Glassy behavior in biological tissues

Complexity in Mechanics
KITP conference
UC Santa Barbara
October 22, 2014

M. Lisa Manning Syracuse University



Defects and vibrational

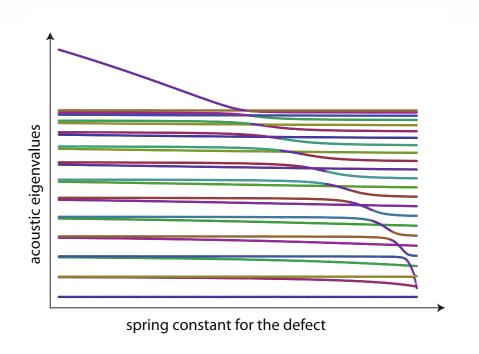
modes in disordered solids

Eigenfuctions are not as useful

 Eigenfuctions are not as useful away from instability

- Instead, find "flow defects" or "soft spots" or "STZs"
- A new and improved algorithm for identifying truly localized soft spots and energy barriers
 - long-ranged elastic tails generate lower energy barriers
- A random matrix definition of the boson peak Recorded KITP talk on this stuff

0.05 0.04 0.03 0.02 0.01 0.01 0.015 0.016 0.017 0.018 strain



http://online.kitp.ucsb.edu Avalanches

Thanks, Jim!





Manning group

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SU Soft Matter
Jorge Lopez
Jennifer Schwartz
Cristina Marchetti
Xingbo Yang





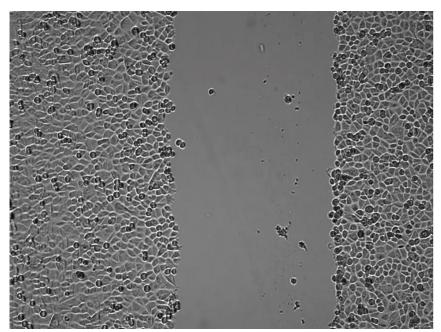
Amack group (SUNY Upstate Medical) Jeff Amack Guangliang Wang Agnik Dasgupta Schoetz lab and affiliates
Eva-Maria Schoetz (UCSD)
Marcus Lanio (Princeton)
Jared Talbot(Princeton)
Ramsey Foty(Princeton)
Mal Steinberg(Princeton)

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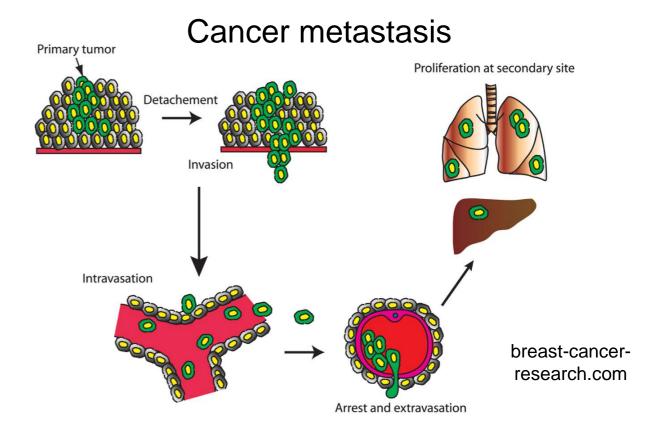
Turner Group(SUNY
Upstate)
Chris Turner
Nick Deakin

Complexity in mechanics....

Wound healing

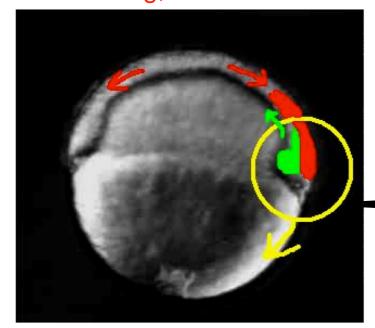


youtube.com/watch?v=v9xq_GiRXeE

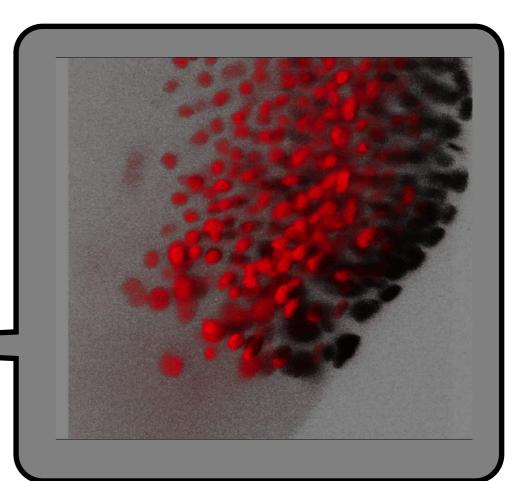


Embryonic development

Differential Adhesion Hypothesis: Steinberg, Science 1962



Schoetz 2008

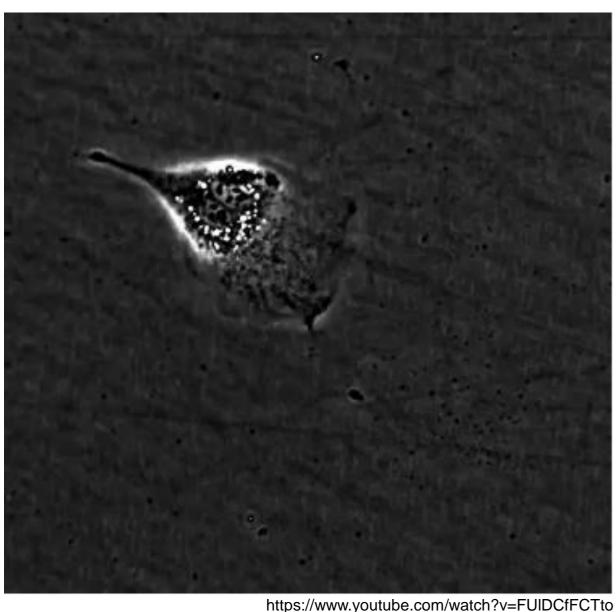


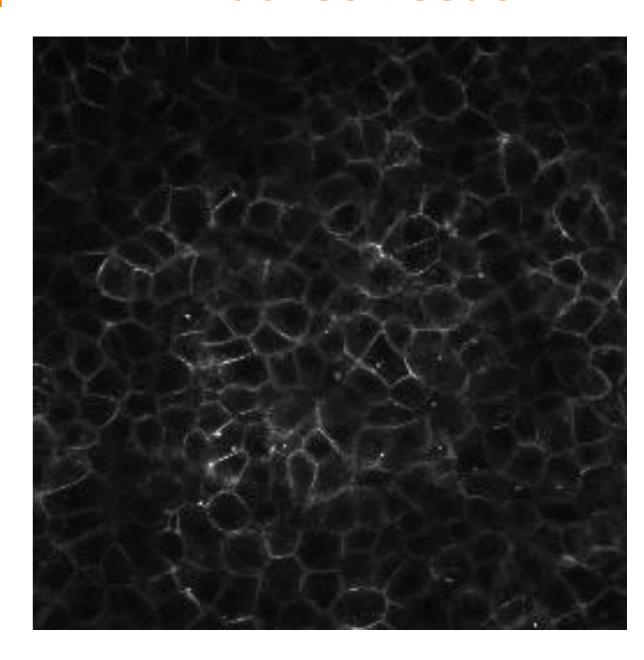
How do cells move?

In isolation

VS.

in dense tissue



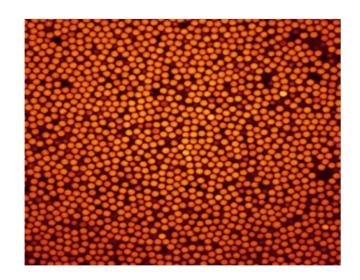


Human bone cancer cell on fibronectin

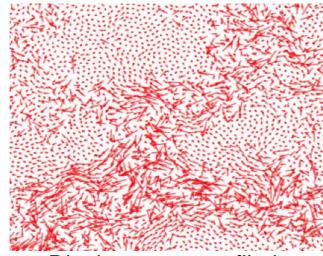
Zebrafish embryo Schoetz Lab, UCSD

Dense (non-active) materials

Thermal

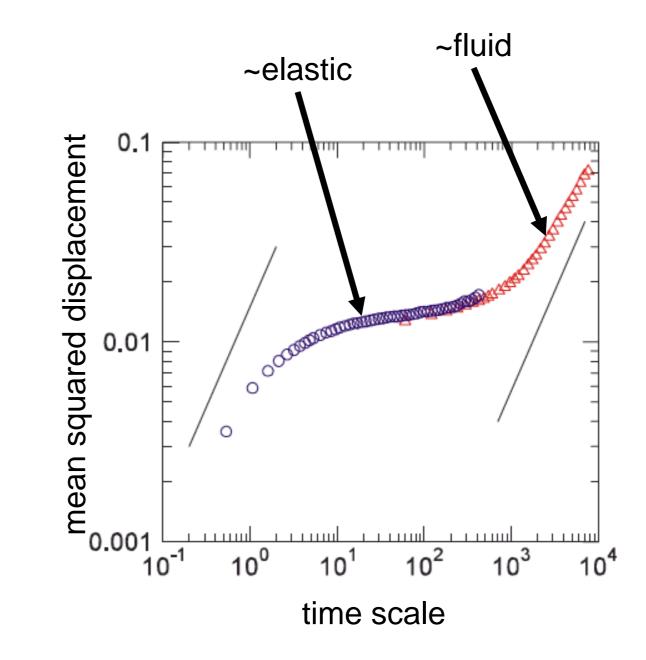


A colloidal glass.



Displacement profile in simulation of a 2-d glass former.

