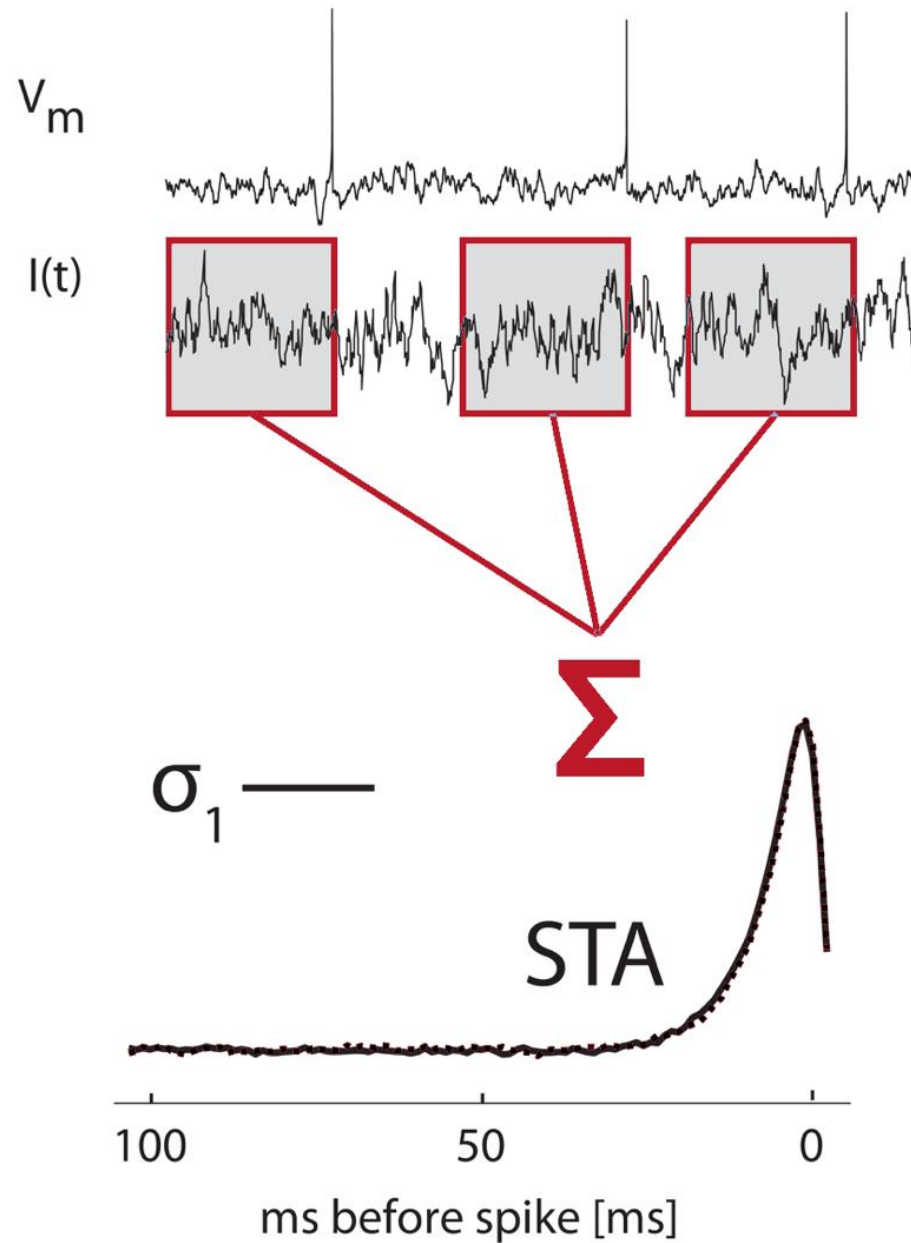
# What does a spike represent?

## **Feature Selection: LN Model**

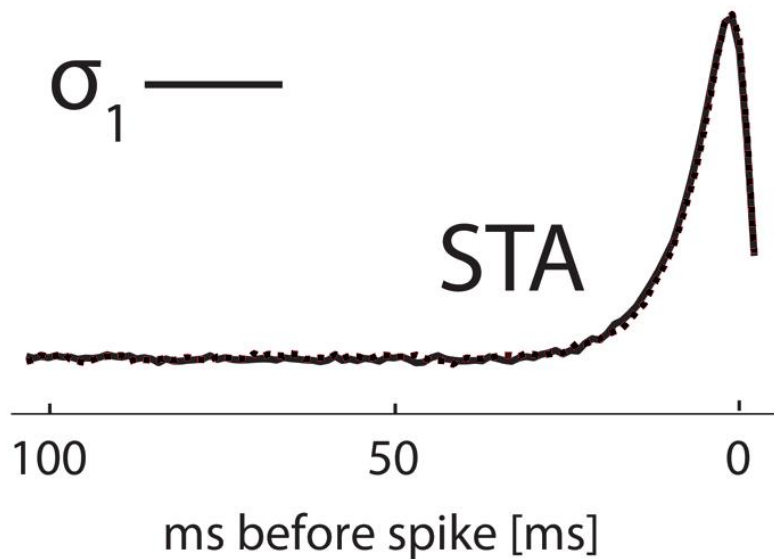


How do system dynamics determine the feature and the nonlinearity?