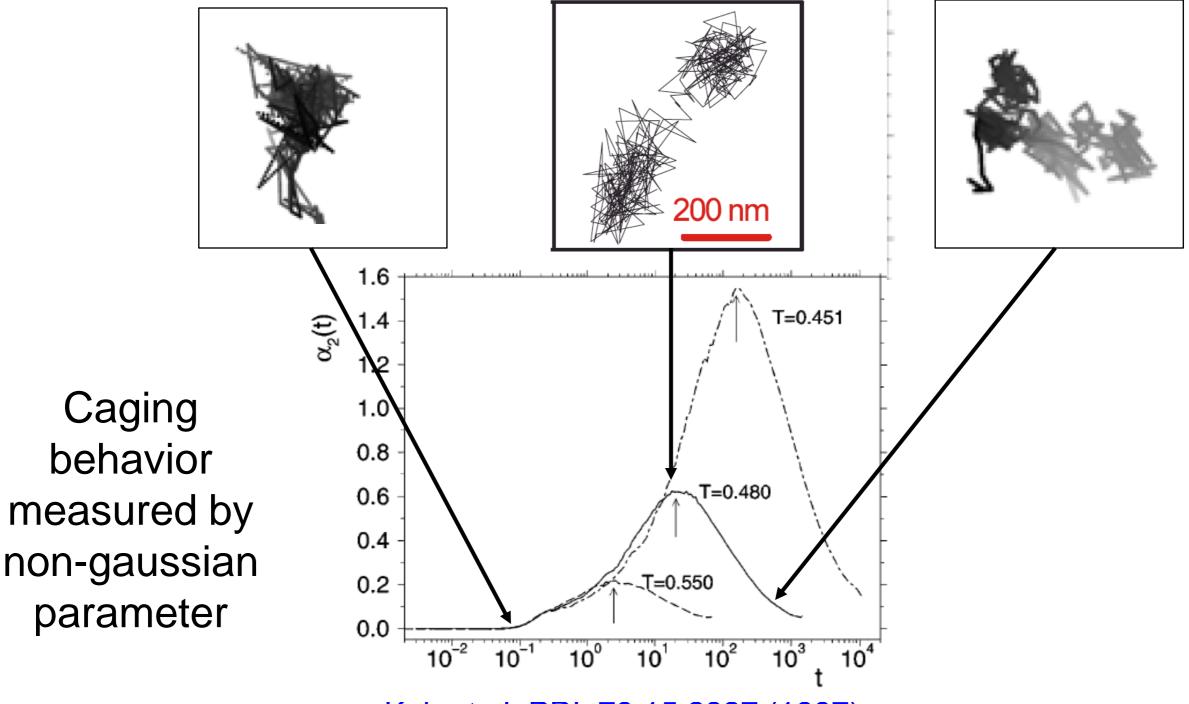
Berthier PRL 2011



Why do mechanical properties change with timescale?

non-active materials

Weeks, Crocker, Weitz (2004)

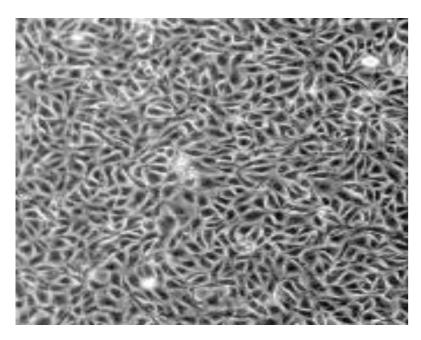


Kob et al, PRL 79 15 2827 (1997)

Dense biological tissues show the same

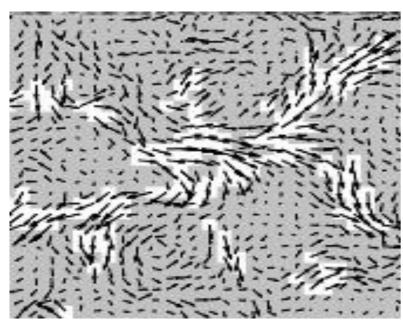


timescale ~ hours

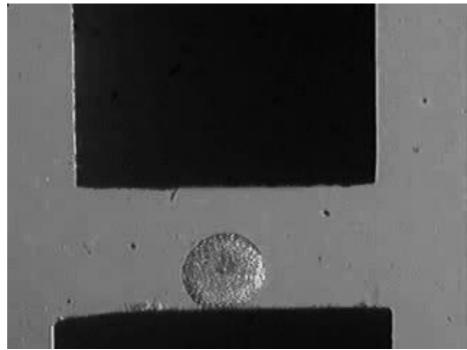


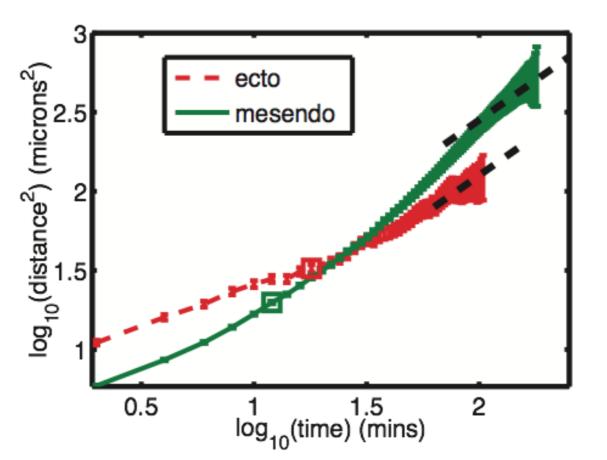
Madin-Darby canine kidney (MDCK) cells forming a 2-d confluent layer.

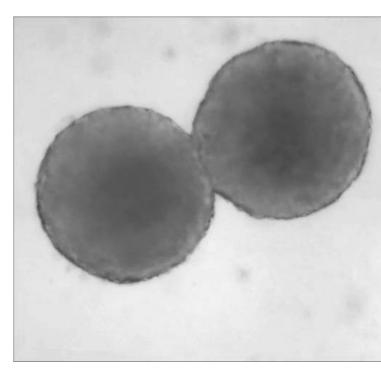
Angelini et al PNAS 2010



Velocity profile of cells show the spatially heterogeneous pattern in MDCK tissue.

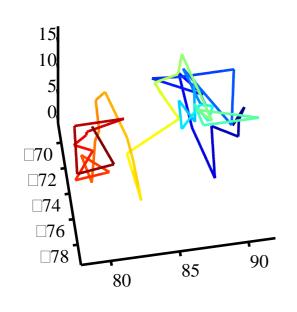


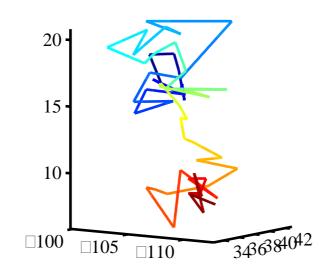


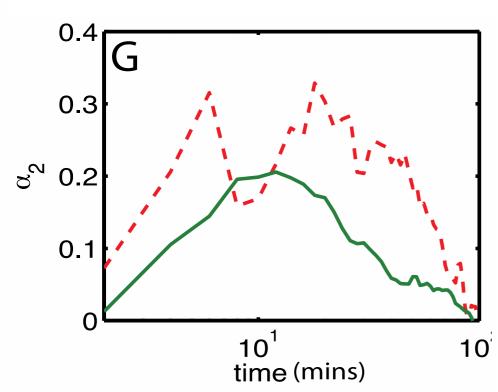


Schoetz, Lanio, Talbot, MLM J. R. Soc. Interface **10(89)**, 20130726 (2013)

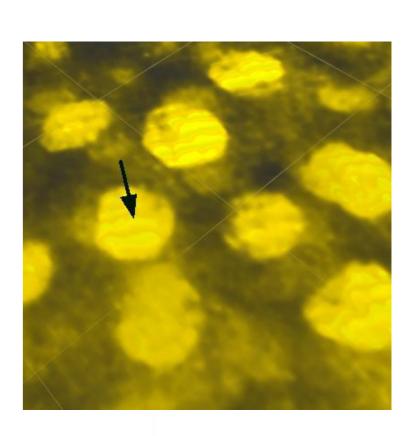
Why do mechanical properties change with timescale? biological tissues



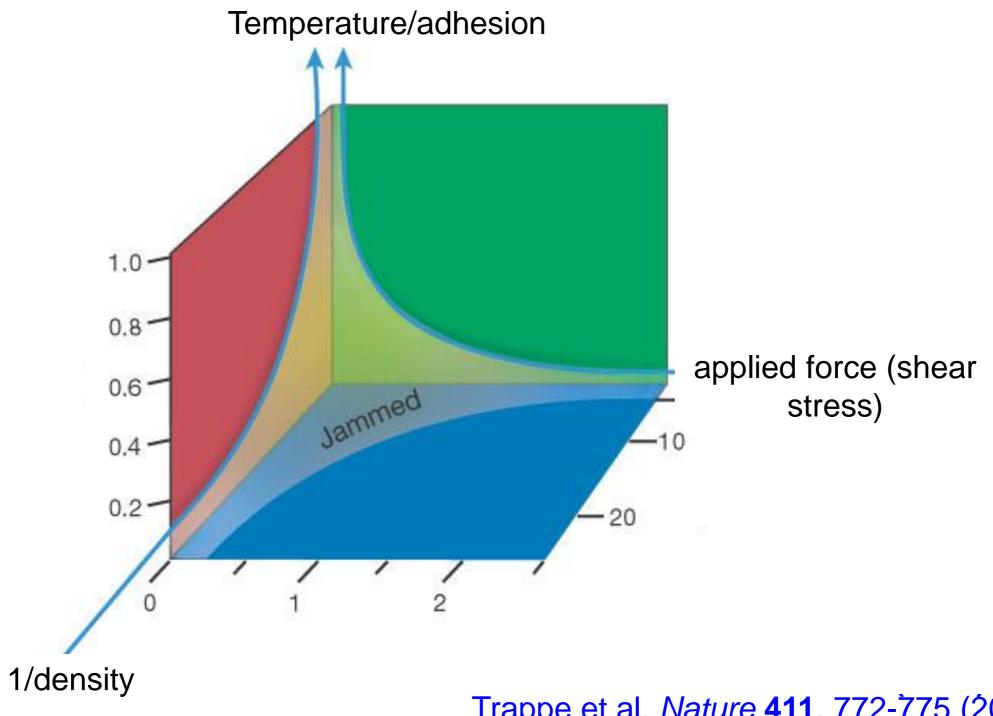




Schoetz, Lanio, Talbot, MLM J. R. Soc. Interface **10(89)**, 20130726 (2013)