# What does a spike represent?

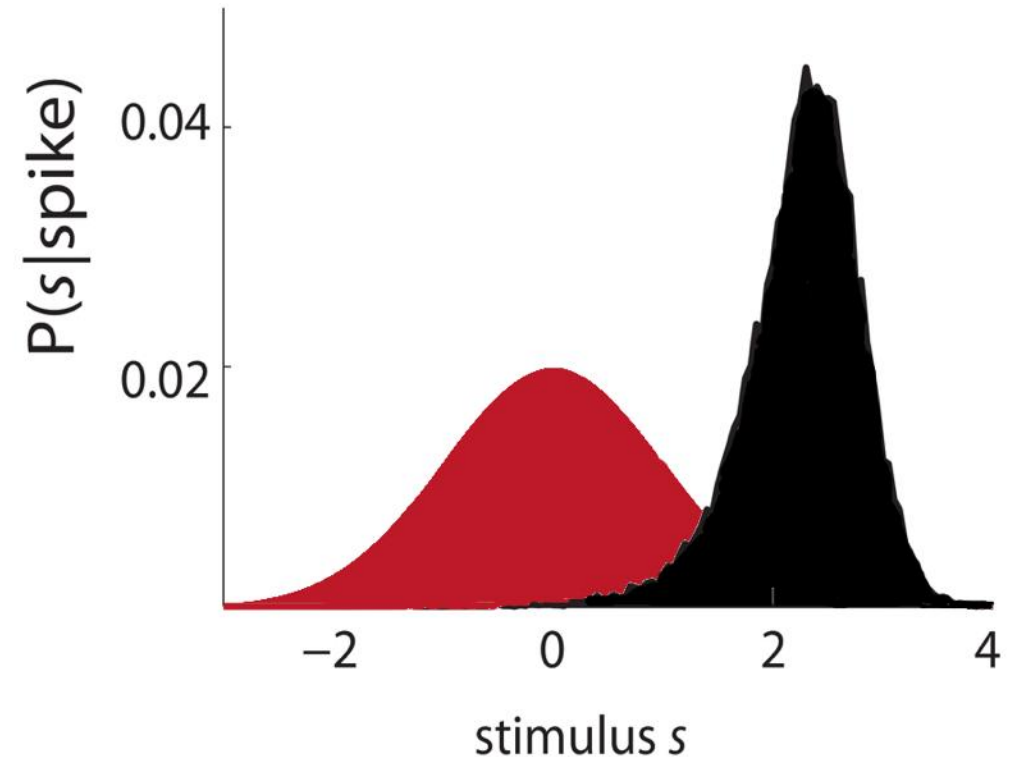


# What does a spike represent?



## Filtered stimulus

$$s(t) \equiv \text{STA}(t) * I(t - \tau)$$

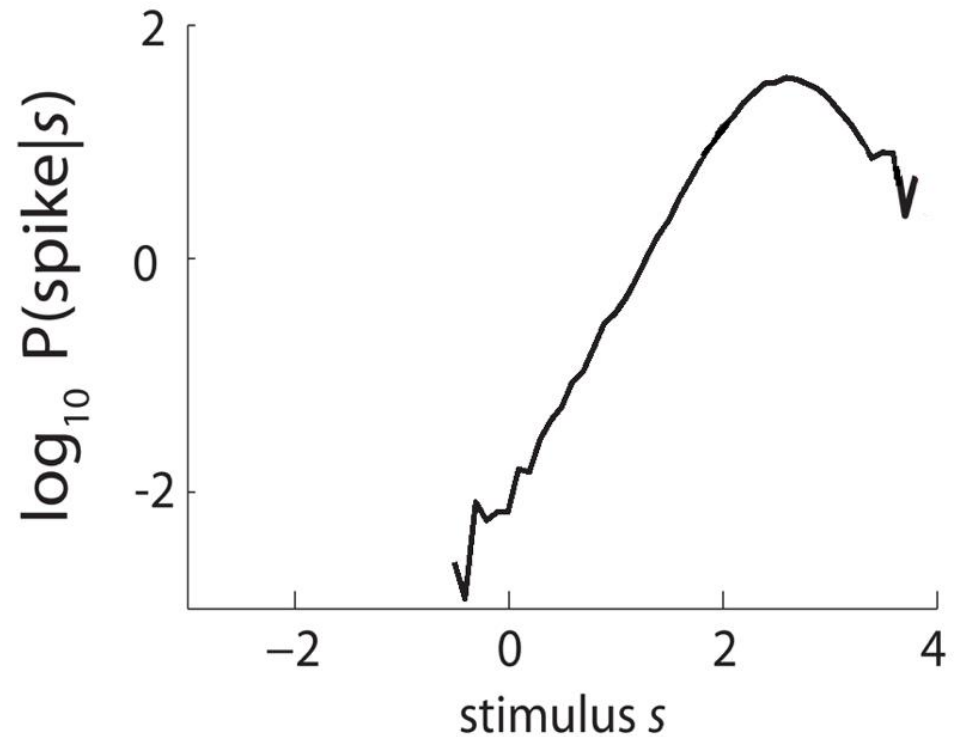
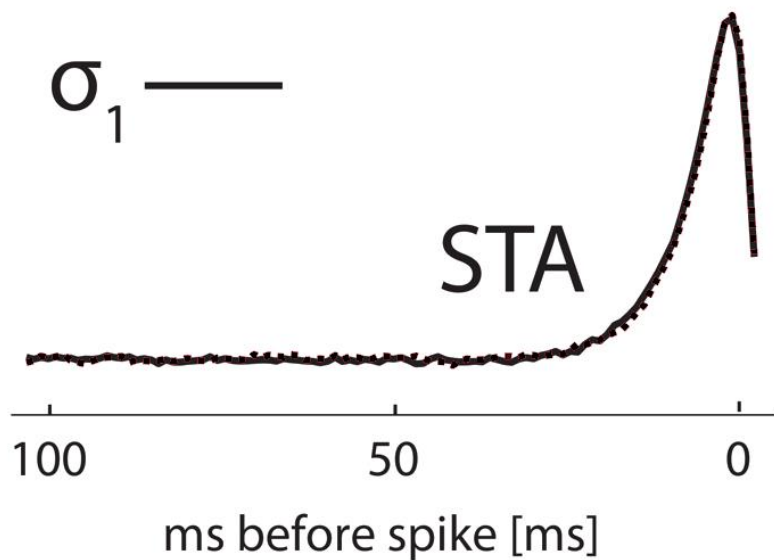


## Decision

## Function

$$P(\text{spike}|s) = \frac{p(s|\text{sp})P(\text{sp})}{p(s)}$$

# What does a spike represent?



## Filtered stimulus

$$s(t) \equiv \text{STA}(t) * I(t - \tau)$$

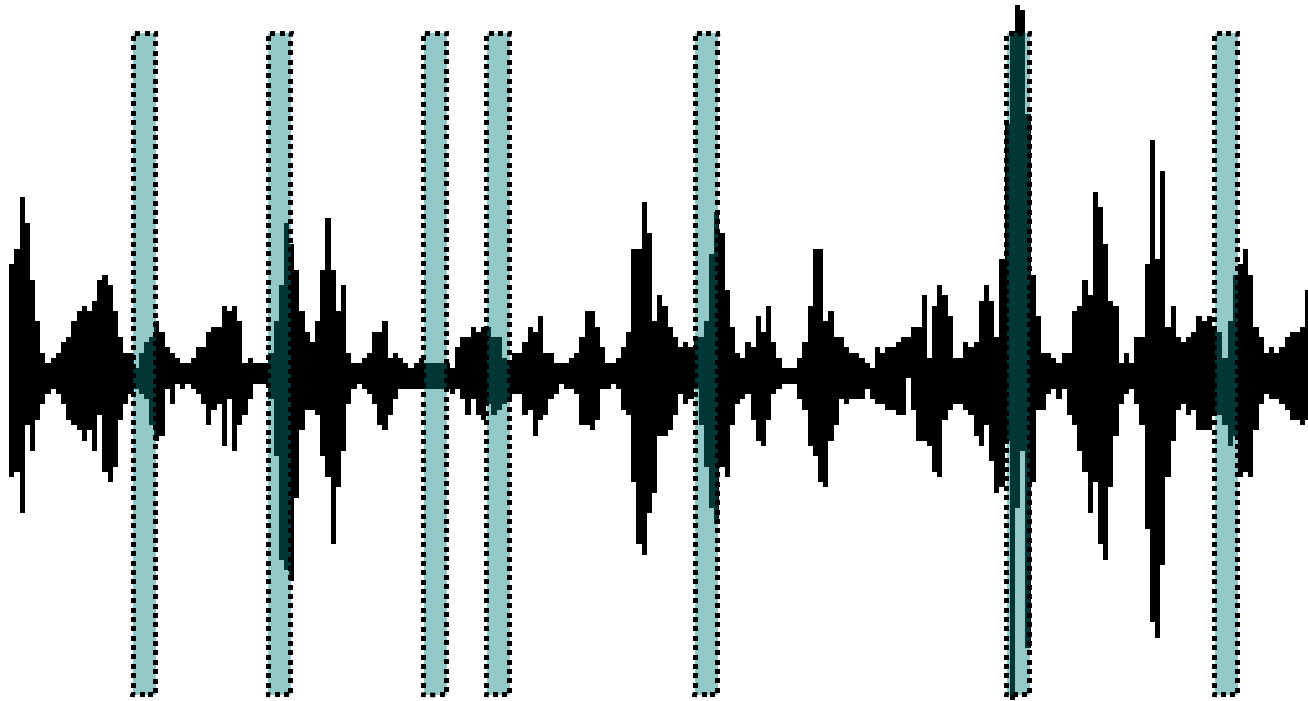
## DECISION

## Function

$$P(\text{spike}|s) = \frac{p(s|\text{sp})P(\text{sp})}{p(s)}$$

# Adaptive coding

Consider inputs with different standard deviations (different “contrast” relative to the mean)  
c/o A. Fairhall

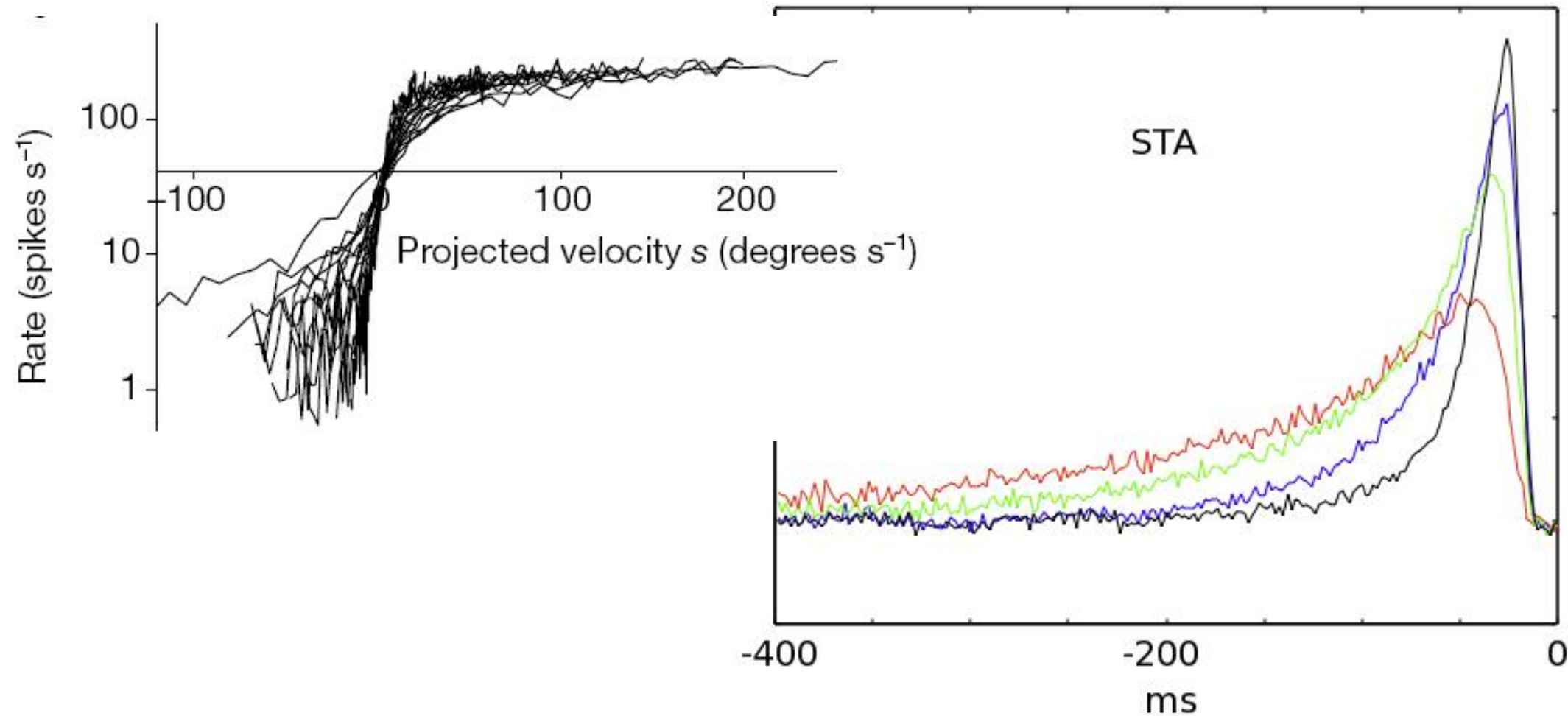


How does the code change as stimulus context varies?



# Adaptive coding

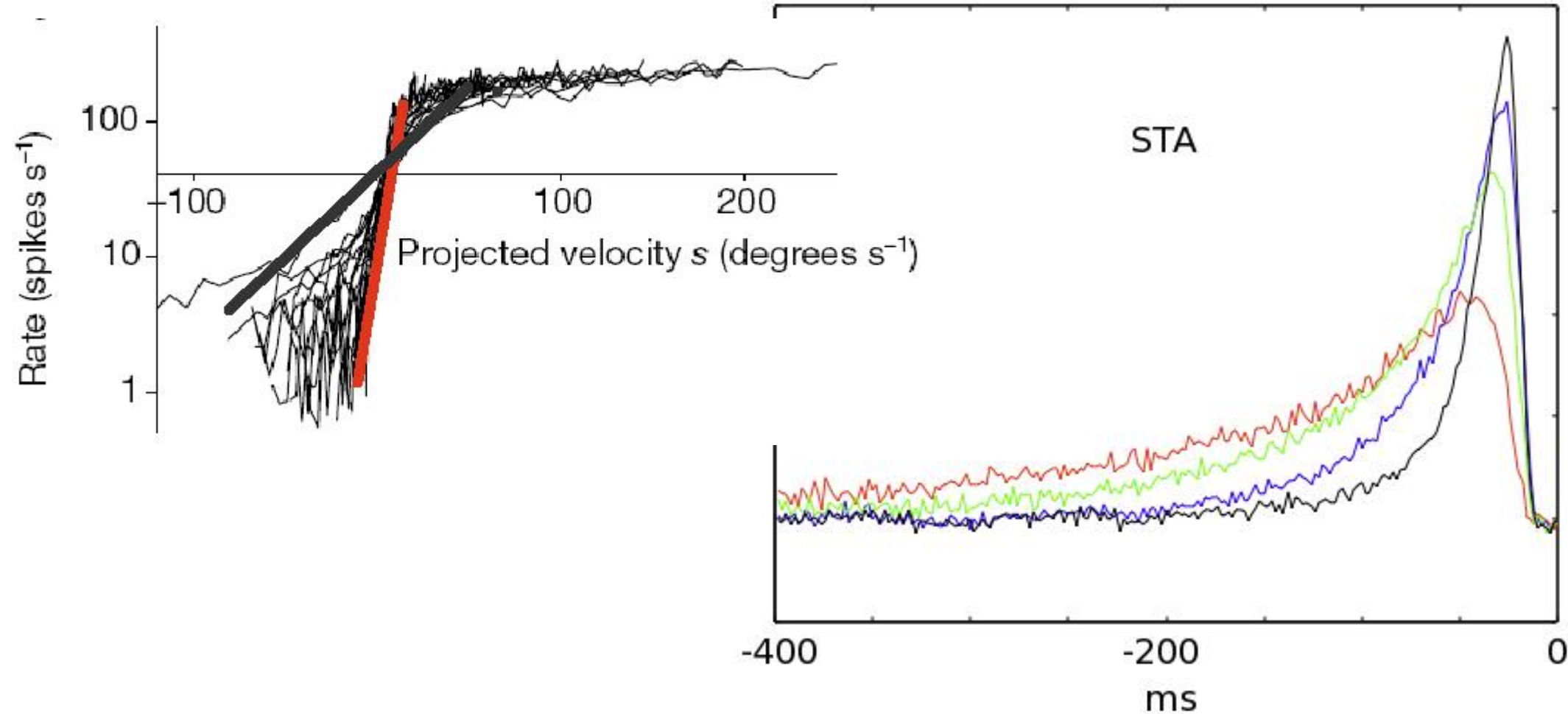
For fly neuron H1, determine the LN models locally in time throughout the stimulus presentation.



A. Fairhall, G. Lewen, R. R. de Ruyter and W. Bialek (2001)

# Adaptive coding

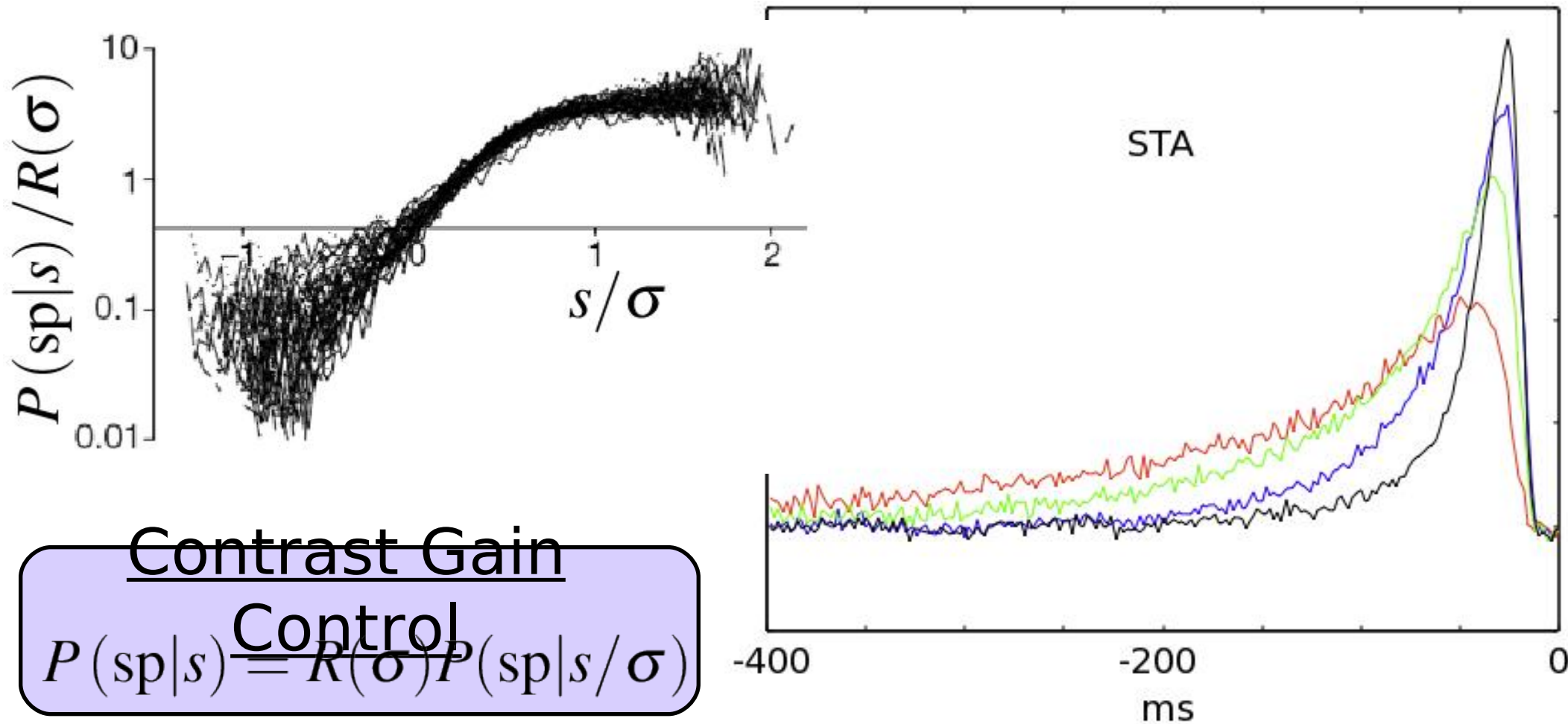
For fly neuron H1, determine the LN models locally in time throughout the stimulus presentation.



A. Fairhall, G. Lewen, R. R. de Ruyter and W. Bialek (2001)

# Adaptive coding

For fly neuron H1, determine the LN models locally in time throughout the stimulus presentation.



# Dynamical origins of the code

$$P(\text{sp}|I(t' \leq t)) = \int ds P(\text{sp}|s) p(s|I(t' \leq t))$$

$$P(\text{sp}|I(t' \leq t)) = \int \mathcal{D}\vec{v} \mathcal{D}\vec{w} \mathcal{D}\vec{x} P(\text{sp}|\vec{v}) p(\vec{v}|\vec{w}, \vec{x}, I) p(\vec{w}, \vec{x}|I(t' \leq t))$$