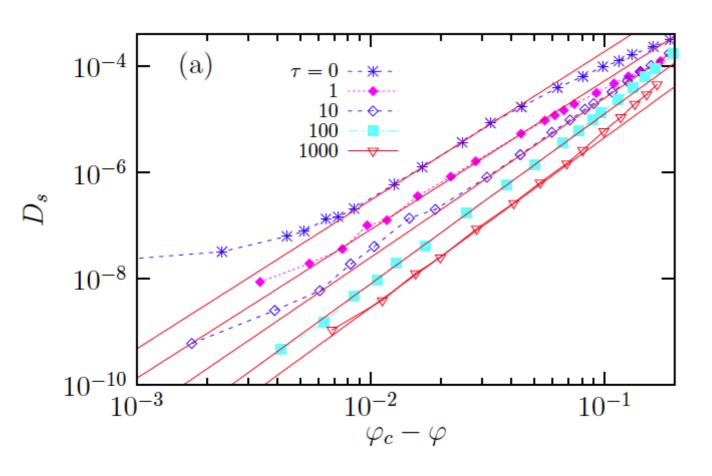


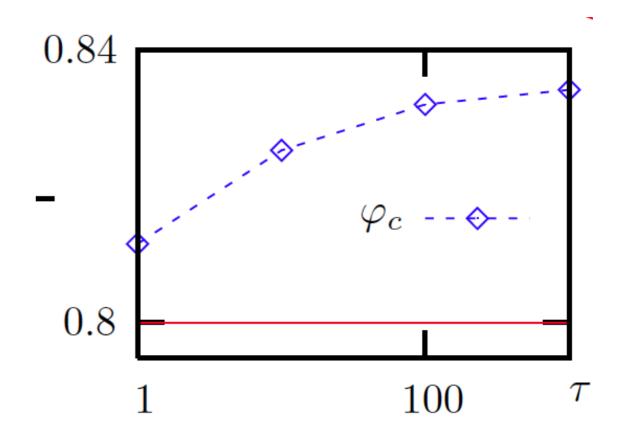
Jamming phase diagram for inert matter



Trappe et al, *Nature* **411**, 772-775 (2001)

Glass transition in self-propelled particle models is identical to adhesive colloids*

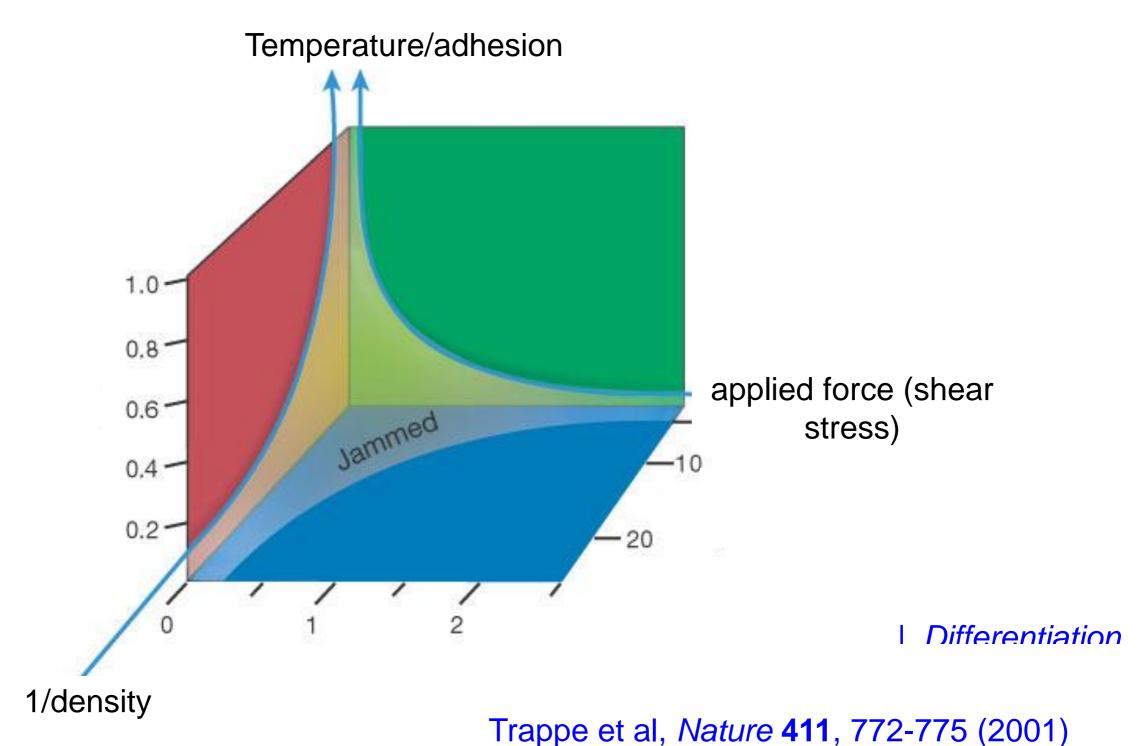




Berthier, PRL 112, 220602 (2014)

*almost: The critical packing fraction changes with the persistence time of the self propelled particles, because the activity generates an effective adhesion

Jamming phase diagram for biological tissues



Vector near jamming transition

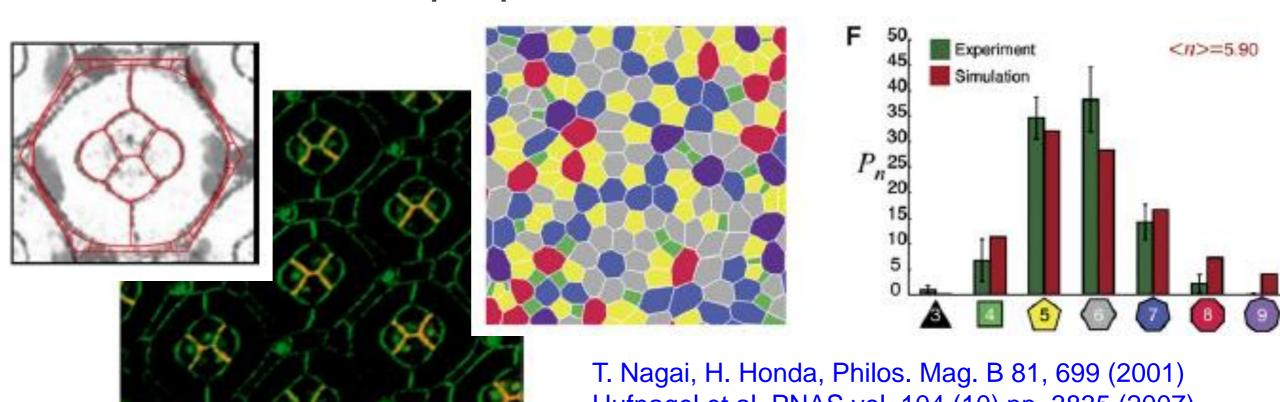
In many tissues, a densitydriven transition is impossible

e.g. confluent tissues where there are no gaps between cells and the packing fraction is one

Is there some analogue to the jamming transition for confluent tissues?

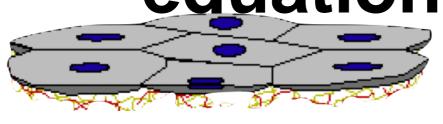
Vertex models for tissues

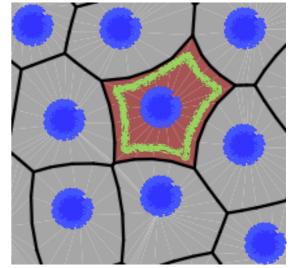
- Developed about 15 years ago
- Good agreement with experimentally observed cell shapes
- Explain/predict mechanically stable cell shapes and statistical properties



Hufnagel et al, PNAS vol. 104 (10) pp. 3835 (2007)
Farhadifar et al, Current Biology (2007)
Jülicher et al Phys. Rep. (2007)
Hilgenfeldt et al, PNAS 105 3 907–911 (2008)
MLM et al, PNAS (2010)
Staple et al EPJE 33 (2) 117 (2010)
Chiou et al PLOS Comp Bio 8 (5) e1002512 (2012)

Vertex model equations





$$E_{cell} = k_A (A-A_0)^2 + k_P (P-P_0)^2$$

$$= k_A (A-A_0)^2 + k_P (P^2-2P_0P+P_0^2) \quad \text{A = area, P = perimeter}$$

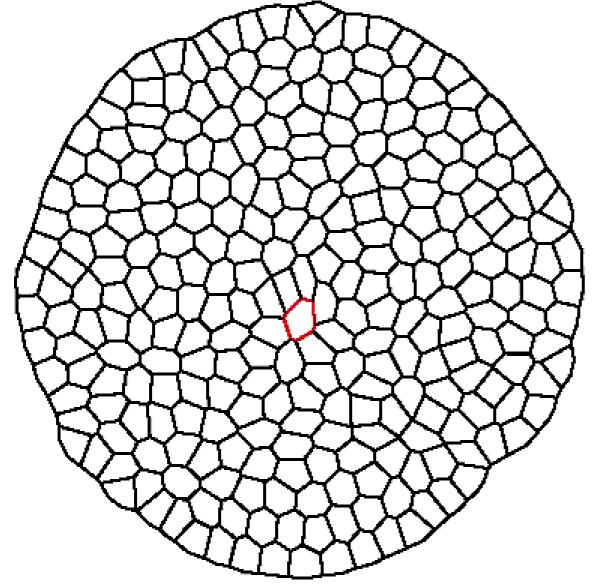
Interfacial tension: adhesion and cortical Incompressibility + tension resistance to heighto-myosin contractilty