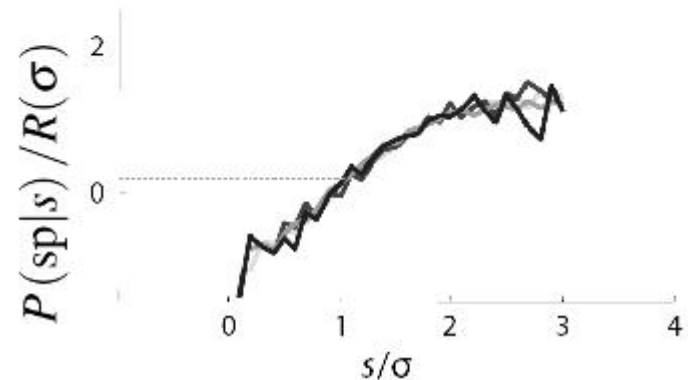
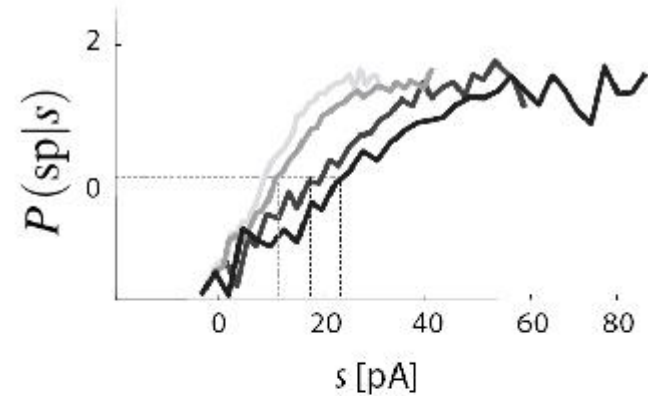
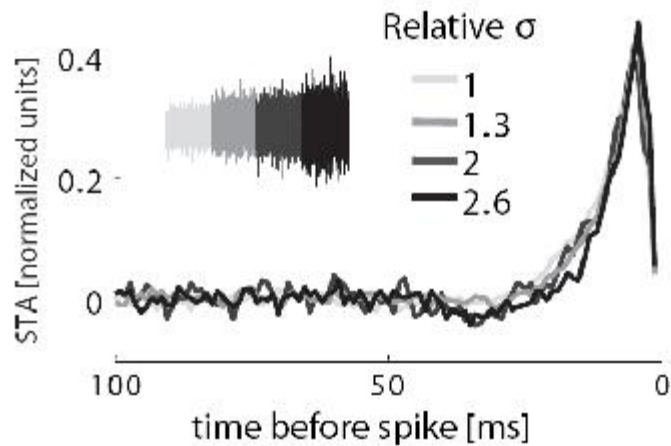
family of inputs  $\{I_{\mu, \sigma}\} \rightarrow$  family of codes  $\{P(\text{sp}|I_{\mu, \sigma}(t' \leq t))\}$

Big question for dynamics and coding:

How do you design the dynamics—the phase space and stimulus-driven flow in that space—to produce desired codes?

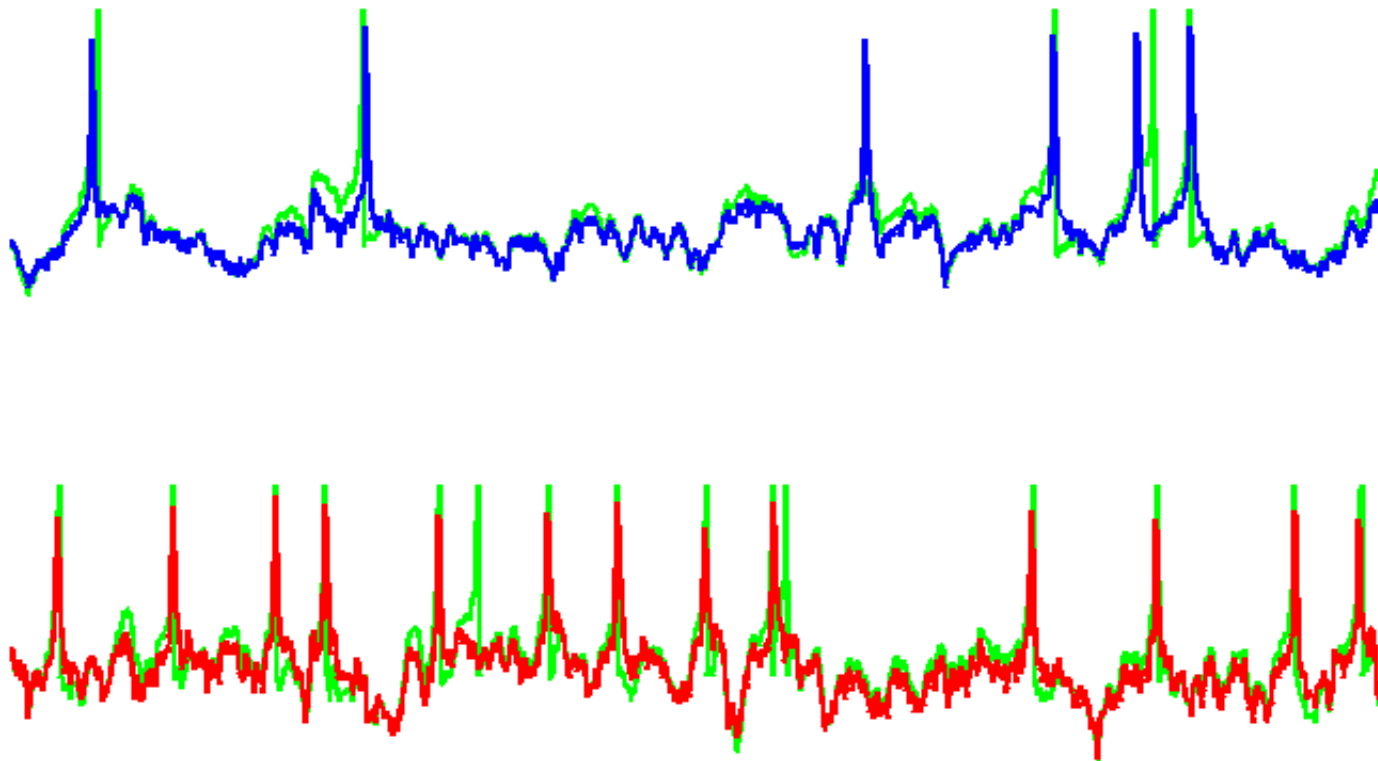
# Contrast gain control in single neurons

Mouse cortex (Mease, Moody, & Fairhall,  
submitted)

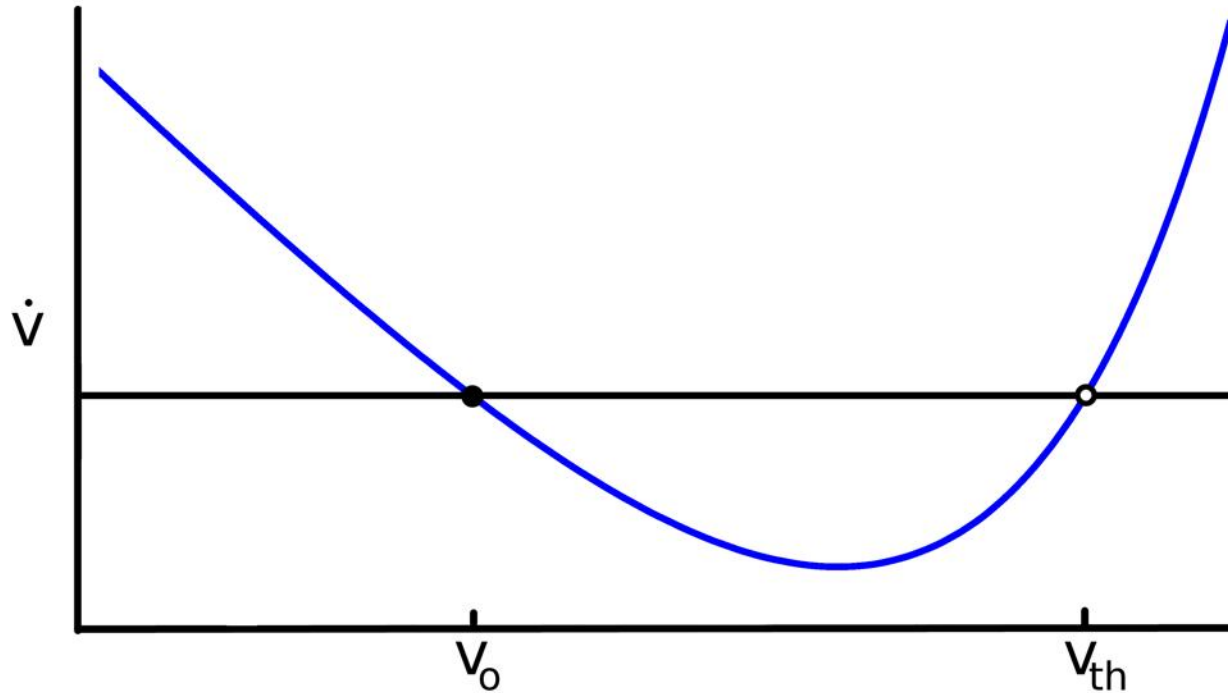


# Fast adaptation experiments are fit by an exponential IF model

Optimize fit to steady-state voltage  
distribution, STA, and coincidence factor



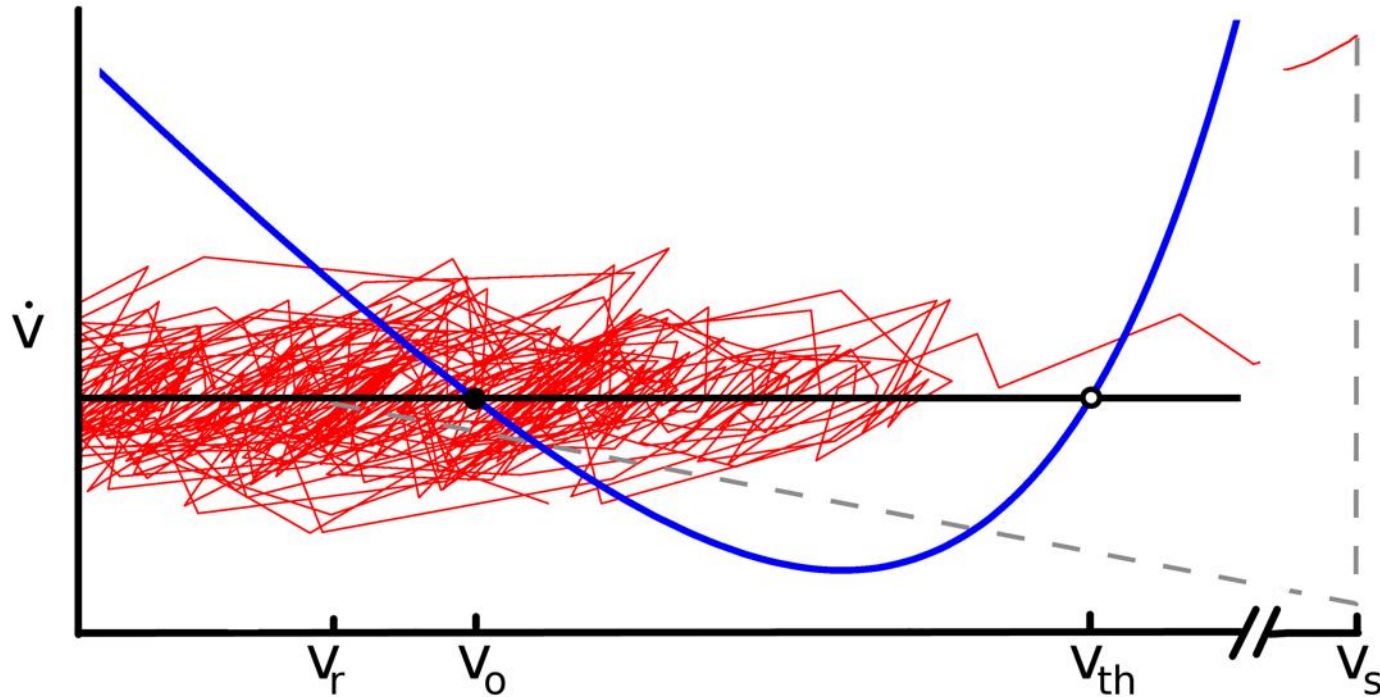
# Exponential integrate-&-fire model



$$\tau \dot{v} = -(v - v_o) + f(v) + rI(t) + (v_r - v_s) \delta(v - v_s) \tau \dot{v} H(\dot{v})$$

$$f(v) = (v_{th} - v_o) e^{\frac{v - v_{th}}{\Delta}}$$

# Exponential integrate-&-fire model



$$\tau \dot{v} = -(v - v_o) + f(v) + rI(t) + (v_r - v_s) \delta(v - v_s) \tau \dot{v} H(\dot{v})$$

$$f(v) = (v_{th} - v_o) e^{\frac{v - v_{th}}{\Delta}}$$



# LN model code from the EIF

$$P(\text{sp}|I(t' \leq t)) = \int \mathcal{D}v P(\text{sp}|v) p(v|I(t' \leq t))$$

LN Model:

$$P(\text{sp}|I(t' \leq t)) = \int ds P(\text{sp}|s) p(s|I(t' \leq t))$$

$$p(s(t)|I(t' \leq t)) = \delta(s - \text{STA} * I)$$

Dynamics in LN model form:

$$P(\text{sp}|I(t' \leq t)) = \int ds \int \mathcal{D}v P(\text{sp}|v) p(v|s) p(s|I(t' \leq t))$$

# LN model code from the EIF

Decision function from dynamics:

$$P(\text{sp}|s) = \int \mathcal{D}v P(\text{sp}|v) p(v|s)$$

$$P(\text{sp}|s) = \int dv_{(t-h)} \int dv_{(t)} P(\text{sp}|v_{(t-h)}, v_{(t)}) p(v_{(t-h)}, v_{(t)}|s_{(t)})$$

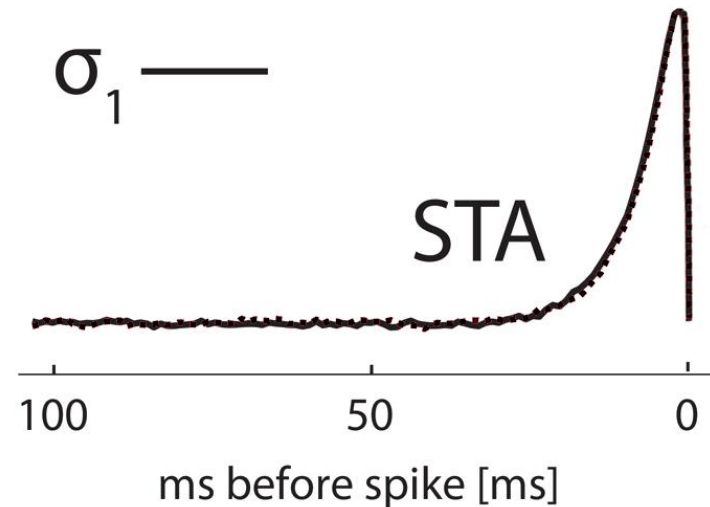
Defining spike times

$$P(\text{sp}|v_{(t-h)}, v_{(t)}) = \mathbb{H}(v_{th} - v_{(t-h)}) \mathbb{H}(v_{(t)} - v_{th})$$

Voltage estimation problem

$$p(v_{(t-h)}, v_{(t)}|s_{(t)}) = p(v_{(t-h)}|v_{(t)}, s_{(t)}) p(v_{(t)}|s_{(t)})$$

# Modeling the filtered stimulus



For everything we talk about today, the STA is monotonic and approximately exponential

$$s(t) \equiv \text{STA}(t) * I(t - \tau)$$

$$\tau \dot{s} = -ks + I(t)$$

# Voltage from filtered stimulus?

infer voltage from filtered stimulus

infer voltage from filtered stimulus  
infer input variable from white noise  $s(t)$  to colored noise  $I(t)$

$$G(v) = f(v) + (v_r - v_s)\delta(v - v_s)\tau\dot{v}H(\dot{v})$$

$$\tau\dot{v} = -(v - v_o) + G(v) + I(t)$$

$$\tau\dot{s} = -ks + I(t)$$

# Voltage from filtered stimulus?

infer voltage from filtered stimulus

infer voltage from filtered stimulus  $s(t)$  to color  $I(t)$

$$G(v) = f(v) + (v_r - v_s)\delta(v - v_s)\tau\dot{v}H(\dot{v})$$

$$\tau(\dot{v} - \dot{s}) = -(v - s) + v_o + (k - 1)s + G(v)$$

$$v(t) \approx v_o + s(t) + \int_0^t \frac{dt'}{\tau} e^{\frac{t'-t}{\tau}} (k - 1)s(t')$$

$$+ \int_0^t \frac{dt'}{\tau} e^{\frac{t'-t}{\tau}} G\left(v_o + s(t') + \int_0^{t'} \frac{dt''}{\tau} e^{\frac{t''-t'}{\tau}} ((k - 1)s(t''))\right)$$

# Best linear estimator

$$v(t) = v_o + s(t) + \text{Mess}[s(t' \leq t)]$$

$$v(t) \sim v_o + s(t) - s_o$$

We want to find a statistically optimal linear approximation to the voltage dynamics below threshold

$$p(s) = \sqrt{\frac{k}{\pi\sigma^2}} \exp\left[\frac{-k}{\sigma^2}(s - s_o)^2\right]$$

$$p(v) \propto \exp\left(\frac{-(v - v_o)^2 + 2\int f(v)}{\sigma^2}\right) \int_{\max(v, v_r)}^{v_s} dv' \exp\left(\frac{(v' - v_o)^2 - 2\int f(v')}{\sigma^2}\right)$$

# Minimizing the KL- divergence

$$D_{KL}(v||s) = \int dv p(v) \ln \frac{p(v)}{p(s)}$$

Measures the “distance” between two distributions.

We are only interested in getting below-threshold statistics correct.

$$\tilde{D} = \int_{-\infty}^{v_{th}} dv p(v|v \leq v_{th}) \ln \frac{p(v|v \leq v_{th})}{p(s)}$$

$$k = \frac{\sigma^2/2}{\text{Var}[v|v \leq v_{th}]}$$
$$s_o = \text{E}[v|v \leq v_{th}]$$

# Optimal Filter Intuition

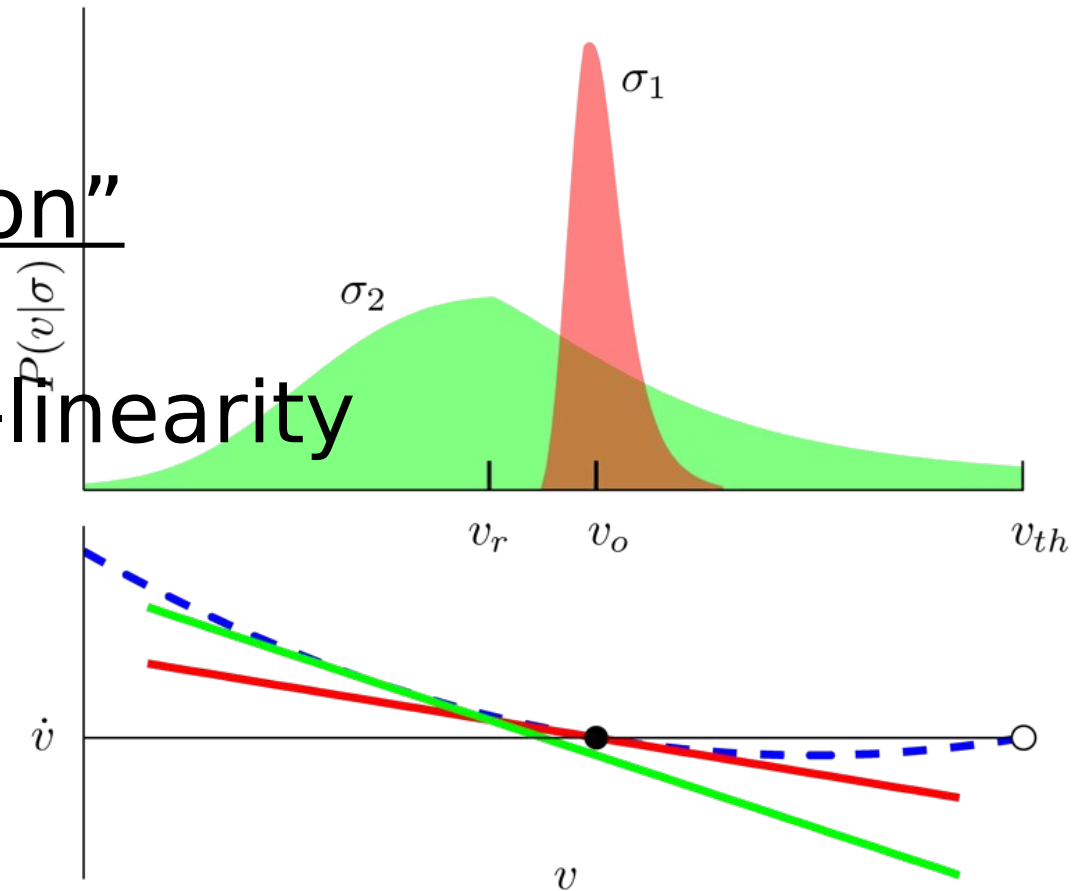
$s$  should be a good linear estimator of the voltage