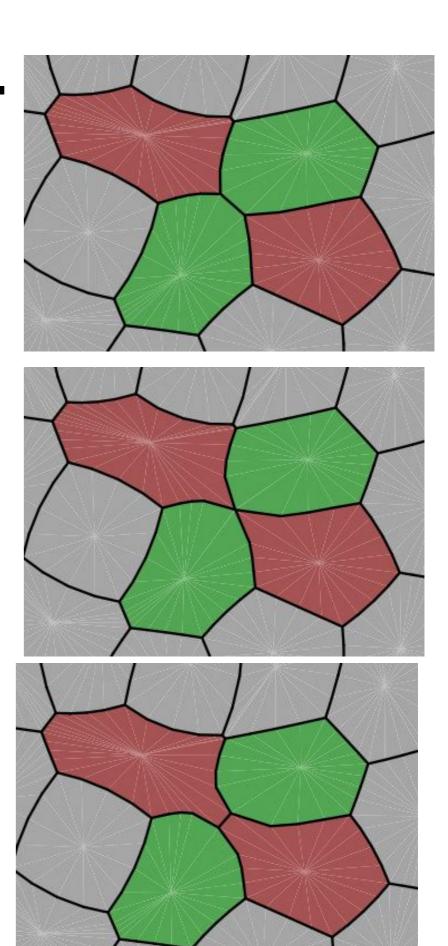
$$\varepsilon = \frac{1}{\beta A_0} \sum_{i}^{N} E_i = \sum_{i} \left[(a_i - 1)^2 + \frac{(p_i - p_0)^2}{r} \right] \quad \text{Non-dimensionalized mechanical energy}$$

Our model has two parameters:

- p₀ = preferred perimeter: interfacial tension generated by adhesion and cortical tension
- r = inverse perimeter modulus: resistance to height fluctuations normalized by perimeter contractility OR ratio between bulk stiffness and interface stiffness

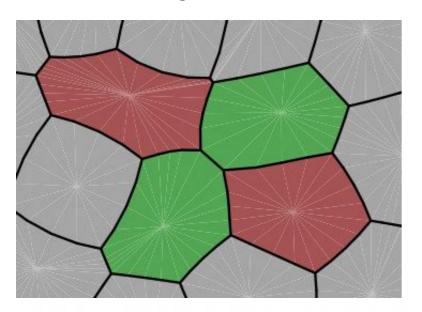
Rearrangements and migration in tissues via T-1 transitions



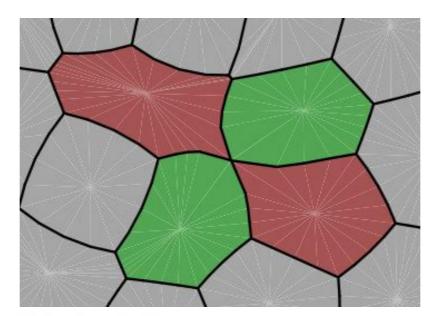


Energy trace for T-1 transitions

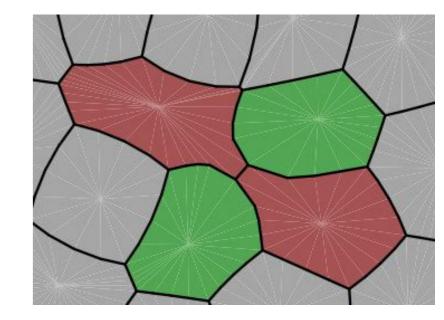
Shrink edge before T-1

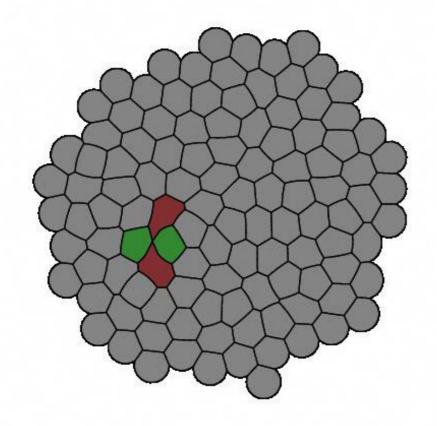


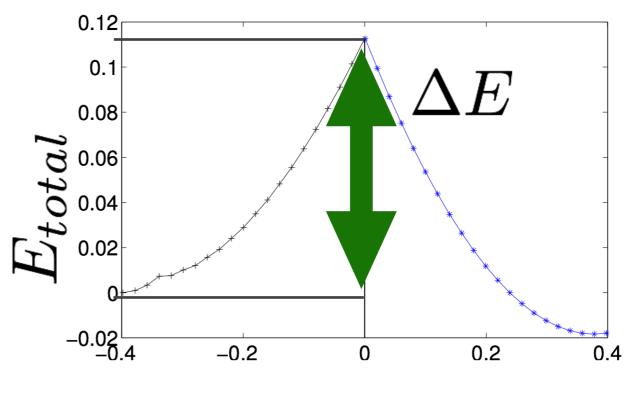
At T-1



Grow edge after T-1

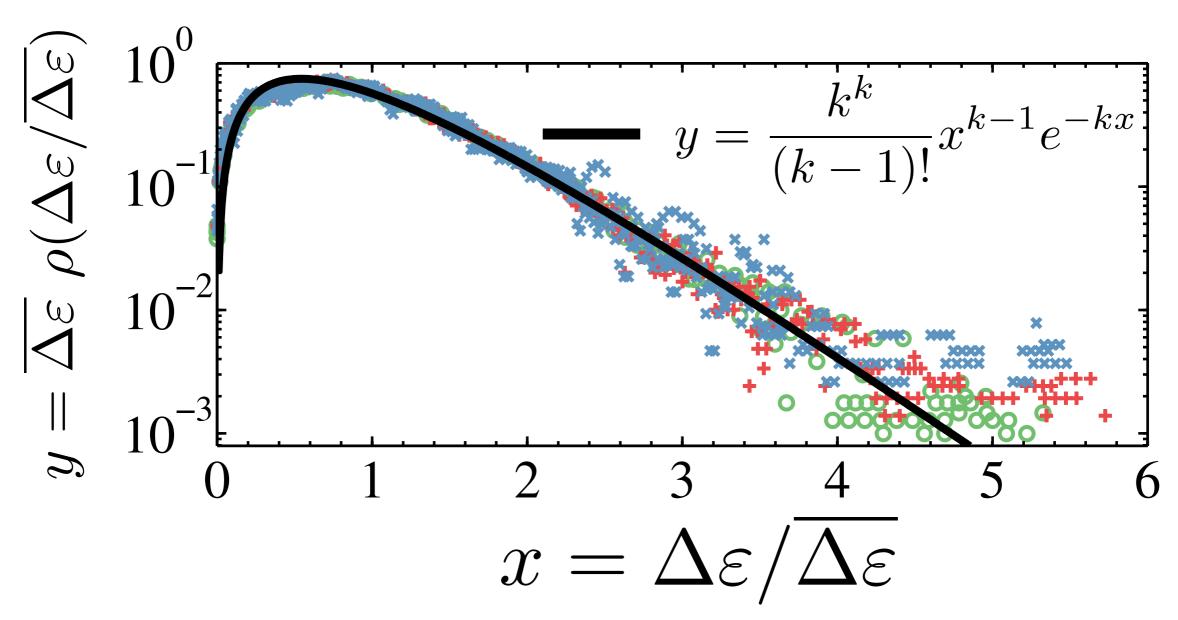






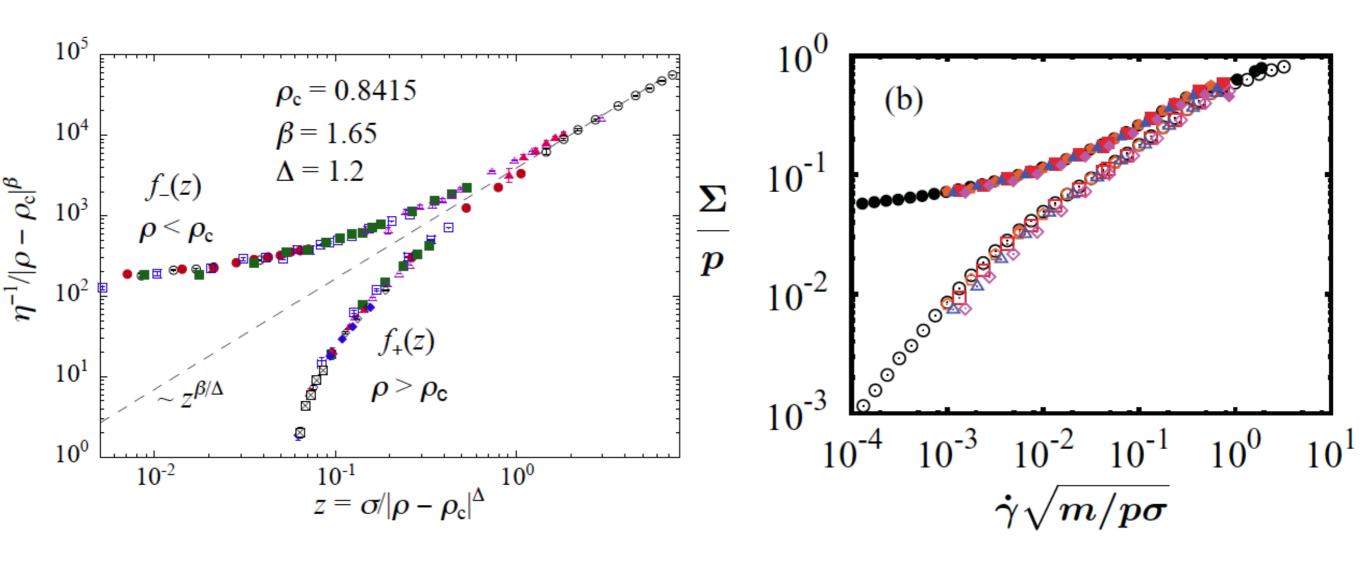
transition path L

Large tissues: energy barrier statistics determined entirely by the mean energy barrier height



k-gamma distribution with one fit parameter: k=2.2± 0.2 (found in many cellular systems)

Proving the existence of a critical "jamming" transition in inert matter:



Olsson and Teitel, PRL 99, 178001 (2007)

Haxton et al PRE 83, 031503 (2011)

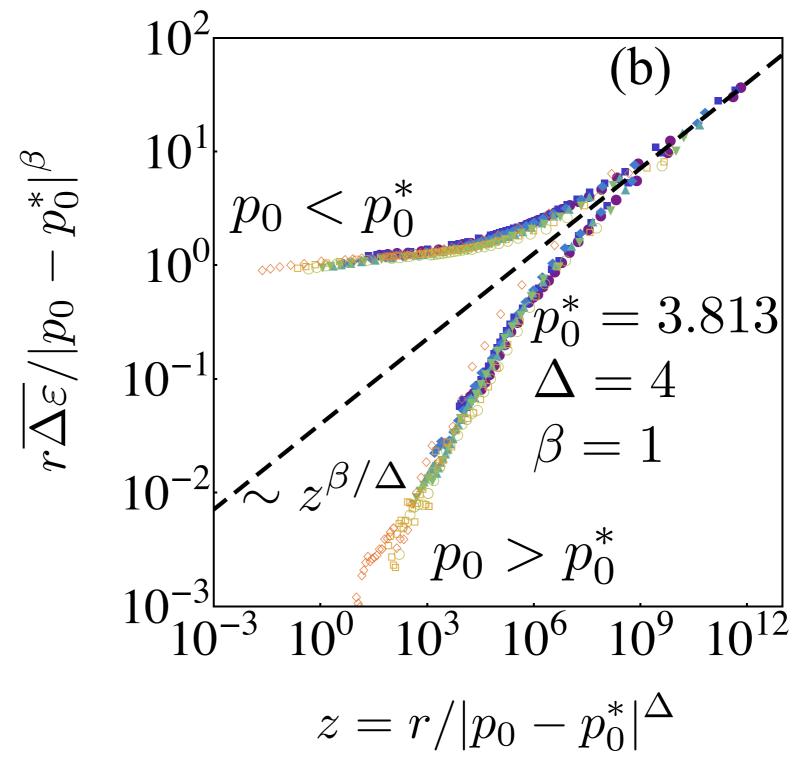
The onset of jamming is controlled by the **density**: $(\rho-\rho_c)$ ~ pressure

A critical rigidity transition controlled by p₀:

CHEAT SHEET: Average energy barrier height ~ yield stress

inverse perimeter modulus r ~ strain rate

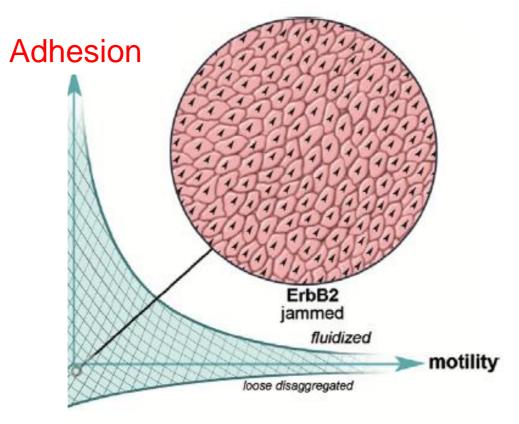
preferred perimeter $p_0 \sim density$



Bi, Lopez, Schwarz, MLM submitted (2014)

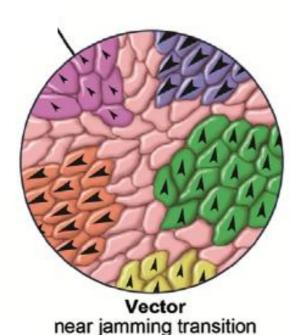
new rigidity phase diagram for biological tissues

Opposite for confluent tissues!

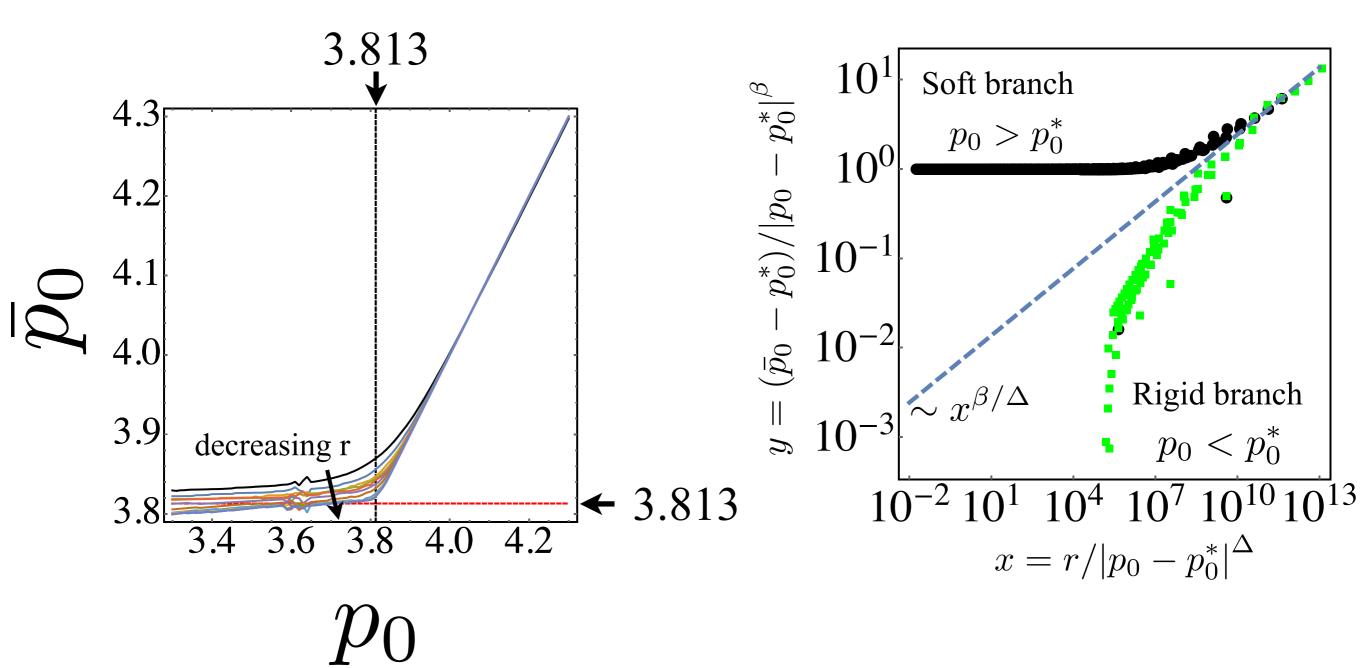


Particulate matter: axis is 1/adhesion

more adhesion means more gelation means more solid-like



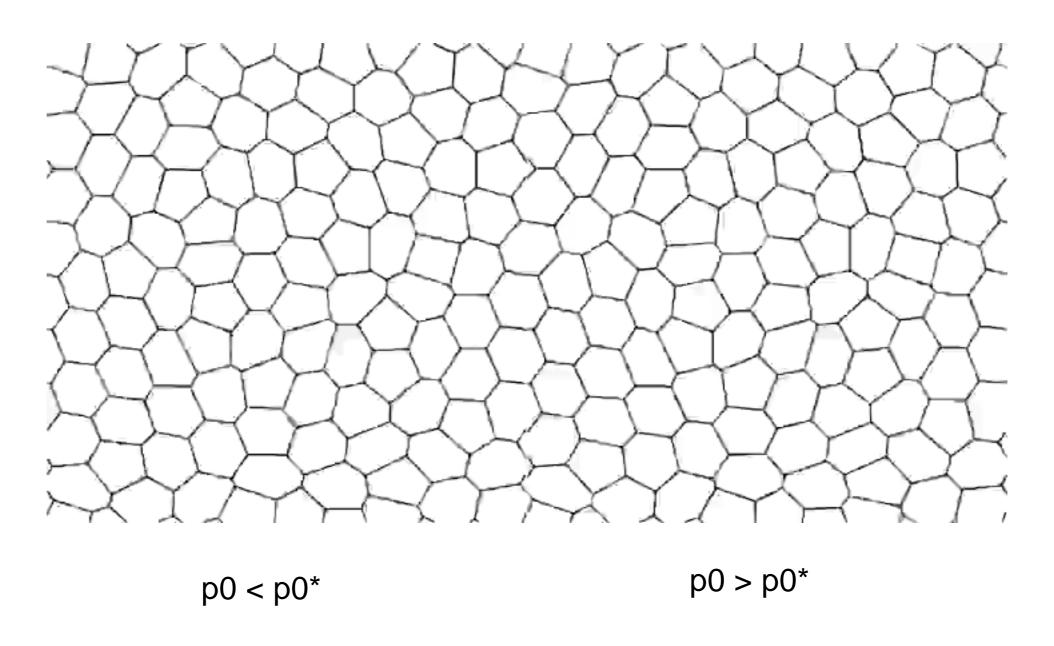
Experimental prediction



p0 is the average OBSERVED perimeter-to-area ratio:

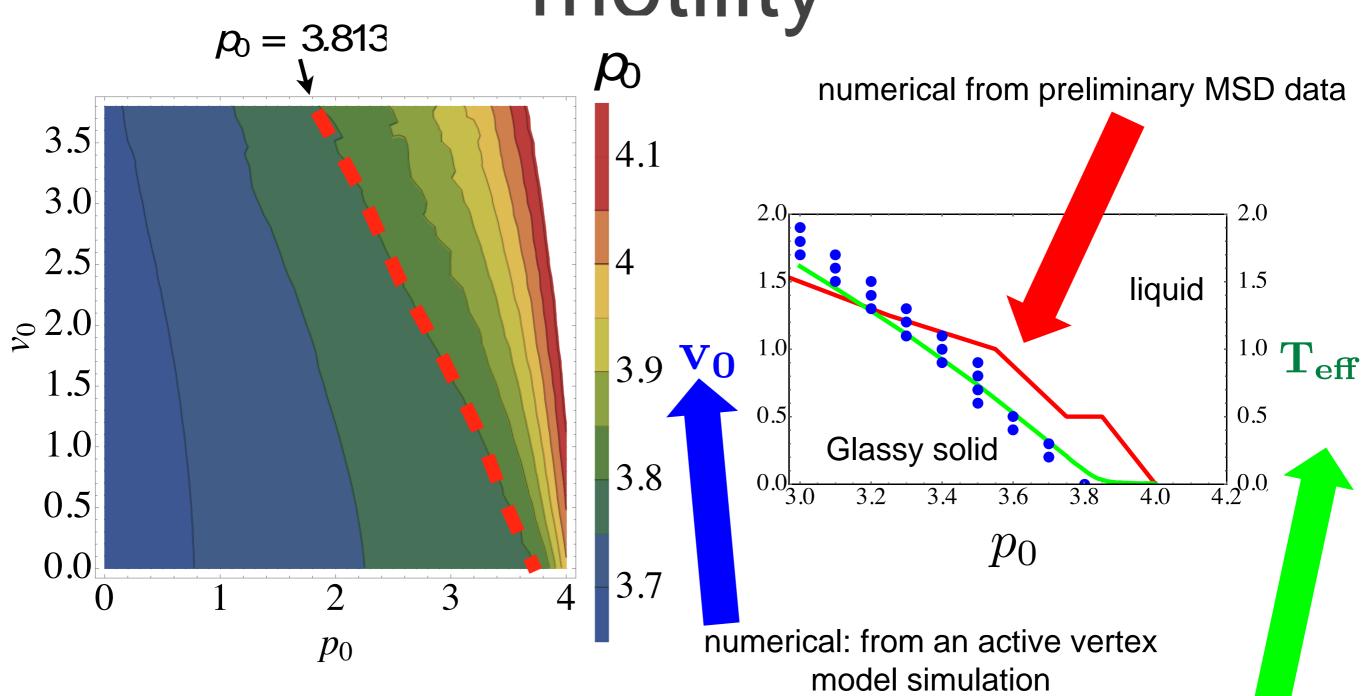
$$\bar{p}_0 = \langle p \rangle / \sqrt{\langle a \rangle}$$

Effect of finite cell motility?



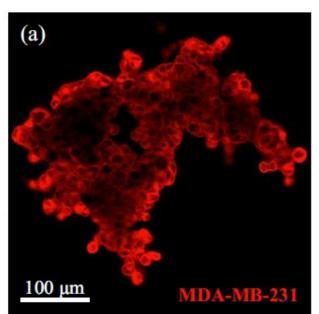
Add an equation for cell polarization (like in selfpropelled particle or Vicsek models)

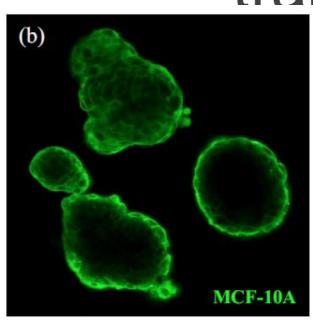
area ratio robust to cell motility

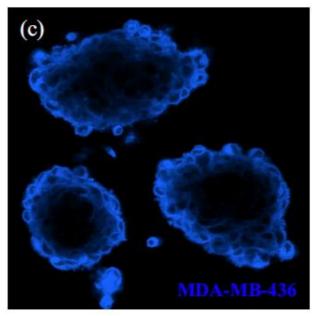


Analytic: from an extended SGR/trap model

Cancer tumor boundaries and the EMT transition



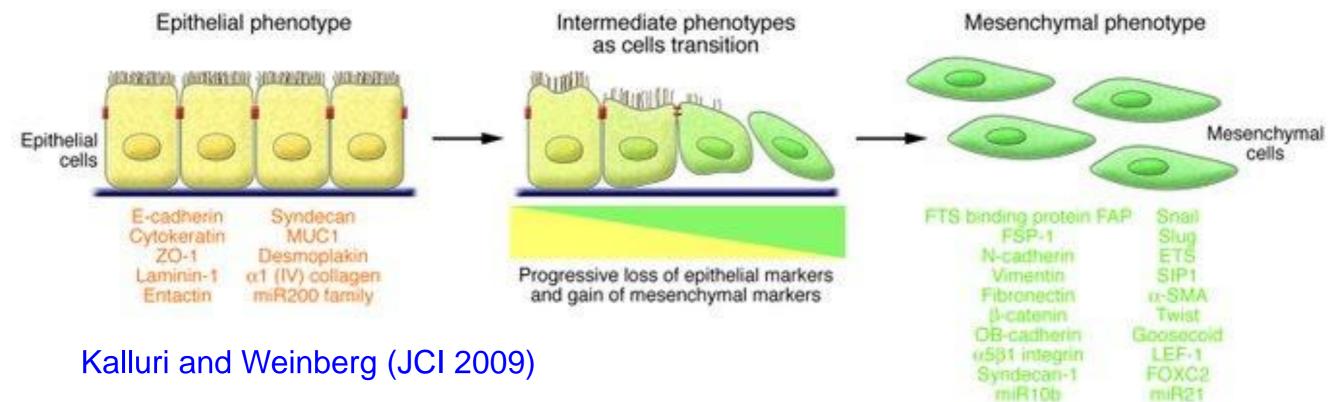




Cancer cell sorting not driven by differential adhesion/ tissue surface tension!

Pawlizak ... MLM ... Kaes, in preparation (2014)

- Could the EMT transition be thought of as a change in p₀ the ratio between the cell area and perimeter?
- If so, mesenchymal cells metastisize easily because they are on liquid side of rigidity transition?



Conclusions

- Biological tissues are complex materials, with mechanical properties that are important for biological function
- Many tissue types are apparently close to a glass transition
- The vertex model for confluent tissues exhibits a novel type of density-independent rigidity transition
 - excellent scaling collapse
 - control parameter is p₀, which is proportional to single-cell adhesion or preferred cell perimeter
 - this is opposite of what you'd expect from particulate matter
- This is a rich framework with lots more to do:
 - cancer cell migration
 - EMT transitions
 - collective modes
 - effect of cell motility

Thanks so much for your attention!

Collaborators:

- Max Dapeng Bi (SU)
- Jen Schwarz (SU), Jorge Lopez (SU), Eva-Mara Schoetz (UCSD), Marcus Lanio(Princeton), Jared Talbot(Princeton)
- Jeff Amack (Upstate), Guliang Wang (Upstate)

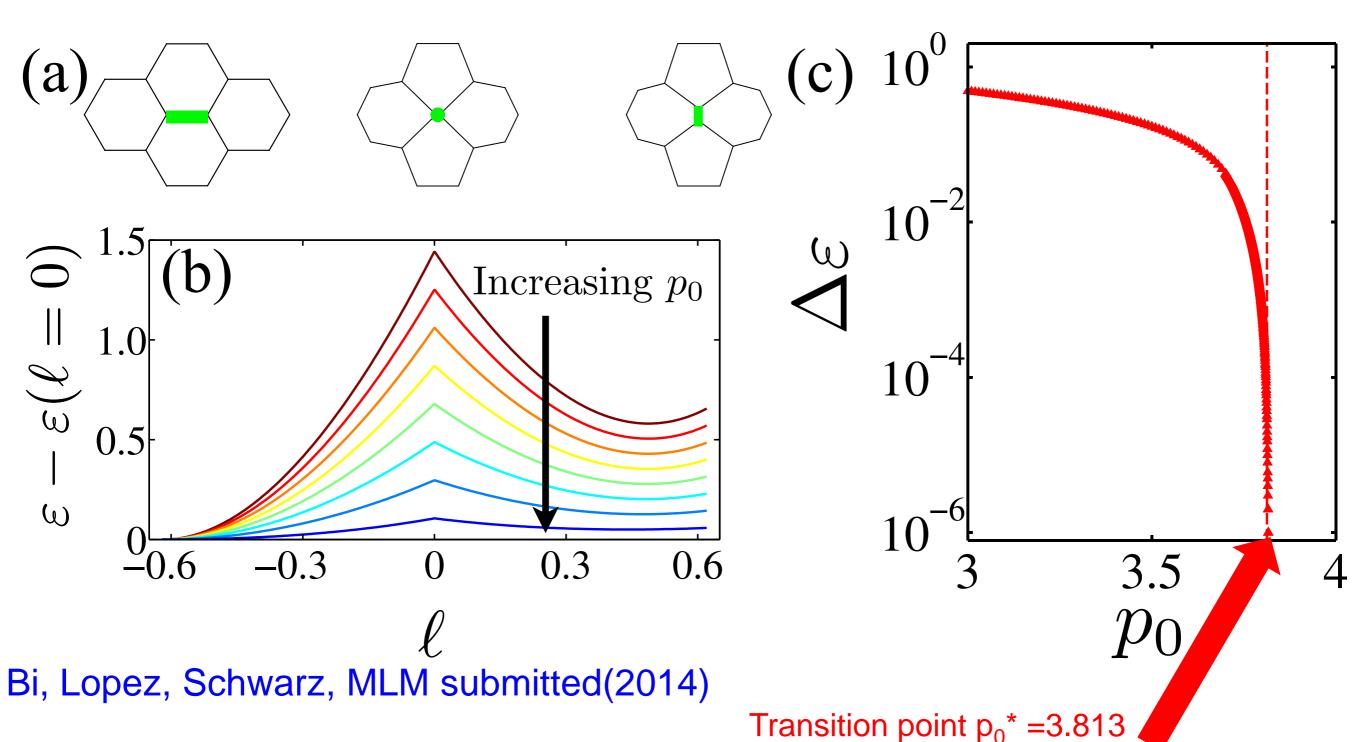
Funding:

- NSF BMMB CMMI-1334611
- NSF DMR CMMT-1352184
- Alfred P. Sloan Foundation
- Soft Interfaces IGERT (DGE-1068780)

http://www.phy.syr.edu/~mmanning/

NSR

Fixed area, four cells p₀ only control parameter

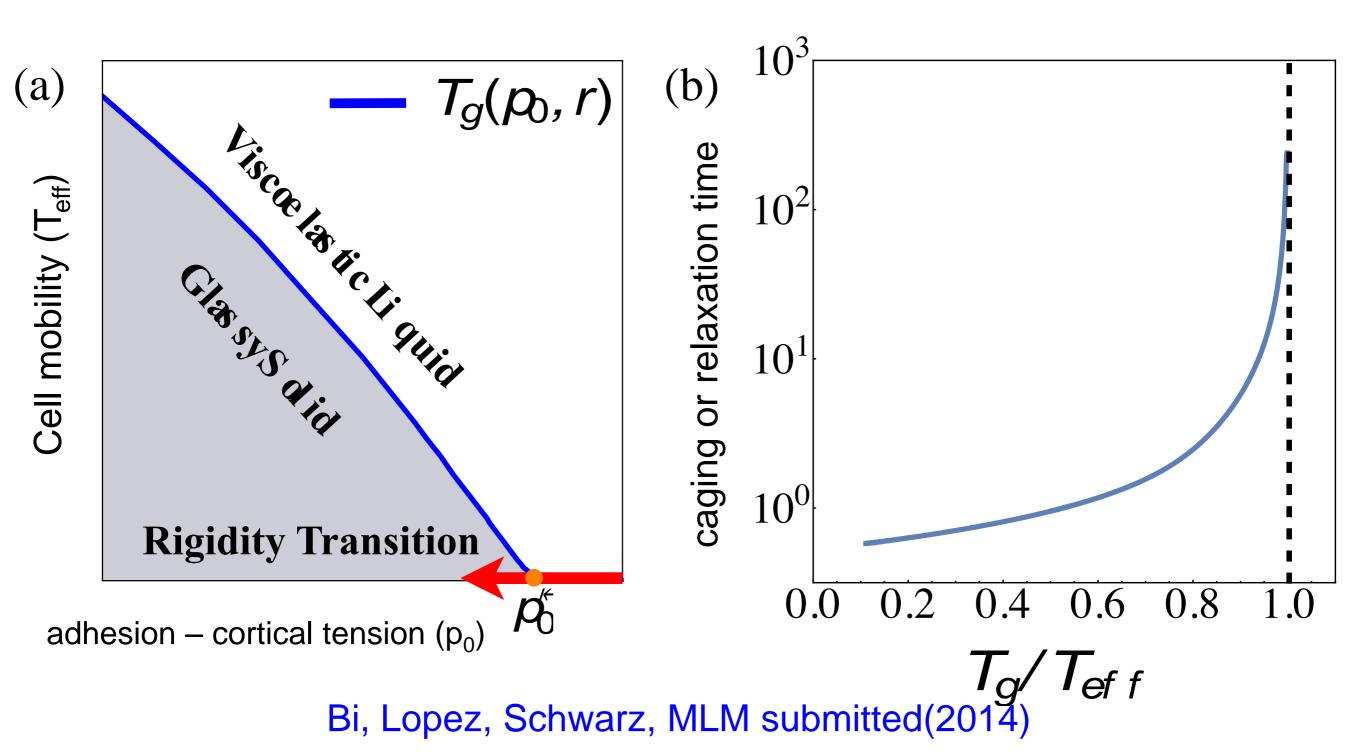


= perimeter of regular

pentagon with unit area

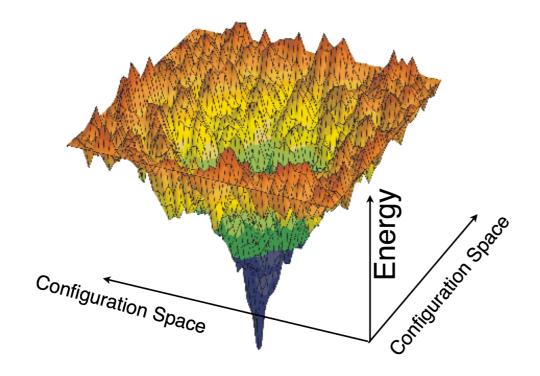
What happens when you include a finite cell activity or mobility?

Using a trap or SGR model to go from energy barriers to cell dynamics



When cells are actively fluctuating and moving, how does this change the transition?

Energy



 $e^{-\Delta E_1/k_BT}$ $e^{-\Delta E_2/k_BT}$ ΔE_2 state 1 state 2

energy landscape

system close to energy landscape surface

System is "trapped" in a metastable state until a rare fluctuation allows it to escape:

trap model C. Monthus and J.-P. Bouchaud, J. Phys. A 29, 3847 (1996) soft glassy rheology Sollich et al, PRL 78 2020 (1997)

From energy barriers to cell migration:

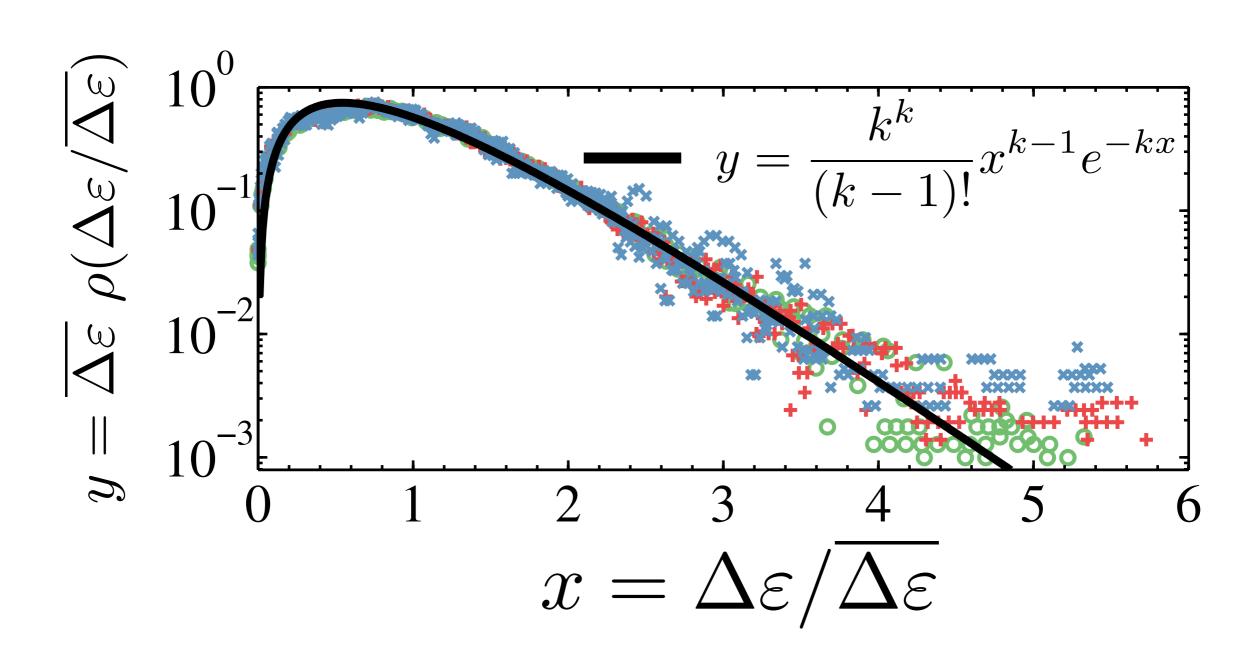
trap model: C.
Monthus and J.-P.
Bouchaud, J. Phys. A
29, 3847 (1996)

soft glassy rheology: Sollich et al, PRL 78 2020 (1997)

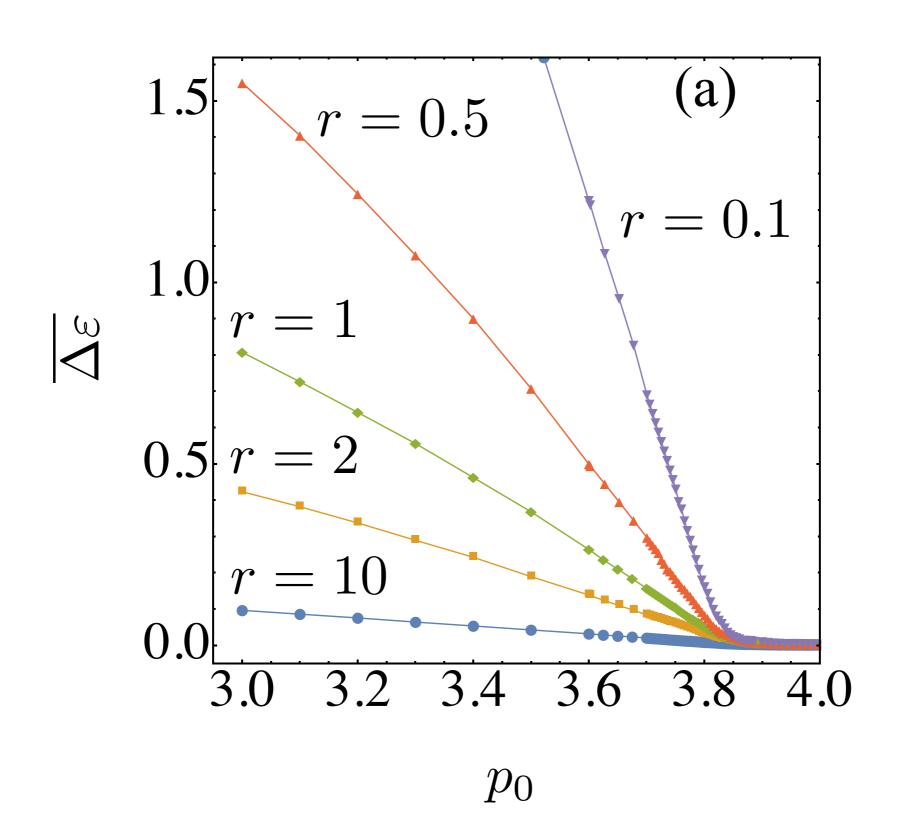
$$R=\omega_0 \exp\left[-(\Delta E-bt)/arepsilon
ight]$$
 models cell shape fluctuations ΔE

$$\frac{\partial}{\partial t}P(\Delta E,t) = -\omega_0 e^{-[\Delta E - bt]/\varepsilon}P(\Delta E,t) + \rho(\Delta E) \int d\Delta E' \omega_0 e^{-[\Delta E' - bt]/\varepsilon}P(\Delta E',t),$$