$$k = \frac{\sigma^2/2}{\text{Var}[v|v \leq v_{th}]}$$

Two sources of “adaptation”

ing of sub-threshold non-linearity  
us- & spike-driven

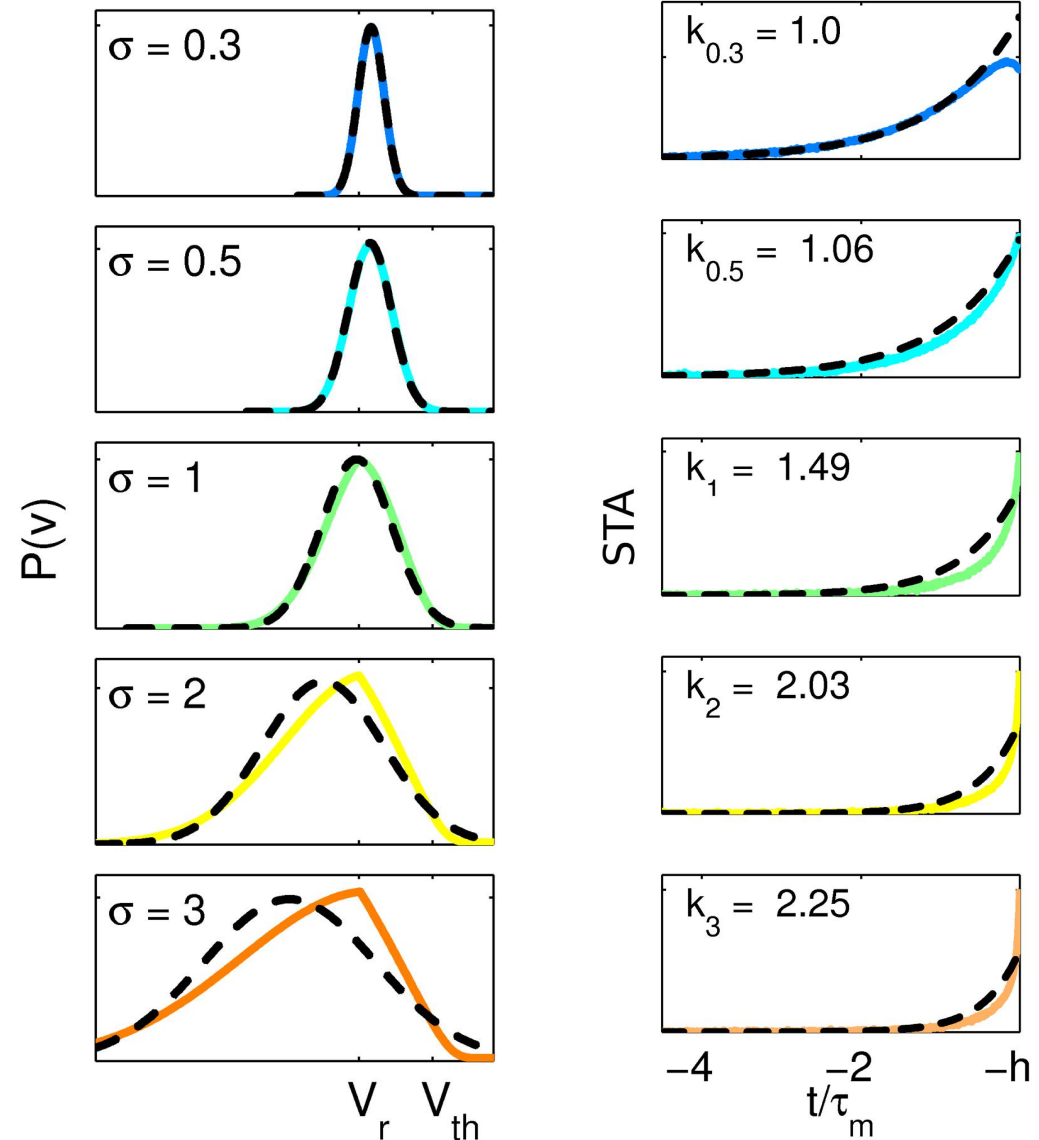
“tting” due to spiking





# Stochastic Linearization Results

$$k = \frac{\sigma^2/2}{\text{Var}[v|v \leq v_{th}]}$$



# Voltage given filtered stimulus

We just saw how the filter time constant  $k$  is roughly determined by the subthreshold voltage statistics.

Given the filter, to derive the LN coding model, we need to understand  $p(v(t)|s(t))$ .

We have  $v[s(t' \leq t)]$

We can study  $p(v(t)|s(t))$  via its moments.

# First Moment

We have:  $v[s(t' \leq t)]$

We want:  $\langle v(t)|s(t) \rangle = \langle v[s(t' \leq t)] \rangle_{\{s(t' < t)|s(t)\}}$

$s$  is an OU-process, so everything about its moments are known.

Expand, average, and re-sum

$$\begin{aligned} \langle v(t)|s(t) \rangle = & v_o + \frac{2k}{k+1}s(t) + f(v_o) \left( \frac{\Delta(k+1)}{2ks(t)} \right) \left( e^{\left(\frac{2ks(t)}{\Delta(k+1)}\right)} - 1 \right) \\ & - (v_s - v_r) \int_0^t dt' e^{\frac{t'-t}{\tau}} R(t'|s(t)) + \mathcal{O}(\sigma^2) \end{aligned}$$

# Deriving contrast gain control

Recall the definition of the decision function:

$$P(\text{sp}|s) = \int \mathcal{D}v P(\text{sp}|v) p(v|s)$$

By definition, a neuron that exhibits perfect contrast gain control obeys:

$$P(\text{sp}|s) = R(\sigma) P(\text{sp}|s/\sigma)$$

This implies that all moments of the voltage given the filtered stimulus must be of the form:

$$\langle (v_{th} - v(t))^n | s(t) \rangle = \sigma^n \mu_n(s/\sigma)$$

# Intuition for contrast gain control

To the Board!

# Constraints for gain control

$$\langle v(t) | s(t) \rangle = v_o + \frac{2k}{k+1} s(t) + f(v_o) \left( \frac{\Delta(k+1)}{2ks(t)} \right) \left( e^{\left( \frac{2ks(t)}{\Delta(k+1)} \right)} - 1 \right) - (v_s - v_r) \int_0^t dt' e^{\frac{t'-t}{\tau}} R(t' | s(t)) + \mathcal{O}(\sigma^2)$$

For gain control, the EIF model must be tuned such that:

$$\langle (v_{th} - v(t)) | s(t) \rangle = \sigma \mu_1(s/\sigma)$$

Can't ever be strictly true!  
Approximately?

# Constraints for gain control

On average, to approximate perfect contrast gain control, the neuron must exhibit

$$1 \gg f(v) \text{ below threshold}$$

$$\bar{R} = \frac{c\sigma - (v_{th} - v_o)}{\tau(v_s - v_r)}$$

Intuition:

sub-threshold dynamics should minimize distortion of the input distribution

rate feedback tunes typical distance to threshold to scale with standard deviation