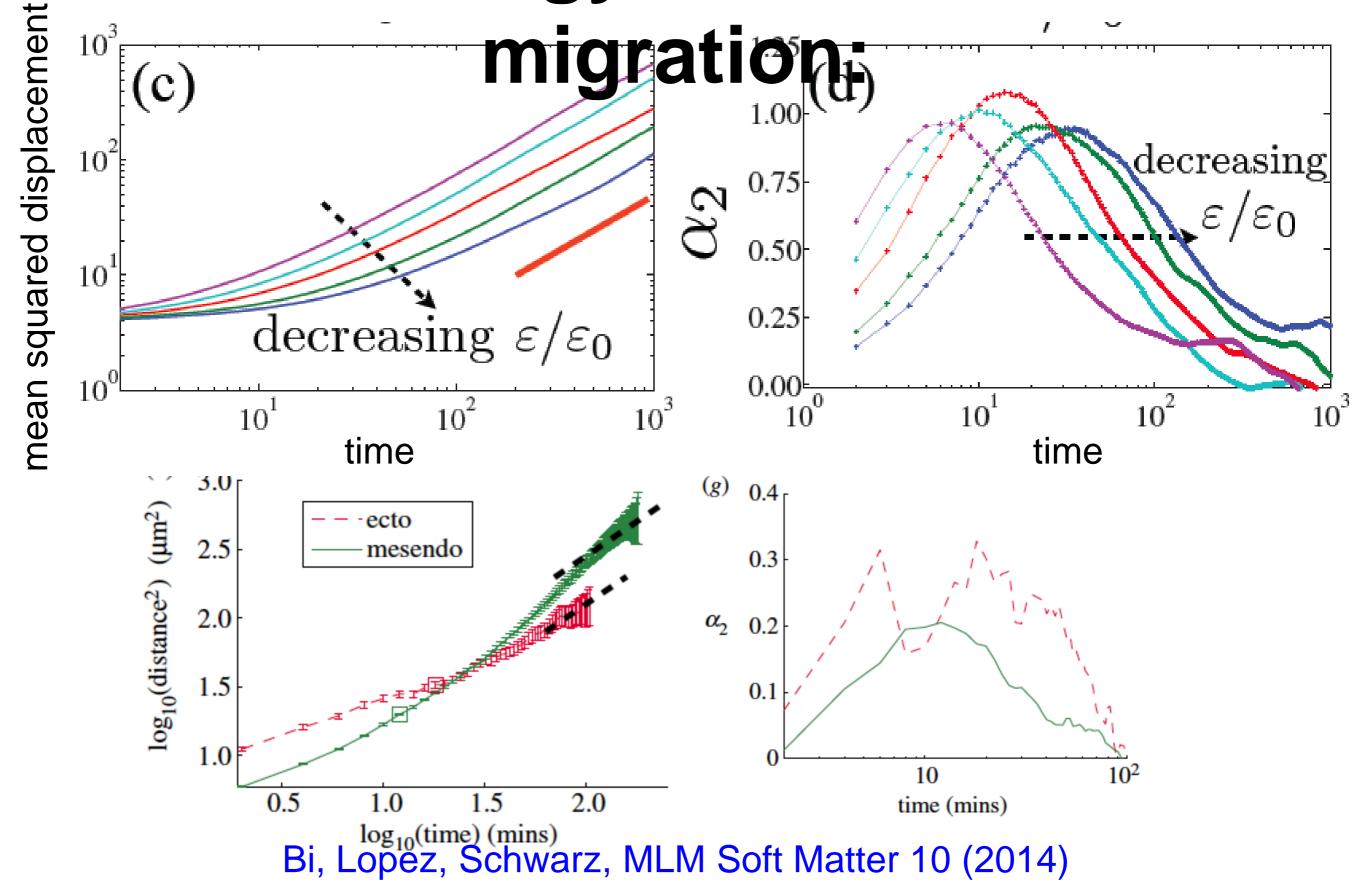
Exponential tail + trap model = glassy dynamics



Average energy barrier height vanishes at $p_0^* \sim 3.813$

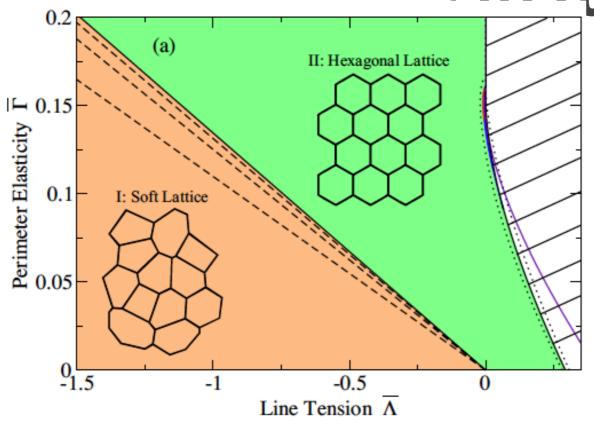


From energy barriers to cell



Previous results on ground

states:



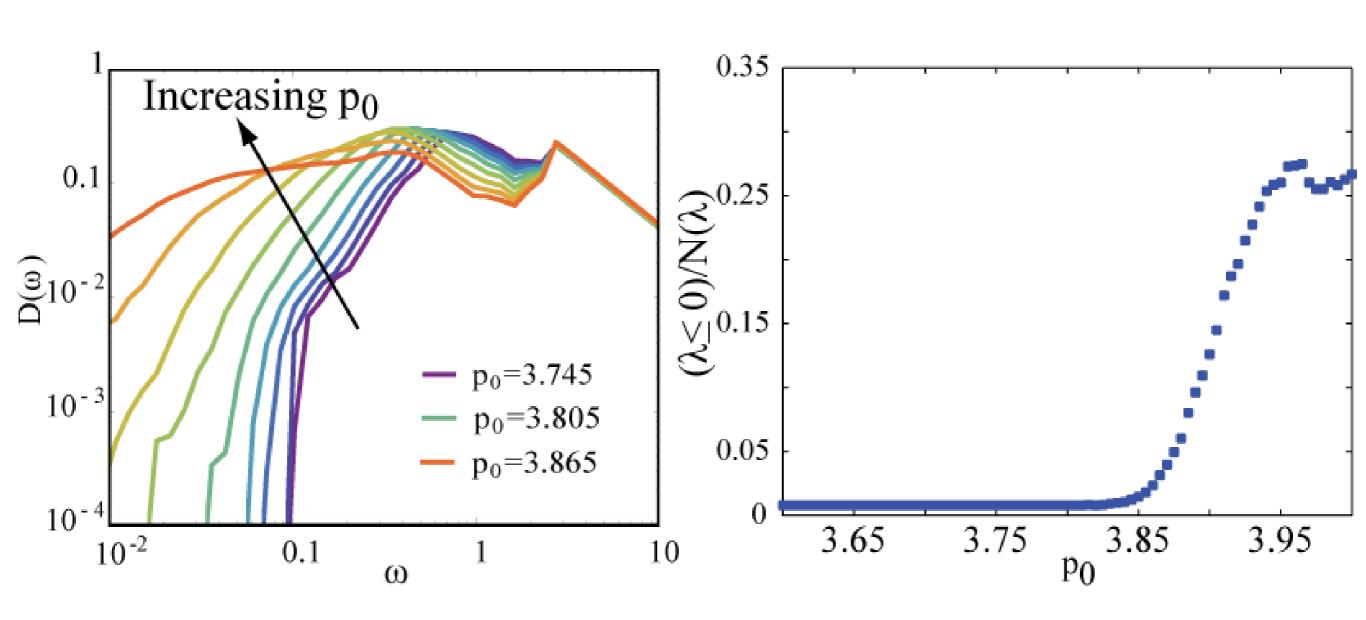
Staple et al EPJE 33 (2010)

$$a = 0.86$$
 $a = 0.90$

$$a = \frac{4\pi A}{L^2}$$

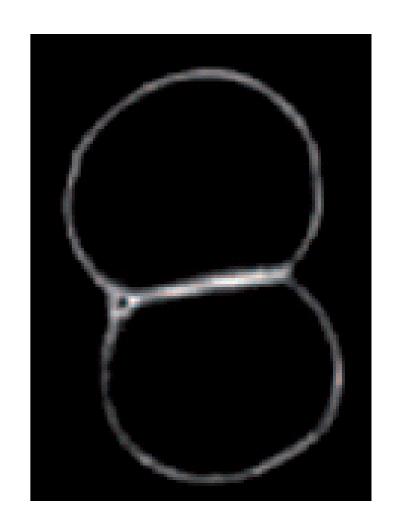
Hocevar and Ziherl PRE 80 11904 (2009)

What about normal modes? Collective behavior? Is it okay to study localized T1s?



"Shape equilibrium" or "vertex" model: what mechanical forces act to generate cell shapes?

- 1. Cell-cell adhesion: cadherins, alphacatenin, beta catenin, etc.
- Active cortical tension: myosin II, actin (Experiments: Evans, Theory: Joanny, Prost et al)
- 3. Bulk effects: fluid resists dialation/compression, cytoskeleton resists shear
- Cortical elasticity: cytoskeletal networks



Devries et al, Development **131**, 4435–4445 (2004)