$$v_{th} - \langle v | v \leq v_{th} \rangle \propto \sigma$$

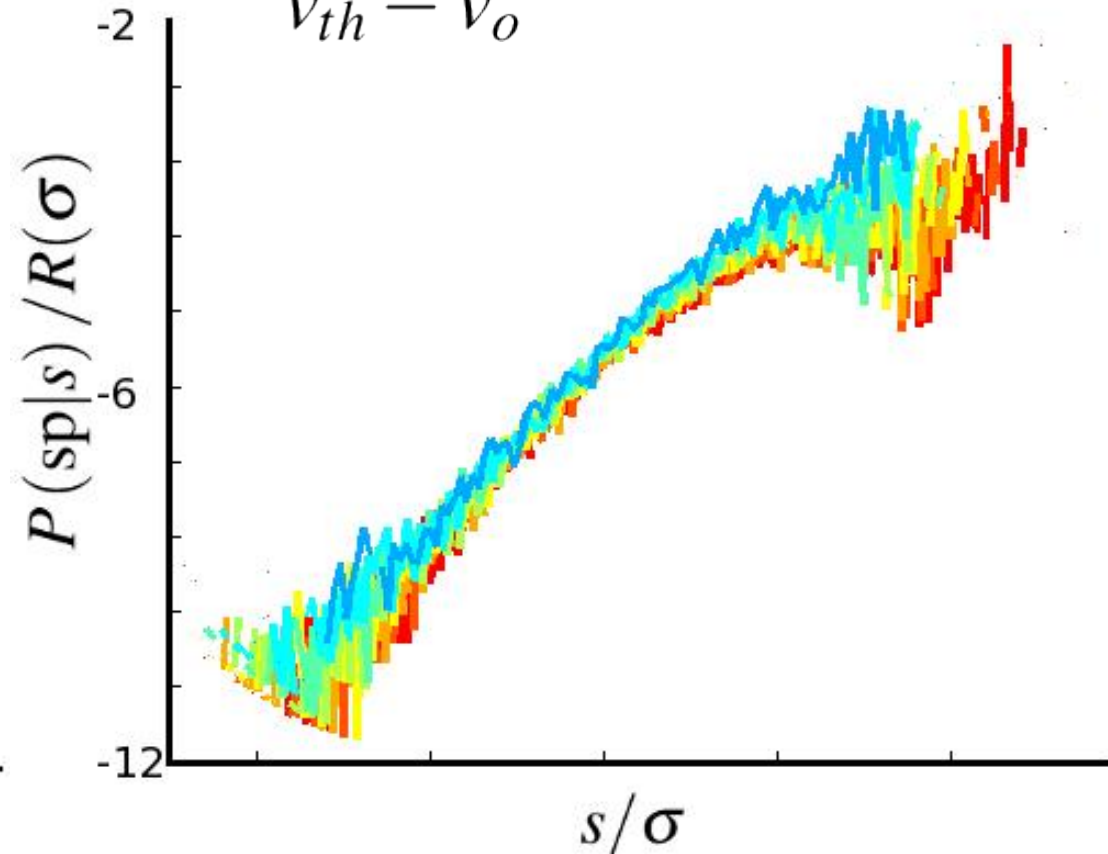
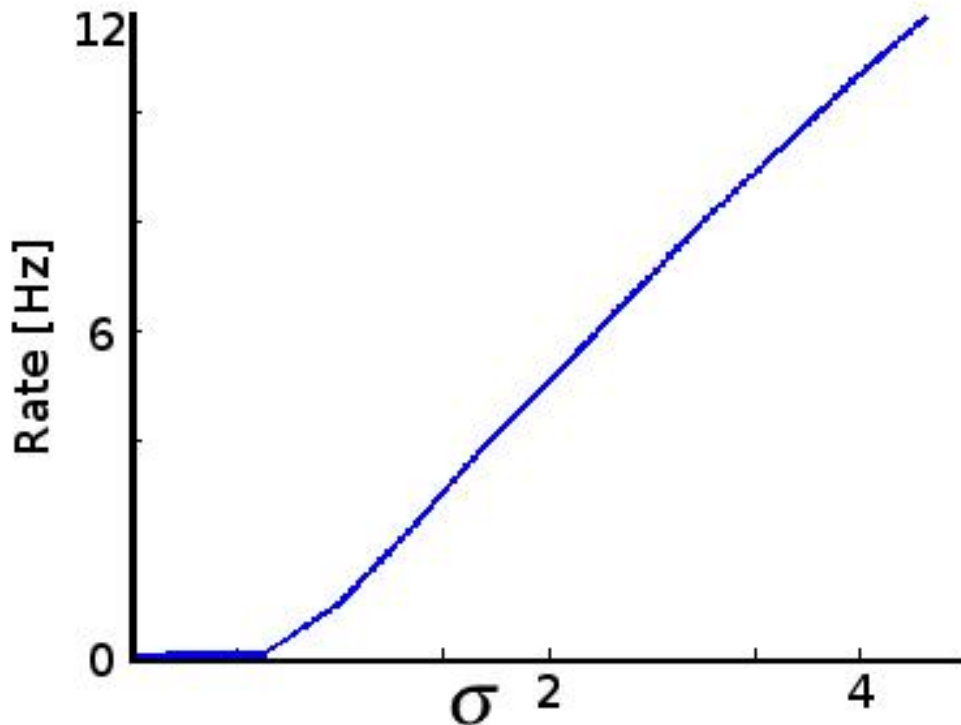
# EIF simulation results

EIF has 7 parameters, 5 of which are determined by choosing units.

To optimize linearity of firing rate:

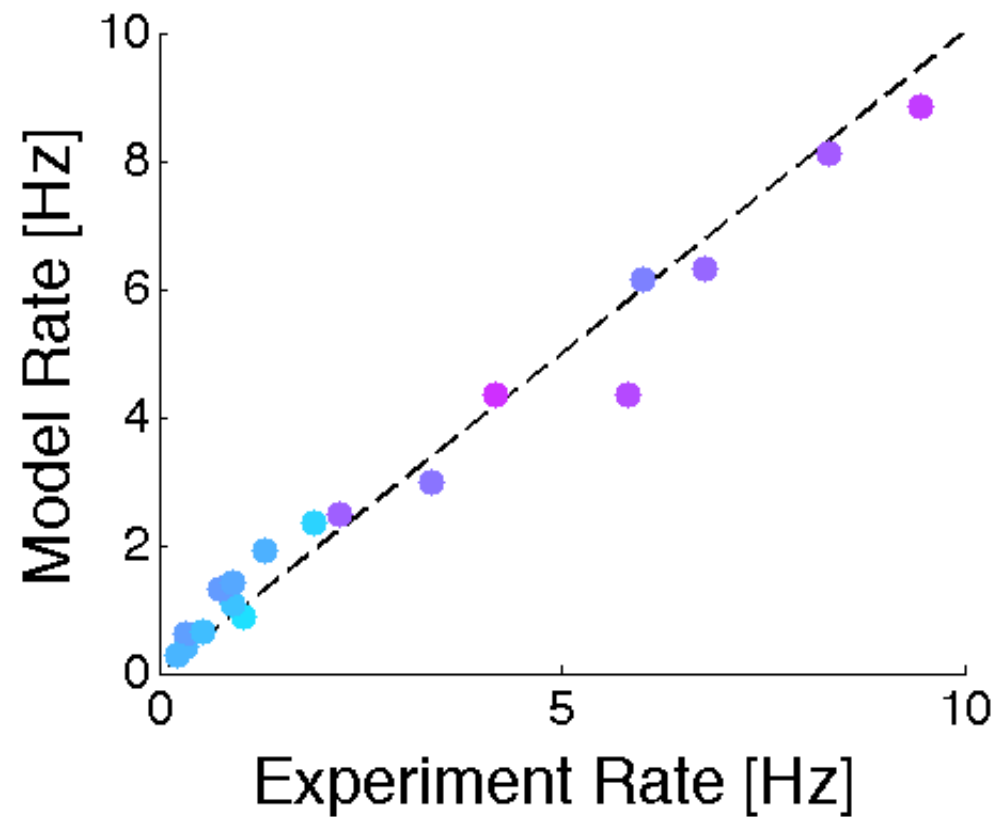
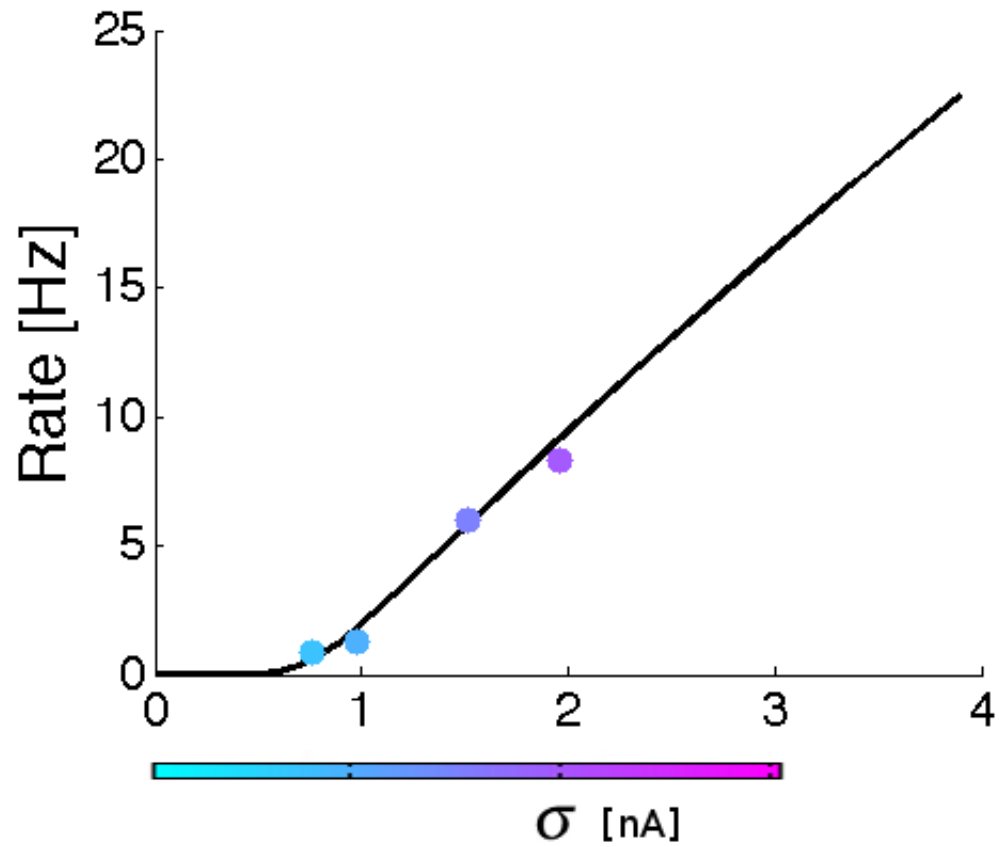
$$\frac{v_{th} - v_o}{\Delta} \approx 2.7$$

$$\frac{v_o - v_r}{v_{th} - v_o} \approx 0.2$$



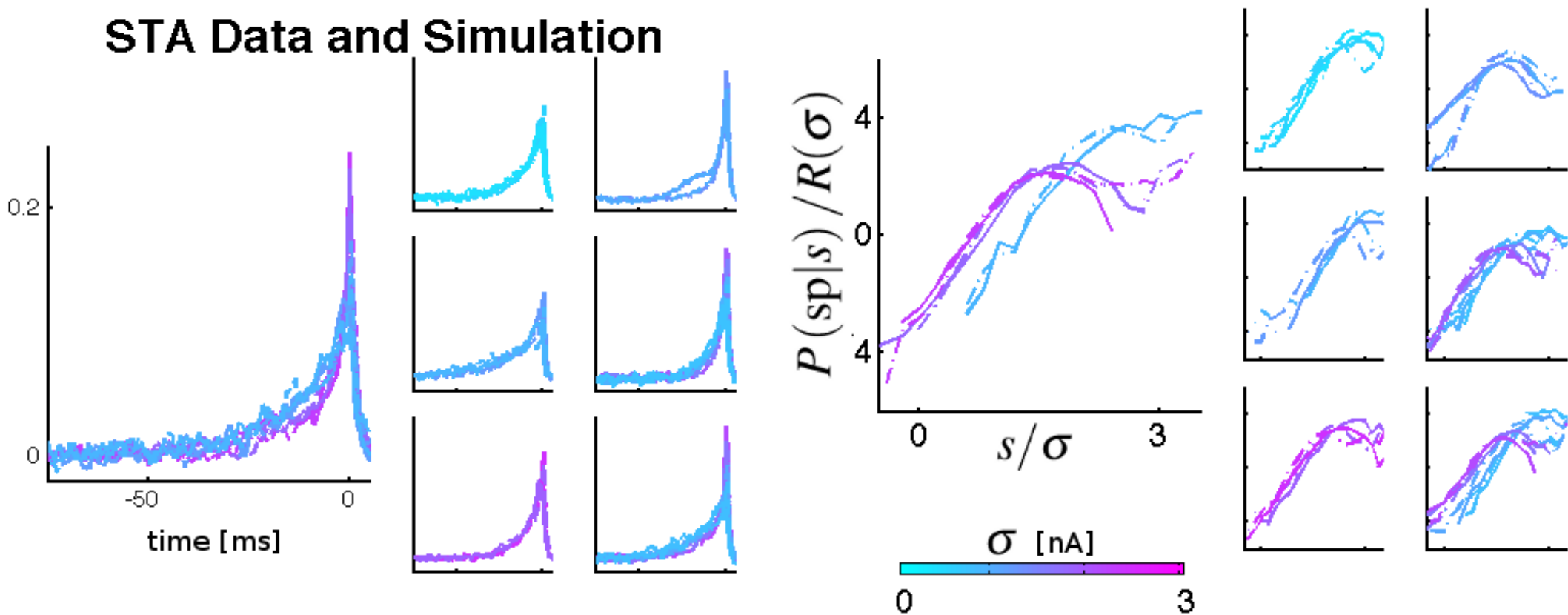


# Rate and LN model comparison



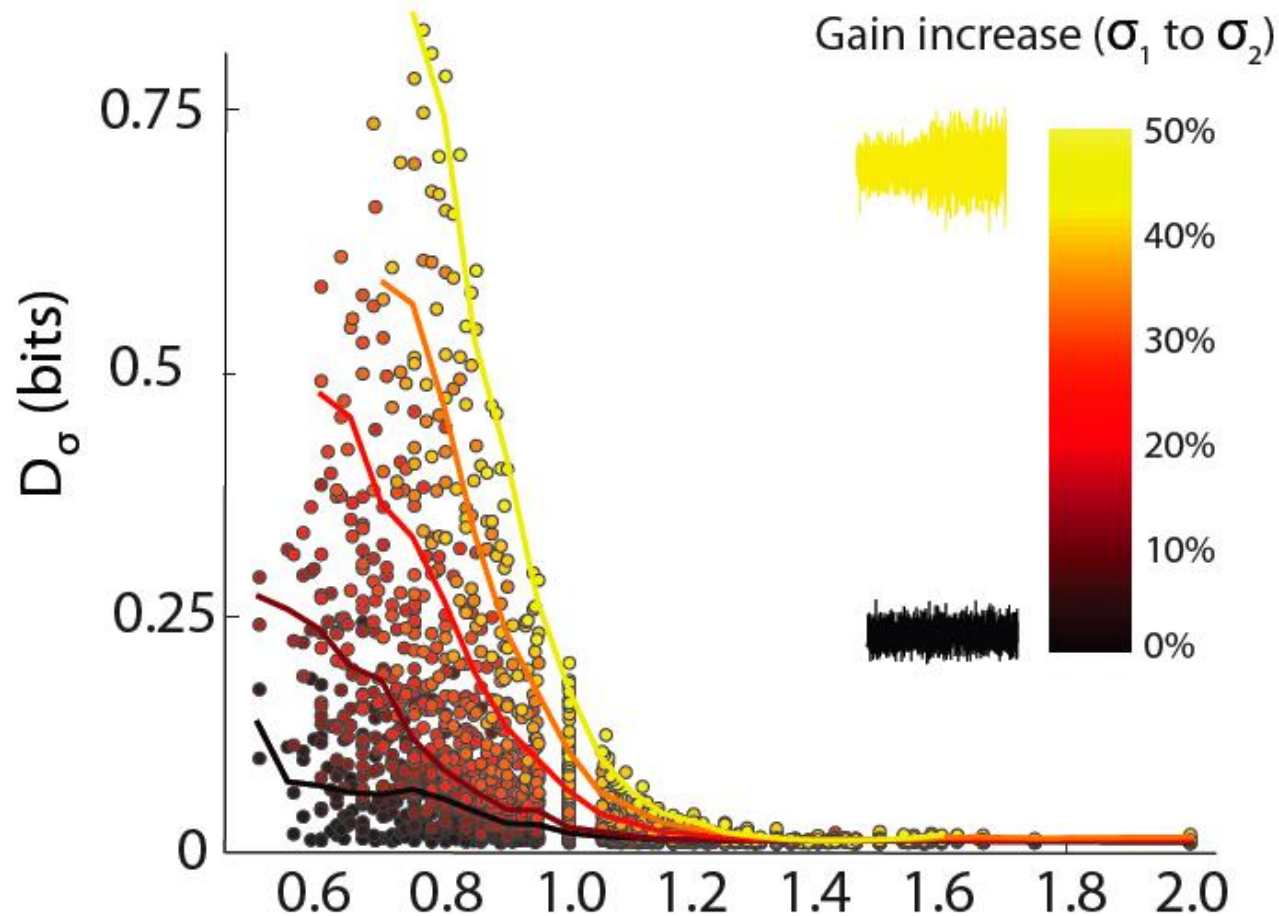
# Rate and LN model comparison

## STA Data and Simulation



# Back to biophysics

Experiment and biophysical modeling finds contrast adaptation is modulated by relative amounts of sodium and potassium conc



# Relating EIF to HH-style models

Minimize presence of active subthreshold channels  $1 \gg f(v)$  below threshold

Relating EIF parameters to channel properties

$$\frac{v_{th} - v_o}{\Delta} \approx 2.7 \quad \frac{v_o - v_r}{v_{th} - v_o} \approx 0.2$$

$$\frac{\bar{g}_{Na}}{\bar{g}_K} \sim \left( \frac{v_{th} - v_o}{v_o - v_r} \right) e^{\frac{v_{th} - v_o}{\Delta}} \left( \frac{v_o - E_k}{E_{Na} - v_o} \right) \left( \frac{\langle n(t) \rangle T_{ref}}{h(v_o) \tau} \right) e^{\frac{v_o - V_{1/2}}{\Delta}}$$

# Relating EIF to HH-style models

Minimize presence of active subthreshold channels  $1 \gg f(v)$  below threshold

Relating EIF parameters to channel properties

$$\frac{v_{th} - v_o}{\Delta} \approx 2.7 \quad \frac{v_o - v_r}{v_{th} - v_o} \approx 0.2$$

$$\frac{\bar{g}_{Na}}{\bar{g}_K} \sim 3 \left( \frac{v_o - E_k}{E_{Na} - v_o} \right) \left( \frac{\langle n(t) \rangle T_{ref}}{h(v_o) \tau} \right) e^{\frac{v_o - V_{1/2}}{k_m/3}}$$

$$\frac{\bar{g}_{Na}}{\bar{g}_K} \sim 1$$

# Summary

We introduced a general mathematical framework for thinking about how neural codes arise from dynamics

We derive and explain LN model properties for the exponential integrate-&-fire model

Specific neural coding properties strongly constrain dynamics

- perfect contrast adaptation requires only properly-tuned spike-generating currents

Strong predictions in simple models can lead to quantitative biophysical predictions